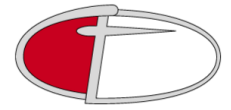
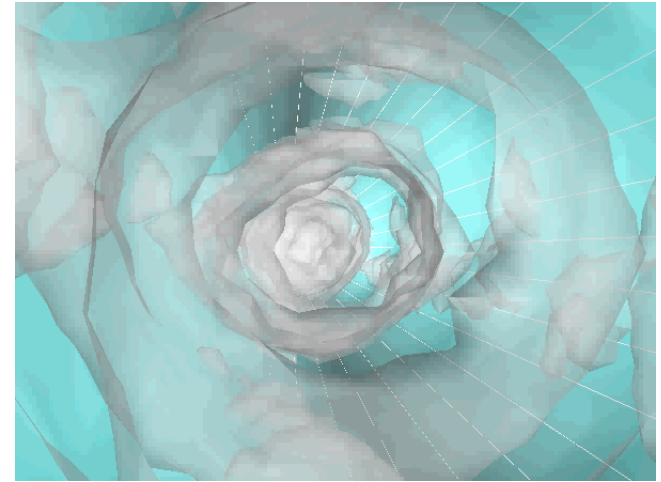


混相流における プロセス・トモグラフィー計測



Chiba University
Laboratory on Multiphase
Flow and Visualization



千葉大学大学院工学研究科
人工システム科学専攻 機械系コース
武居 昌宏

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- **PTの概要 ソフトフィールドとハードフィールド**
- **ソフトフィールドPT**
 - **原理**
 - **プラントへの展開**
 - **血流への展開**
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- **ハードフィールドPT**
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- **まとめ**

トモグラフィーとは

Wikipediaより

tomo- 【連結】切断{せつだん}、切開{せっかい}、部分{ぶぶん}

graphy 【連結】記述法{きじゅつほう}、書法{しょほう}、画法{がほう}

トモグラフィー

逆解析技術(逆問題: 結果から原因を見つける問題) で、対象領域を取り囲む形でセンサ(線源(ソース)と検出器)を配置し、内部の物性(電気的な物性、機械的な物性など)の分布を調べる技術。

CT コンピューティッド・トモグラフィー

PT プロセス・トモグラフィー

医療用トモグラフィーとプロセス・トモグラフィー

医療用トモグラフィー

X-ray or NMR

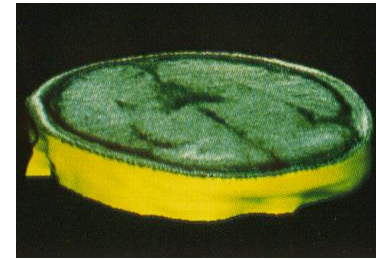
静止した人体内部

高空間解像度

低時間解像度



日立メディコWebより



ウィキペディアWebより

Fig. Tomographic image of inside head by medical CT

混相流への応用

プロセス・トモグラフィー

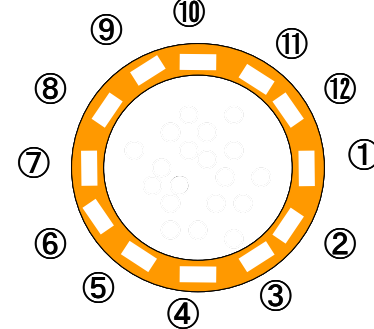
低空間解像度

高時間解像度



PTLのWebより

Pipeline Electrode



Particle

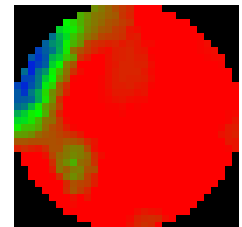
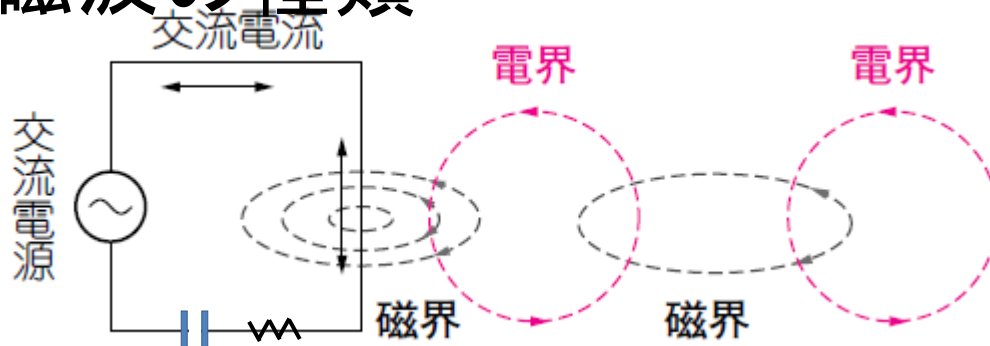


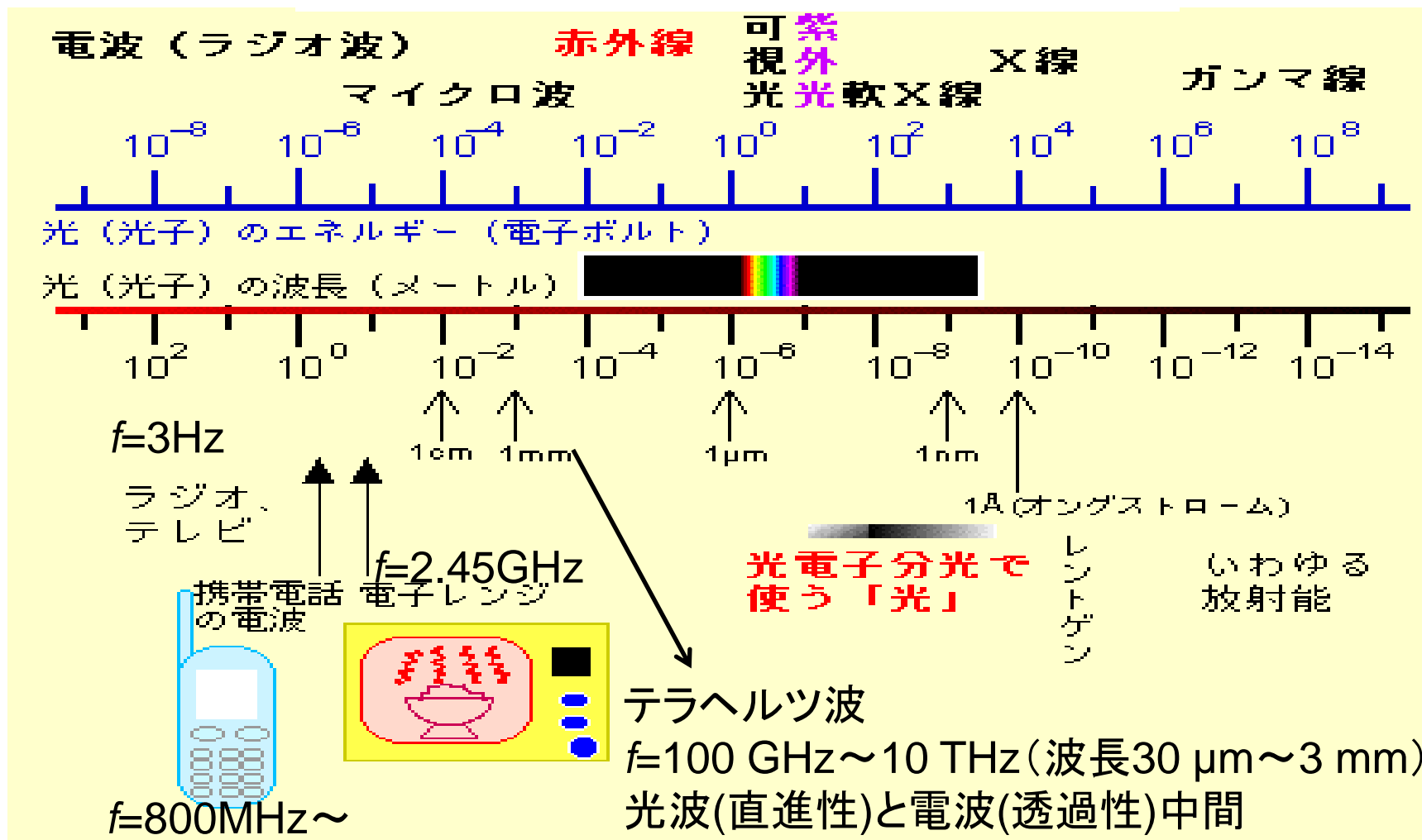
Fig. Overview of PT for particle flow

交流電流と電磁波の種類

ソフトフィード:
交流電流で混相流
の抵抗やキャパシタ
ンスを計測



ハードフィード
電磁波で混相流
の透過、屈折、反
射度を計測



ハードフィールド・トモグラフィーにおける線の分類

●電磁波(Electromagnetic wave)

空間の電場と磁場の変化によって形成された横波となって伝播する波動。波長の長い方から、電波・赤外線・可視光線・紫外線・X線・ γ 線など

●粒子線(Particle beam)

イオン化された原子や分子などの粒子が束状になって進んでいくビーム。例えば、電子線、陽子線(Proton,水素原子核)、 α 線(ヘリウム4原子核(陽子2個と中性子2個))、 β 線(原子核(中性子)が β 崩壊する際に放出される電子または陽電子)、中性子線など。

●放射線(Ionizing radiation)

電離性を有する高いエネルギーを持った電磁波や粒子線(ビーム)

強い電離作用(軌道電子をはじき飛ばすことによって、原子を陽イオンと電子に分離する作用)や蛍光作用を有する。

例えば、 α 線、 β 線、 γ 線、中性子線、X線

●放射線の透過能力

α 線 紙1枚程度

β 線 厚さ数mmのアルミニウム板

γ 線 透過力が強く、コンクリートで50cm程度、鉛で10cm程度。

中性子線 最も透過力が強く水やコンクリートの厚い壁に含まれる水素原子によって遮断される。

ハードフィールドPTの歴史

●ヨハン・ラドン(Johan Radon) オーストリアの数学者 1917年 ラドンの画像再構成則

“Über die Bestimmung von Funktionen durch ihre Integralwerte I” angs gewisser Mannigfaltigkeiten *Math.-Phys.Kl.*, 69, 262 267
三次元物体はその投影データ(Projection data)の無限集合から一意的に再生できる

●アラン・コーマック(Allan MacLeod Cormack)
アメリカの物理学者。コンピュータ断層撮影 (CT) 技術の開発により、1979年にノーベル生理学・医学賞を受賞。Journal of applied physics (1963,1964)CT理論の論文を公表

●ゴッドフリー・ハウズフィールド(Godfrey Hounsfield)
イギリスの電子技術者。コーマックCT理論を用いて1972年にCT装置開発に成功
ノーベル生理学・医学賞(1979)にアラン・コーマックとともに受賞。



Fig. Godfrey Hounsfield
日本放射線技術学会雑誌
Vol58No1より転写

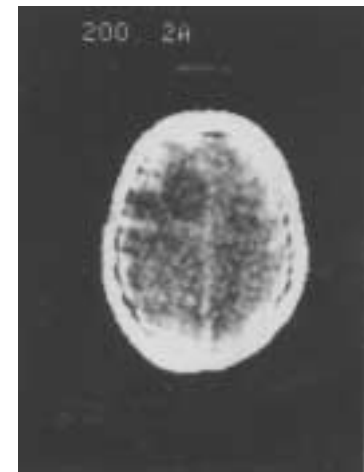


Fig.最初の臨床画像
(Atkinson Moley病院の
J.Ambrose医師とともに)

ハードフィールド・トモグラフィの基礎原理

Hard Field Sensorはソースからの走査線が対象内を直進する。
Soft Field Sensorは直進しない。

ランベルト・ベールの法則 Lambert-Beer law

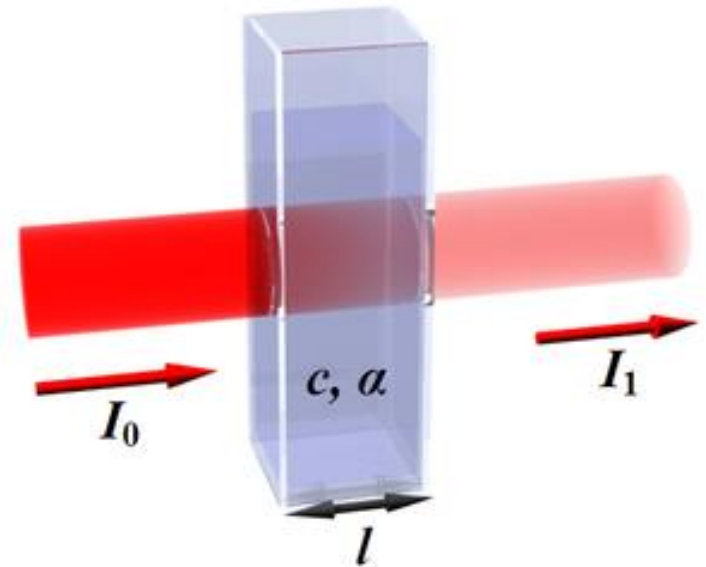
媒質に入射する前の光の放射照度を I_0 、媒質中を距離 L 移動したときの光の強度を I_1 としたとき

$$\log_{10} \left(\frac{I_1}{I_0} \right) = -\alpha L = -\epsilon c l$$

ここで α は吸収係数

$\alpha \propto$ 分散相の濃度

光吸収透過CT, 光干涉CT



ハードフィールド・トモグラフィー画像再構成の原理

●ランベルト・ベールの法則 $\int_s f(x, y) ds = \ln \frac{I_i}{I_0}$

$f(x, y)$: 断面吸収係数分布 I_i : 入射側の強度、
 I_0 : 透過強度 ds : 走査線に沿った線素

↓ x - y 座標系から角度 θ 回転した r - s 座標系
 $p(r, \theta)$: 投影データ

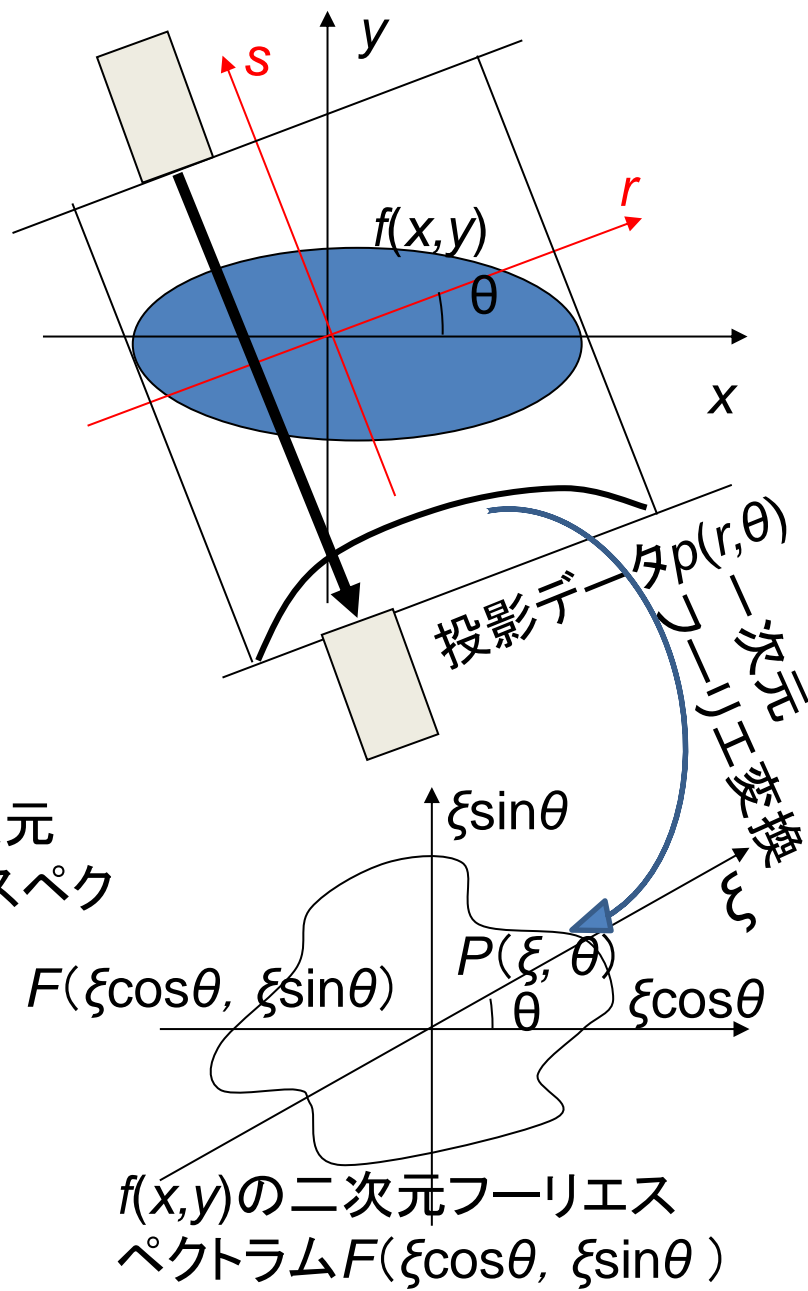
●ラドン変換

$$p(r, \theta) = \int_{-\infty}^{\infty} f(r \cos \theta - s \sin \theta, r \sin \theta + s \cos \theta) ds$$

●投影切断面定理: θ 方向の投影データの一次元フーリエスペクトラムは、 $f(x, y)$ の二次元フーリエスペクトラムの θ 方向の切断面に等しい

$$F(\xi \cos \theta, \xi \sin \theta) = \int_{-\infty}^{\infty} p(r, \theta) \exp(-j\xi r) dr$$

ξ : フーリエ級数の波数 ξ



フィルタ補正逆投影(FBP)法

$f(x,y)$: 断面吸収係数分布 | $|\xi|$: 波数 ξ の絶対値のフィルタ補正

$$f(x, y) = \int_0^{\pi} \left[\int_{-\infty}^{\infty} P(\xi, \theta) |\xi| \exp(j\xi r) r d\xi \right] d\theta$$

逆フーリエ変換

$P(\xi)$: 角度 θ のときの投影データ $p(r, \theta)$ の ξ (波数)における一次元フーリエスペクトラム

$$P(\xi, \theta) = \int_{-\infty}^{\infty} p(r, \theta) \exp(-j\xi r) r dr$$

フーリエ変換

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ソフトフィールド・トモグラフィ

走査線が対象内を直進しない

拡散光トモグラフィ

名称	対象となる二相流		測定と求める物理量	
	連続相	拡散相	測定物理量	求める物理量
キャパシタンス・トモグラフィ (ECT)	非導電性物質(空気)	誘電性物質(粒子)	キャパシタンス	誘電率分布 Permittivity ϵ
抵抗トモグラフィ (ERT)(EIT)	高導電性物質(水)	抵抗物質(粒子)	電流流したときの電位	導電率分布 Conductivity σ
磁気インダクタンス・トモグラフィ (EMT)	非透磁性物質(空気)	透磁性物質(磁性粒子)	渦電流によるコイル内の電流変化	透磁率分布 Permeability μ

ソフトフィールド・トモグラフィーのハードウェア

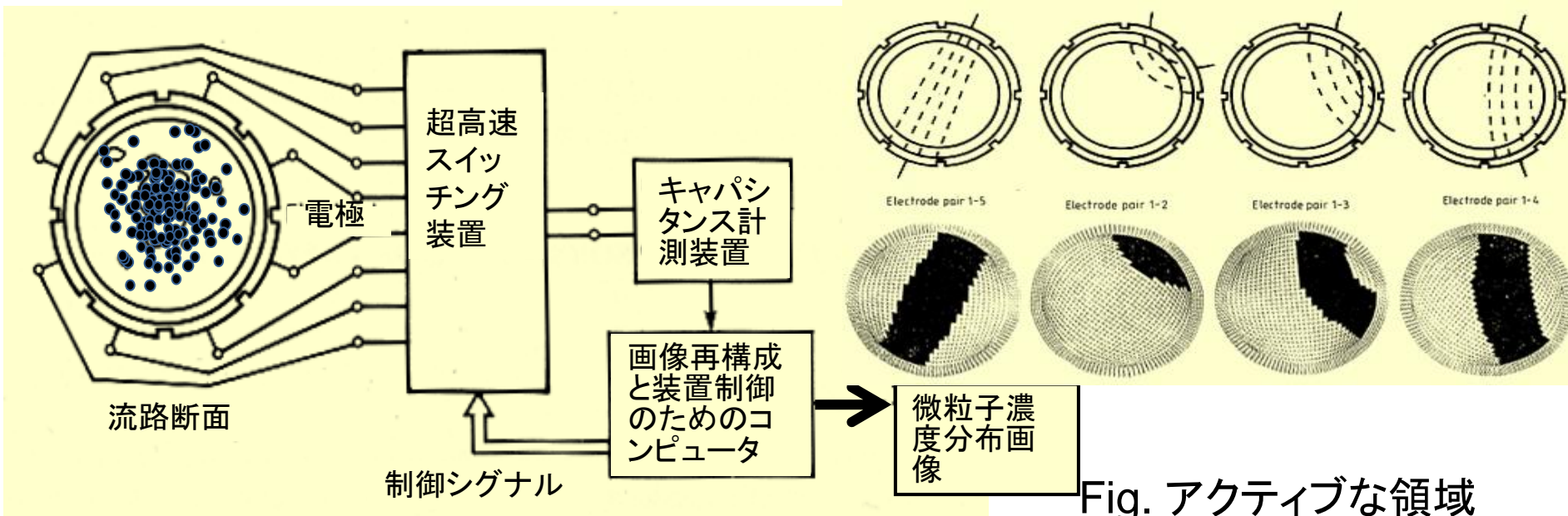
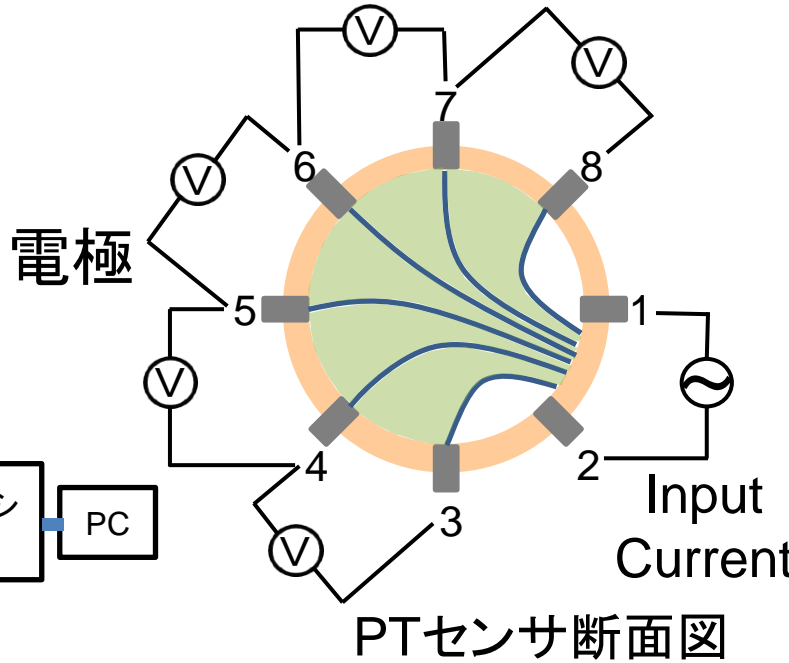
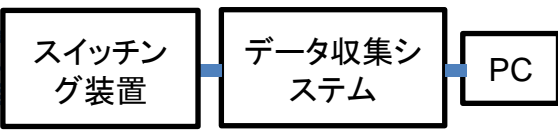
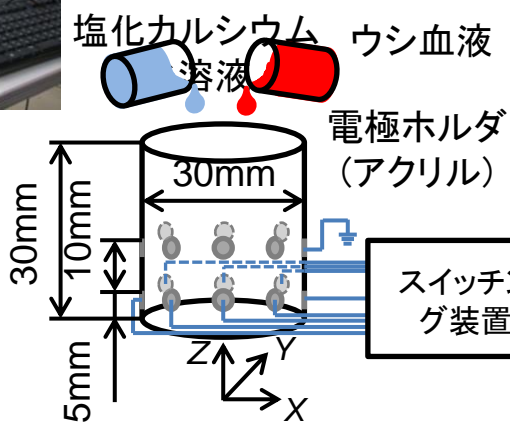
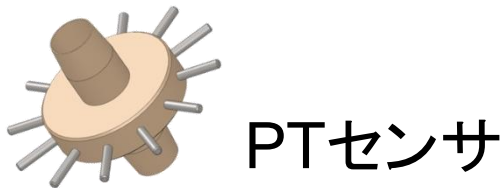
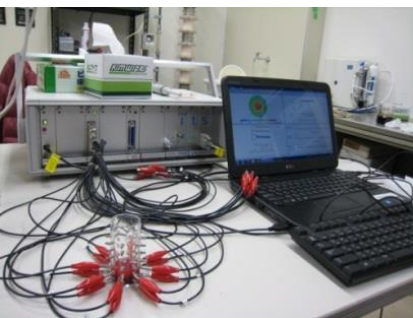


Fig. PT(ECT)法のシステム

Fig. アクティブな領域



ECTセンサ

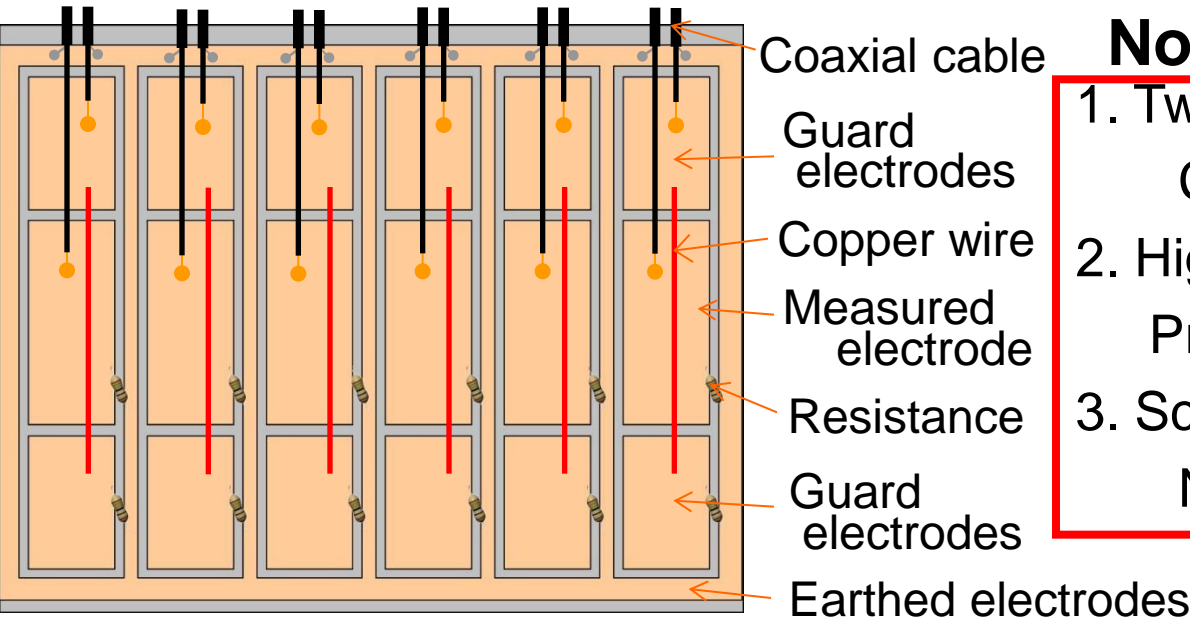


Fig. CT sensor

Noise protection method

1. Two guard electrodes
 Concentration of electrical line
2. High Ω Resistance
 Protection of stray capacitance
3. Screen electrodes
 Noise Absorption

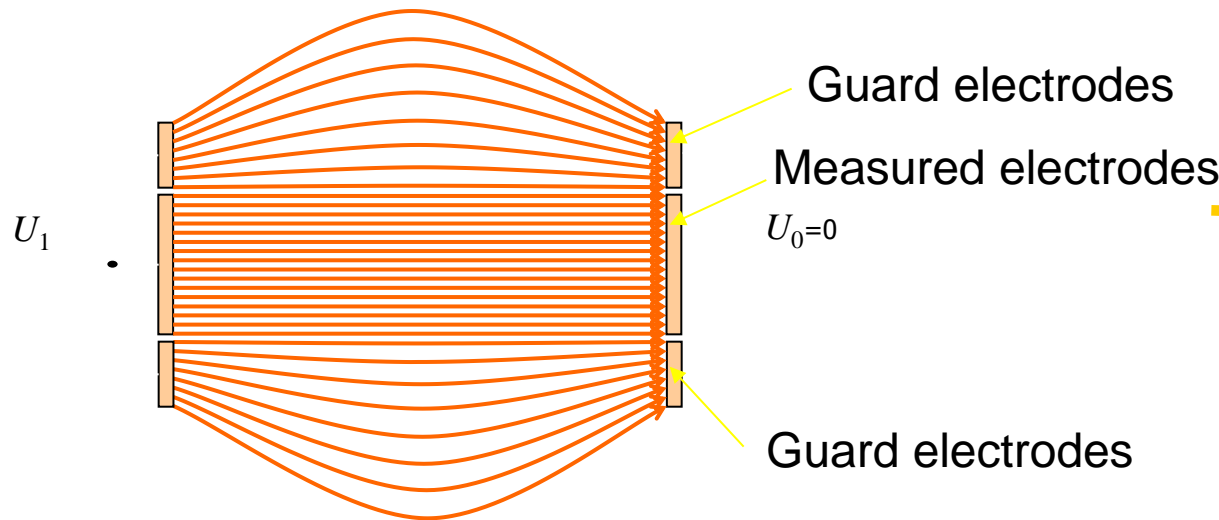


Fig. Guard electrodes

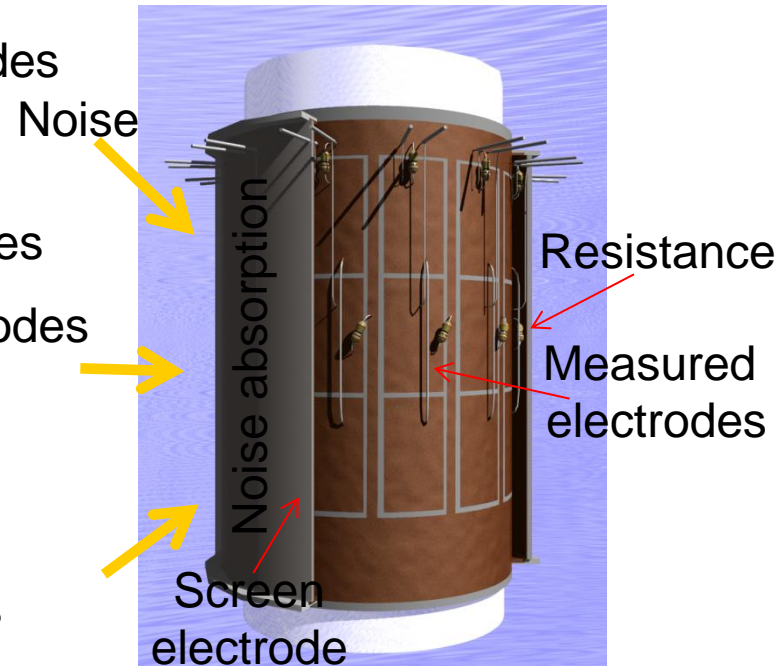


Fig. Screen electrode

ERT基礎式#1

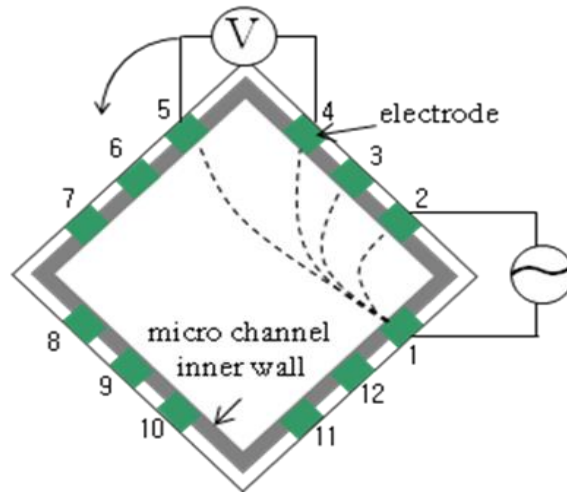


Fig. Neighboring method

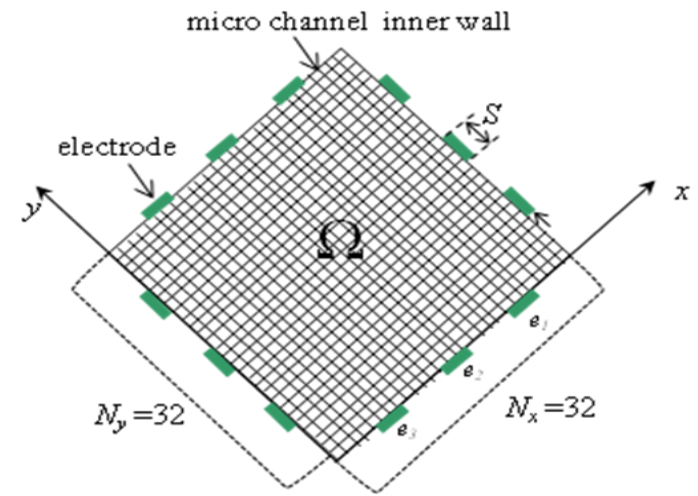


Fig. 空間解像度

$U(\rho)$: 電極上の電位 $\leftarrow U = J\rho \rightarrow \rho$: 抵抗率分布

未知数(空間解像度) < 式数

逆問題で求める

$$J = \begin{pmatrix} \frac{\partial U_1^1}{\partial \rho_1} & \dots & \frac{\partial U_1^1}{\partial \rho_N} \\ \frac{\partial U_2^1}{\partial \rho_1} & \dots & \frac{\partial U_2^1}{\partial \rho_N} \\ \vdots & \ddots & \vdots \\ \frac{\partial U_1^K}{\partial \rho_1} & \dots & \frac{\partial U_1^K}{\partial \rho_N} \\ \vdots & \ddots & \vdots \\ \frac{\partial U_L^K}{\partial \rho_1} & \dots & \frac{\partial U_L^K}{\partial \rho_N} \end{pmatrix}$$

J : ヤコビ行列(感度関数)
順問題で求める

N : 空間要素
 L : 電圧測定パターン
 K : 電流印加パターン

基礎式#2と境界条件

Laplace 方程式
$$\nabla \cdot \left(\frac{1}{\rho} \nabla u \right) = 0, \quad \text{on } x \in \Omega$$

j : 電流密度 [A/m²], ρ : 抵抗率 [$\Omega \cdot \text{m}$] u : 電位 [V]

境界条件

1) Summation of current density on electrodes is currency on electrodes:

$$\int_{e_l} \frac{1}{\rho} \frac{\partial u}{\partial \nu} dS = I_l, x \in e_l, l = 1, 2, \dots, L$$

2) Current is zero except for the current electrode pair:

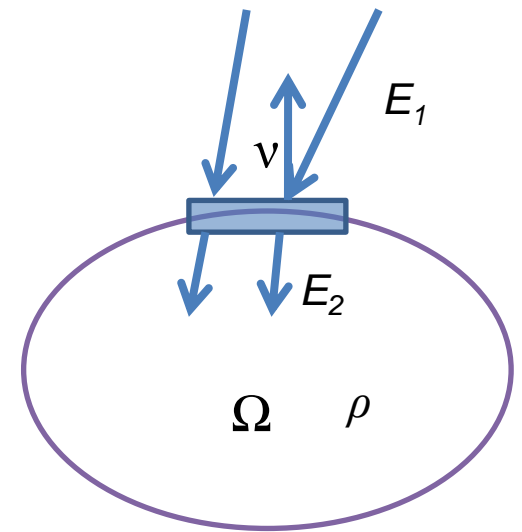
$$\frac{1}{\rho} \frac{\partial u}{\partial \nu} = 0, x \in \partial\Omega \setminus \bigcup_{l=1}^L e_l$$

3) Contact impedance is considered on the electrodes

$$u + z_l \frac{1}{\rho} \frac{\partial u}{\partial \nu} = U_l, x \in e_l, l = 1, 2, \dots, L$$

4) All current and voltage on all electrodes are zero

$$\sum_{l=1}^L I_l = 0, \sum_{l=1}^L U_l = 0$$



ρ : Resistivity distribution on Ω I : Current on electrodes u : Potential distribution on Ω
 U : Voltage on electrodes e_l : Surface on l th electrode ν : outward directed normal vector
 S : Electrode boundary L : electrode number z : Contact impedance

境界条件(complete electrode models)

1) Summation of current density on electrodes is current on electrodes:

$$\int_{e_l} \frac{1}{\rho} \frac{\partial u}{\partial \nu} dS = I_l, x \in e_l, l = 1, 2, \dots, L$$

2) Current is zero except for the current electrode pair:

$$\frac{1}{\rho} \frac{\partial u}{\partial \nu} = 0, x \in \partial\Omega \setminus \bigcup_{l=1}^L e_l$$

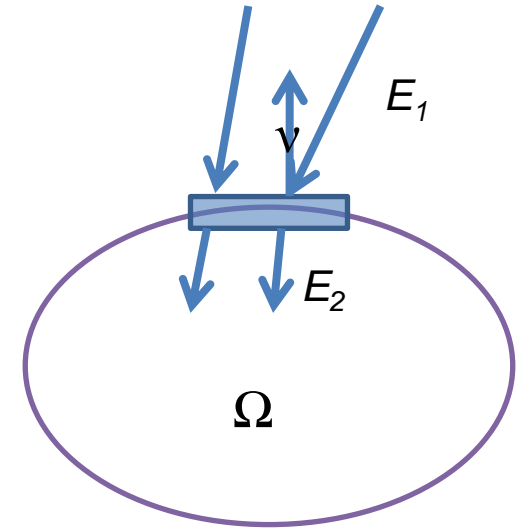
3) Contact impedance is considered on the electrodes

$$u + z_l \frac{1}{\rho} \frac{\partial u}{\partial \nu} = U_l, x \in e_l, l = 1, 2, \dots, L$$

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ρ : Resistivity distribution on Ω I : Current on electrodes u : Potential distribution on Ω U : Voltage on electrodes e_l : Surface on l th electrode ν : outward directed normal vector S : Electrode boundary
 L : electrode number z : Contact impedance



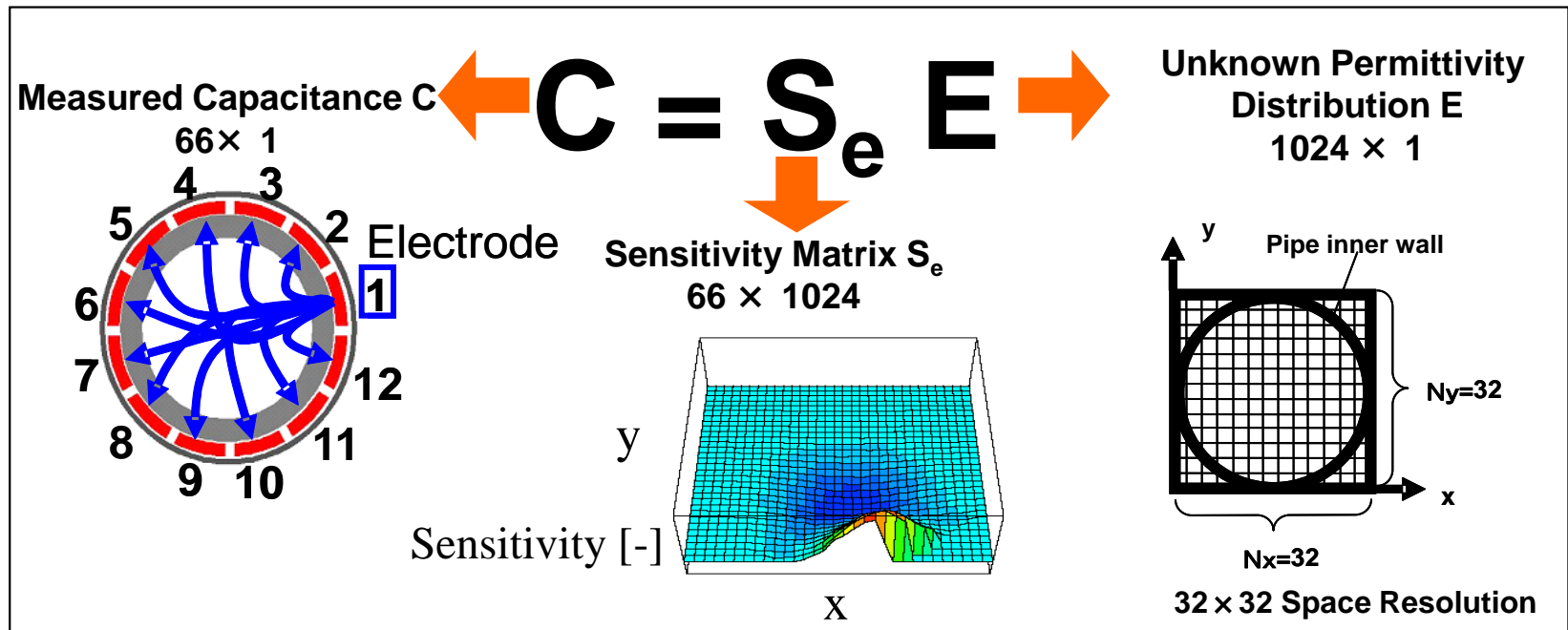
ECTの基礎式

Governing Equation in the Electrostatic Field

$$C_{i,j} = -\frac{\epsilon_0}{V_c} \oint_{r \in \Gamma_j} \epsilon(\mathbf{r}) \nabla V_i(\mathbf{r}) \cdot d\mathbf{r} \quad \nabla \cdot [\epsilon(\mathbf{r}) \nabla V(\mathbf{r})] = 0$$

($i=1,2,\dots,11; j=i+1,\dots,12$)

$C_{i,j}$: Capacitance between i and j electrodes, ϵ_0 : Vacuum permittivity, V_c : Electrode voltage, \mathbf{r} : Position vector, ϵ : Relative permittivity, V_i : Potential in cross section, Γ_j : Area covered with electric force line



Ill posed Inverse Problem

Unknown Number > Expression Number



Image Reconstruction

Approximate Permittivity E

通常の逆問題の解法

Linear Back Projection (LBP) Method

Blurred Image

Landweber (LW) method

Necessary Artificial Gain Value

$$\mathbf{E}^{(0)} = \mathbf{S}_e^T \mathbf{C}^{(0)}$$

$$\mathbf{C}^{(1)} = \mathbf{S}_e \mathbf{E}^{(0)}$$



$$\Delta \mathbf{C}^{(1)} = (\mathbf{C}^{(1)} - \mathbf{C}^{(0)})$$

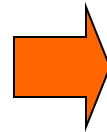
$$\Delta \mathbf{C}_g^{(1)} = g \times \Delta \mathbf{C}^{(1)}$$



$$\Delta \mathbf{E}^{(1)} = \mathbf{S}_e^T \Delta \mathbf{C}_g^{(1)}$$



$$\mathbf{E}^{(1)} = (\mathbf{E}^{(0)} - \Delta \mathbf{E}^{(1)})$$



$$\begin{aligned} \mathbf{E}^{(k)} &= \mathbf{E}^{(k-1)} + \Delta \mathbf{E}^{(k-1)} \\ &= \mathbf{S}_e^T \mathbf{C}^{(0)} + g \left(\mathbf{I}_m - \mathbf{S}_e^T \mathbf{S}_e \right) \mathbf{E}^{(k-1)} \end{aligned}$$

Iterative Tikhonov Regularization (ITR) method

$$\mathbf{E}^{*(k)} = \mathbf{E}^{*(k-1)} - \left(\mathbf{S}_e^T \mathbf{S}_e + \gamma \right)^{-1} \mathbf{S}_e^T \left(\mathbf{S}_e^T \mathbf{E}^{*(k-1)} - \mathbf{C}^{*(0)} \right)$$

CHARACTERISTICS OF GVSPM METHOD

Takei, M. et. al 2004 & 2006 *Meas. Sci. & Technol.*

Normalization by Norm

$$C = S_e E = \sum_{i=1}^m (S_{e_i} e_i) \quad \begin{array}{l} \text{Space resolution} \\ m=1024 \end{array}$$

Normalization

$$C' = \frac{C}{|C|} \quad S_{e_i}' = \frac{S_{e_i}}{|S_{e_i}|} \quad e_i' = e_i \frac{|S_{e_i}|}{|C|}$$

$$|C| = \sqrt{c_1^2 + c_2^2 + \dots + c_n^2}$$

$$|S_{e_i}| = \sqrt{S_{ei_1}^2 + S_{ei_2}^2 + \dots + S_{ei_n}^2}$$

Total pair number of electrodes $n=66$

$$C' = \sum_{i=1}^m (S_{e_i}' e_i') = S_e' E'$$

Accurate Images

Evaluation Function

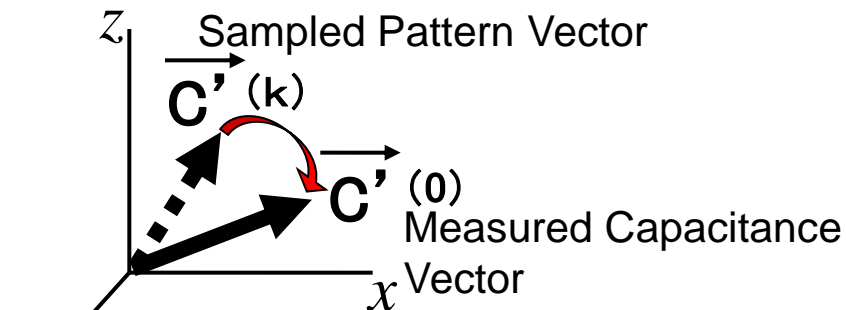


Fig. Iteration process in the case of $n=3$

$$f(E'^{(k)}) = C'^{(0)} C'^{(k)} \rightarrow 1.0$$

$E'^{(k)}$: k^{th} iterative solution of SPM

$C'^{(k)}$: Capacitance from $E'^{(k)}$

$C'^{(0)}$: Measured capacitance

Iterative Solution

No Artificial Gain Value

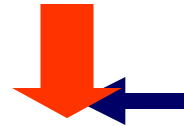
INCLUSION OF EVALUATION FUNCTION IN ITERATIVE SOLUTION

Evaluation Function

$$f(E'^{(k)}) = C'^{(0)} C'^{(k)} \rightarrow 1.0$$

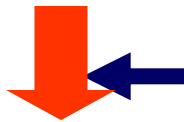


$$1 - f(E'^{(k)}) = 1 - C'^{(0)} \frac{S_e' E'^{(k-1)}}{|S_e' E'^{(k-1)}|} \rightarrow 0$$



Multiply $C'^{(0)}$

$$C'^{(0)} - C'^{(0)} C'^{(0)} \frac{S_e' E'^{(k-1)}}{|S_e' E'^{(k-1)}|} \rightarrow 0$$

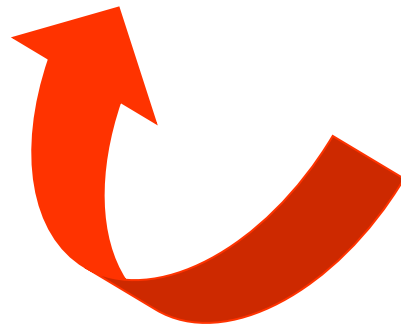


$$C'^{(0)} C'^{(0)} = 1.0$$

$$C'^{(0)} - \frac{S_e' E'^{(k-1)}}{|S_e' E'^{(k-1)}|} \rightarrow 0$$

General Iterative Solution of GVSPM

$$E'^{(k)} = E'^{(k-1)} + S_e' T \left(C'^{(0)} - \frac{S_e' E'^{(k-1)}}{|S_e' E'^{(k-1)}|} \right)$$



RECONSTRUCTION OF PSEUDO IMAGES

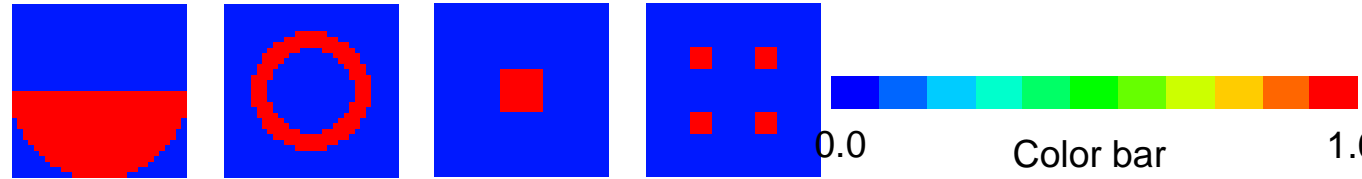
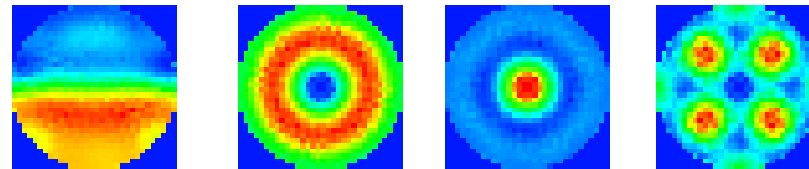
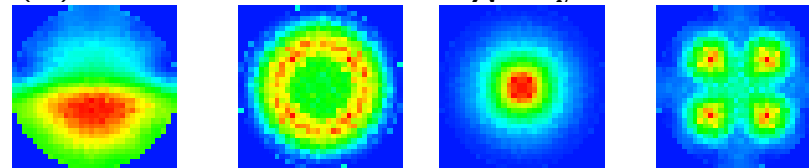


Fig. Pseudo particle images



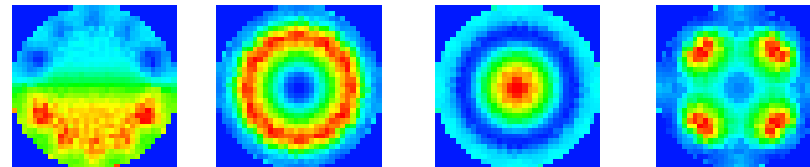
(a-1)Bottom(a-2)Annular(a-3)Center(a-4)Four-bulk

(a) Reconstructed image by Landweber



(b-1)Bottom(b-2)Annular(b-3)Center(b-4)Four-bulk

(b) Reconstructed image by Iterative Tikhonov

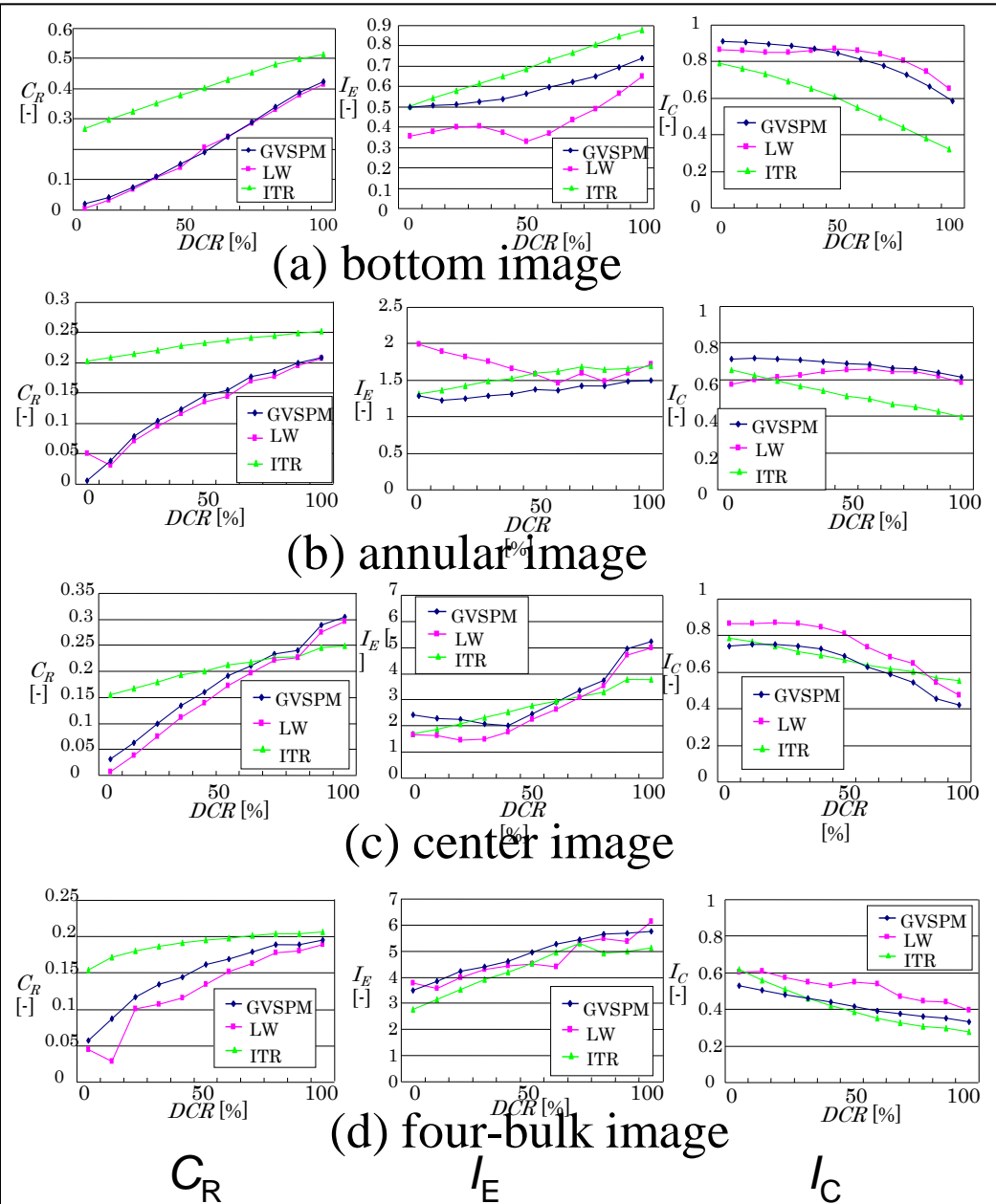


(c-1)Bottom(c-2)Annular(c-3)Center(c-4)Four-bulk

(c) Reconstructed image by GVSPM

Fig. Reconstructed images of pseudo particle images

EVALUATION OF RECONSTRUCTION



Evaluation Method
Residual Capacitance C_R

$$C_R = \frac{\sqrt{\sum_{i=1}^n (c_i^{(k)} - c_i^{(0)})^2}}{\sqrt{(\mathbf{C}^{(0)})^2}}$$

Image Error I_E

$$I_E = \frac{\sqrt{\sum_{i=1}^m (e_i^{(k)} - e_i^{original})^2}}{\sqrt{(\mathbf{E}^{original})^2}}$$

Image Correlation I_C

$$I_C = \frac{\sum_{i=1}^m \left[(e_i^{(k)} - \overline{\mathbf{E}^{(k)}}) (e_i^{original} - \overline{\mathbf{E}^{original}}) \right]}{\sum_{i=1}^m \sqrt{(e_i^{(k)} - \overline{\mathbf{E}^{(k)}})^2} \sum_{i=1}^m \sqrt{(e_i^{original} - \overline{\mathbf{E}^{original}})^2}}$$

High accuracy reconstructed images
low C_R low I_E high I_C

CORRELATION OF CAPACITANCE

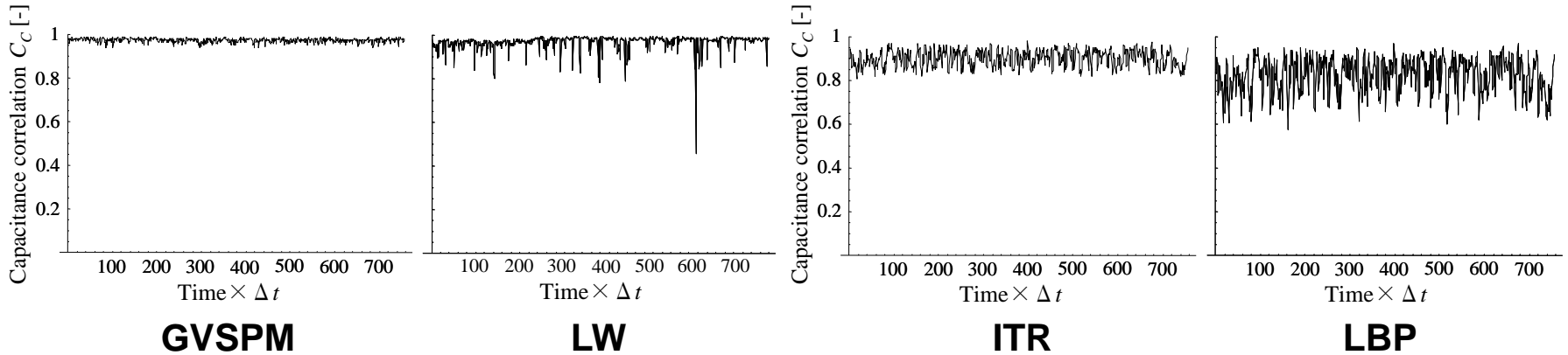
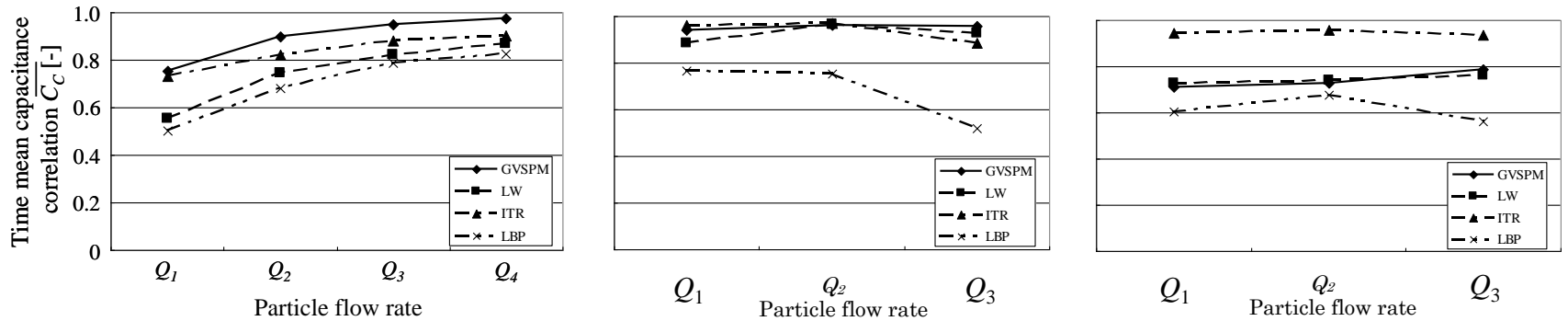


Fig. Correlation of capacitance for polyethylene pellet (Particle flow rate: Q_4)



(a) Polyethylene Pellet (PP)



(b) Silica Particle (SP)



(c) Polyvinyl Chloride (PVC)

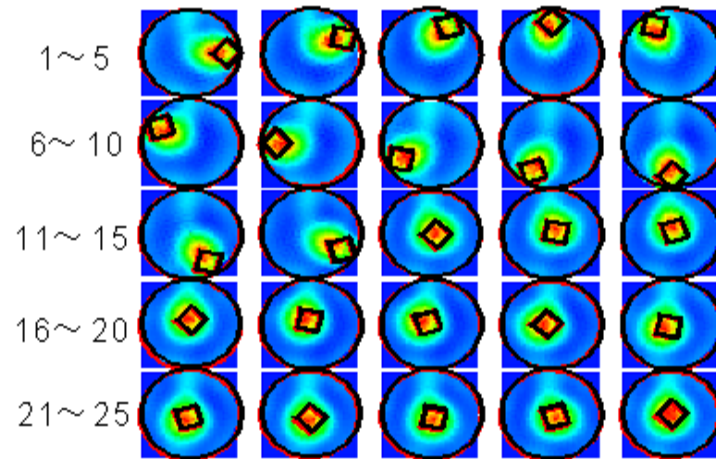
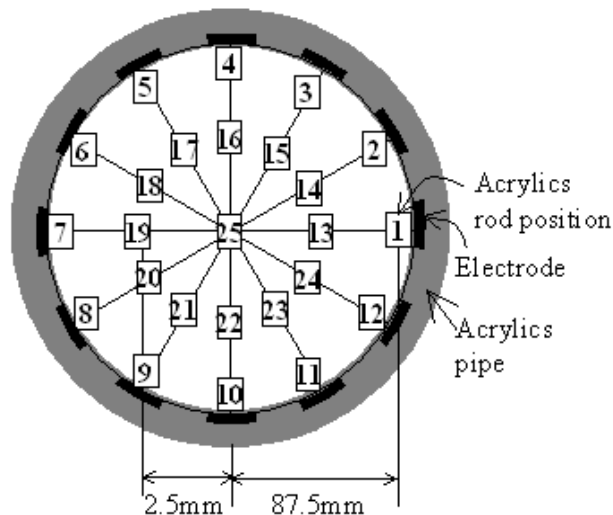


Fig. Time mean correlation of capacitance

STATIC ACCURACY TEST

M.Takei et al., *Powder Technology, Elsevier, (2004)*

Test Rod: Acrylic rod 500mm (L) × 60mm (W) × 60mm (H)
Permittivity : 2.8
Experiment: PTL300E Electrical capacitance tomography system
Process Tomography Ltd.
Input voltage: 15V (1.25 MHz)



(a) Positions of test rod

(b) Reconstructed images by LBP

Fig. Static accuracy of CT sensor

CONTENTS

- PTの概要 ソフトフィールドとハードフィールド
 - ソフトフィールドPT
 - 電気PTの原理
 - プラントへの展開
 - 血流への展開
 - マイクロ流路への展開
 - ハードフィールドPT
 - Optical CT
 - X ray CT
 - γ ray CT
 - Neutron Radiography
 - Ultrasound CT
 - MRI
 - Positron Emission Tomography (PET)
 - まとめ
- ①ECTの例 ②ERTの例
③温度分布計測の例

Circulating Fluidized Bed (Downer)

High demand of sulfur free & high-octane gasoline

FCC (fluid catalytic cracking) gasoline

Residual oil + FCC catalysts in CFB
(Circulating Fluidized Bed)



Key factor of high quality
Uniform concentration of FCC powder
in CFB



Nondestructive visualization technique in pipe cross section



Fig. FCC catalysts

1-2 μm zeolites dispersed on an
amorphous silica-alumina
forming 60 μm powders

Comparison with Previous Study

H. Zhang et al., *Chemical Engineering Science*, 1999

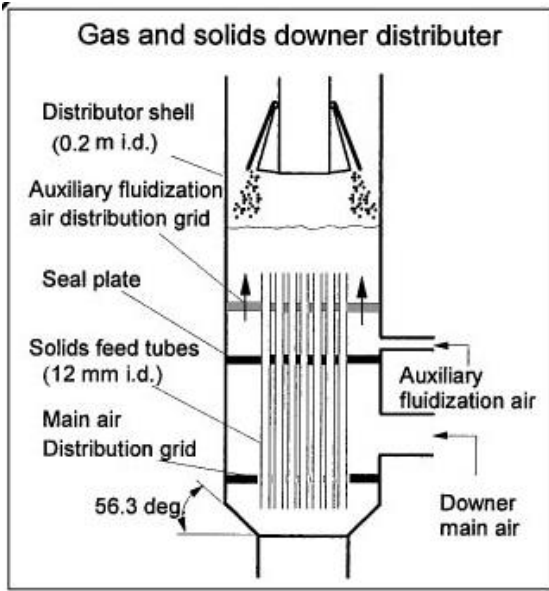
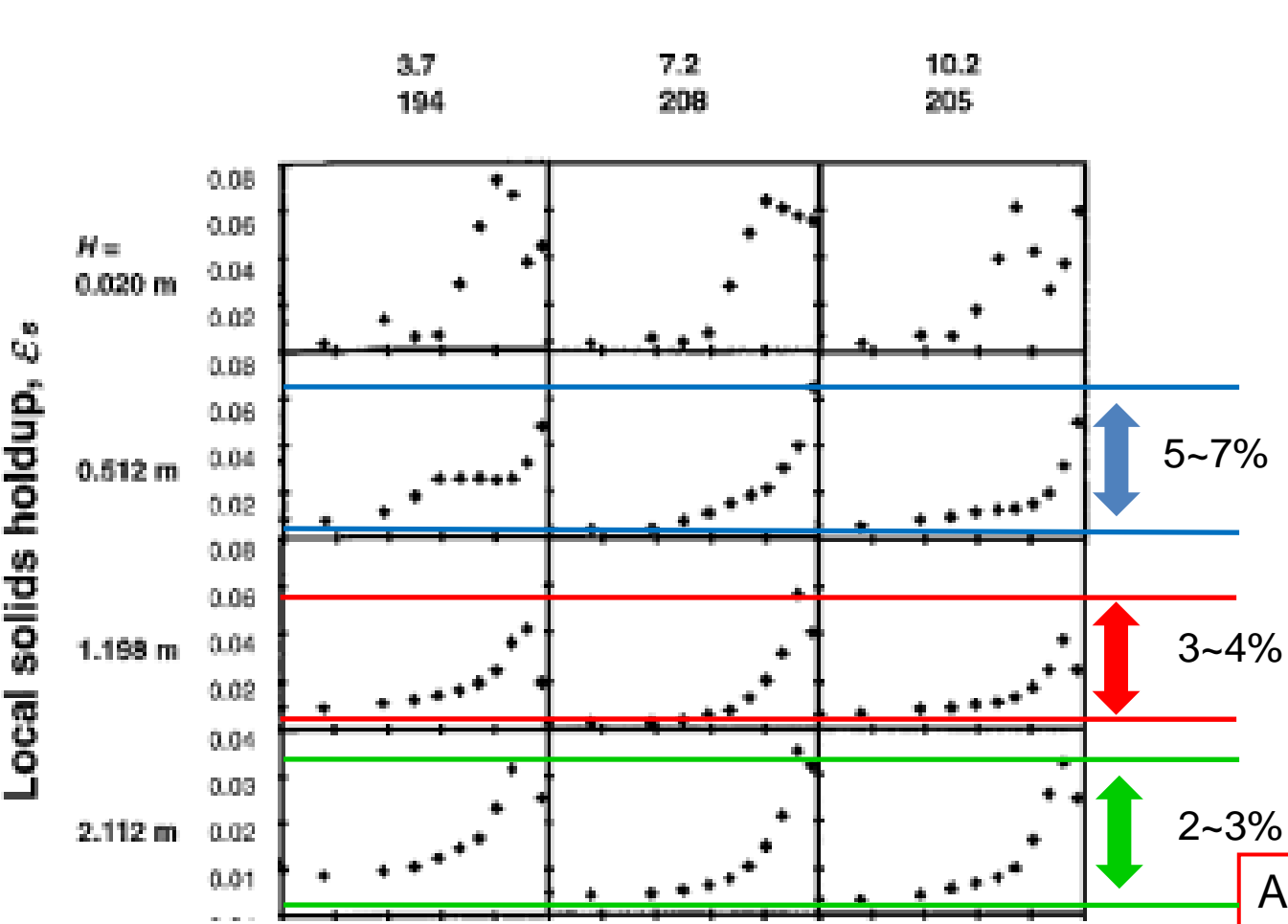


Fig. Radial solids holdup profiles along the downer

A non-uniform distribution is clearly seen near the entrance of the CFB in conventional distributor.

Experimental Setup

Pipe I.D:	270mm
Total Height:	5.3m
Sensor length :	660mm
Particle:	MFI-type zeolite
Particle Density:	1200 [kg/m ³]
Particle diameter:	69.6 μm
Sampling time:	10ms/one frame

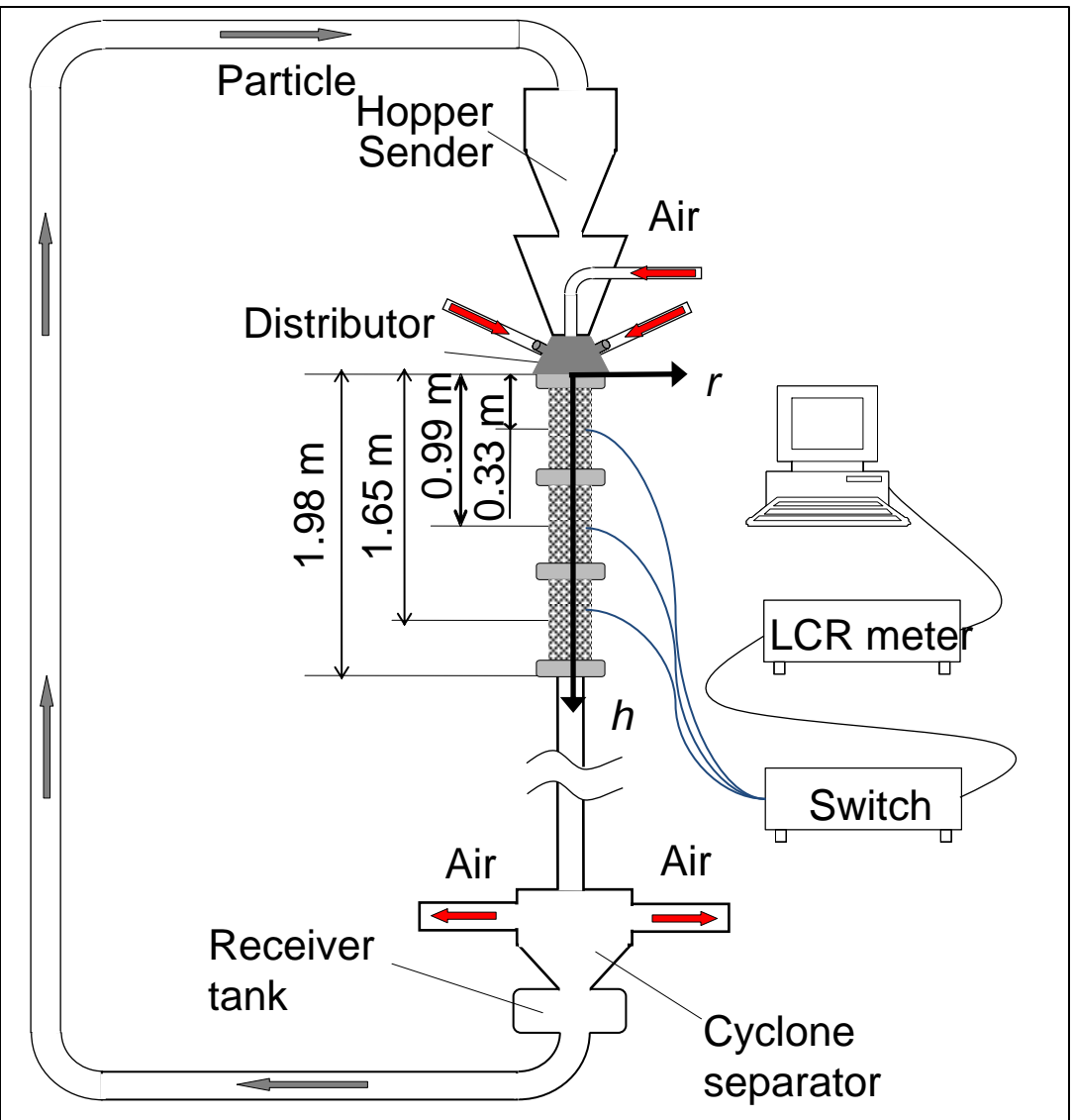


Fig. Experimental Setup

PT(ECT)による循環流動層濃度分布可視化計測

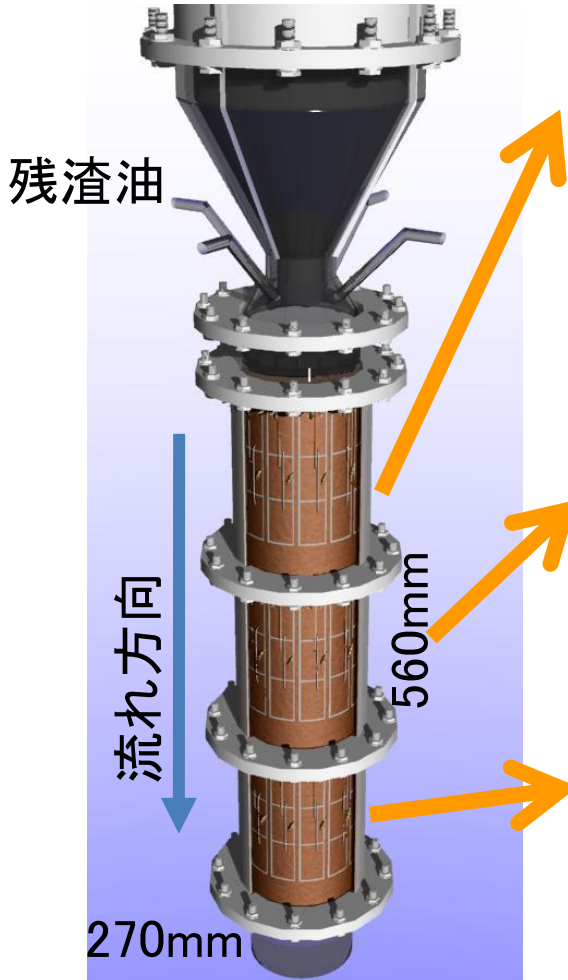
M.Takei et al. *Powder Technology* (2009)
 M.Takei, et al., *Experiments in Fluids*, Springer, (2008)



Fig. FCC 循環流動層テストプラント

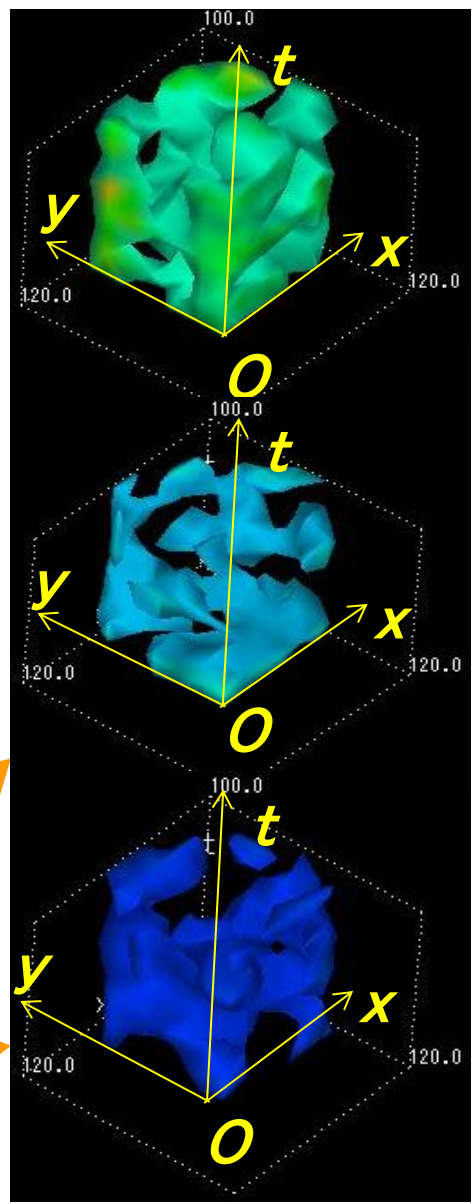


FCC 触媒粒子



270mm

大口径のPTセンサ

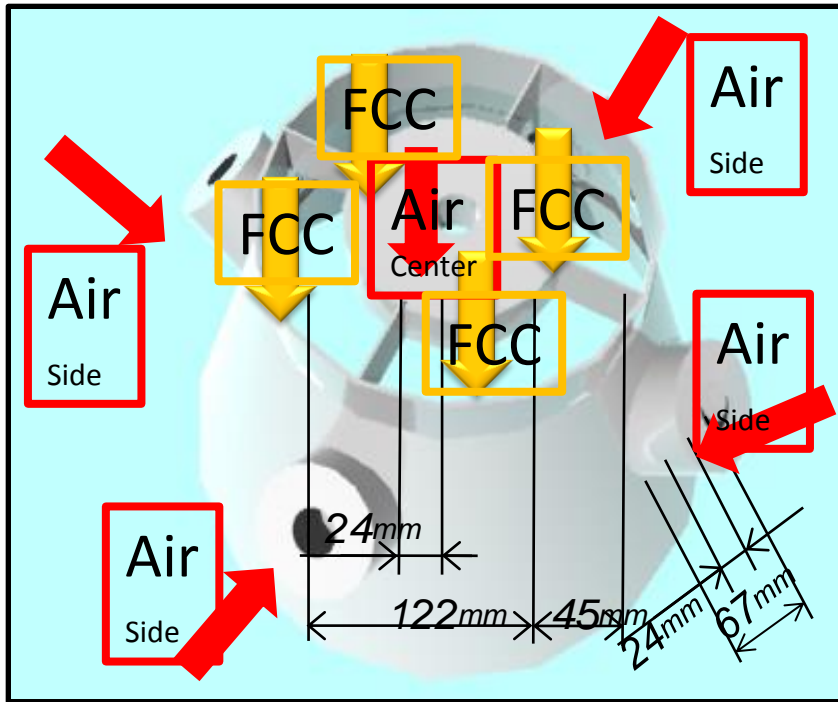


高
濃度
低
濃度
粒子濃度分布

粒子の3D拡散現象

New Designed Distributor & Experimental Conditions

T.Zhao, M.Takei, *Flow Measurement and Instrumentation*, 2007
 Tong Zhao, Masahiro Takei, et al., *Powder Technology*, (2011)



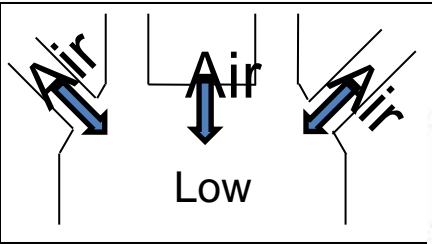
Center : Side = 1:4
 (Ratio of Air flow rate)

Fig. New designed distributor

Table Experimental condition

		Case 1.1	Case 1.2	Case 1.3	Case 1.4
Powder circulation rate (particle flow rate) G_s [kg/m ² s]		175	233	292	349
Center: Side 1:4	Air flow rate of center nozzle Q_{ac} [m ³ /s]	0.094			
	Total air flow rate of side nozzle Q_{as} [m ³ /s]	0.378			

Time Mean Reconstructed Images (Centre : Side =1:4)



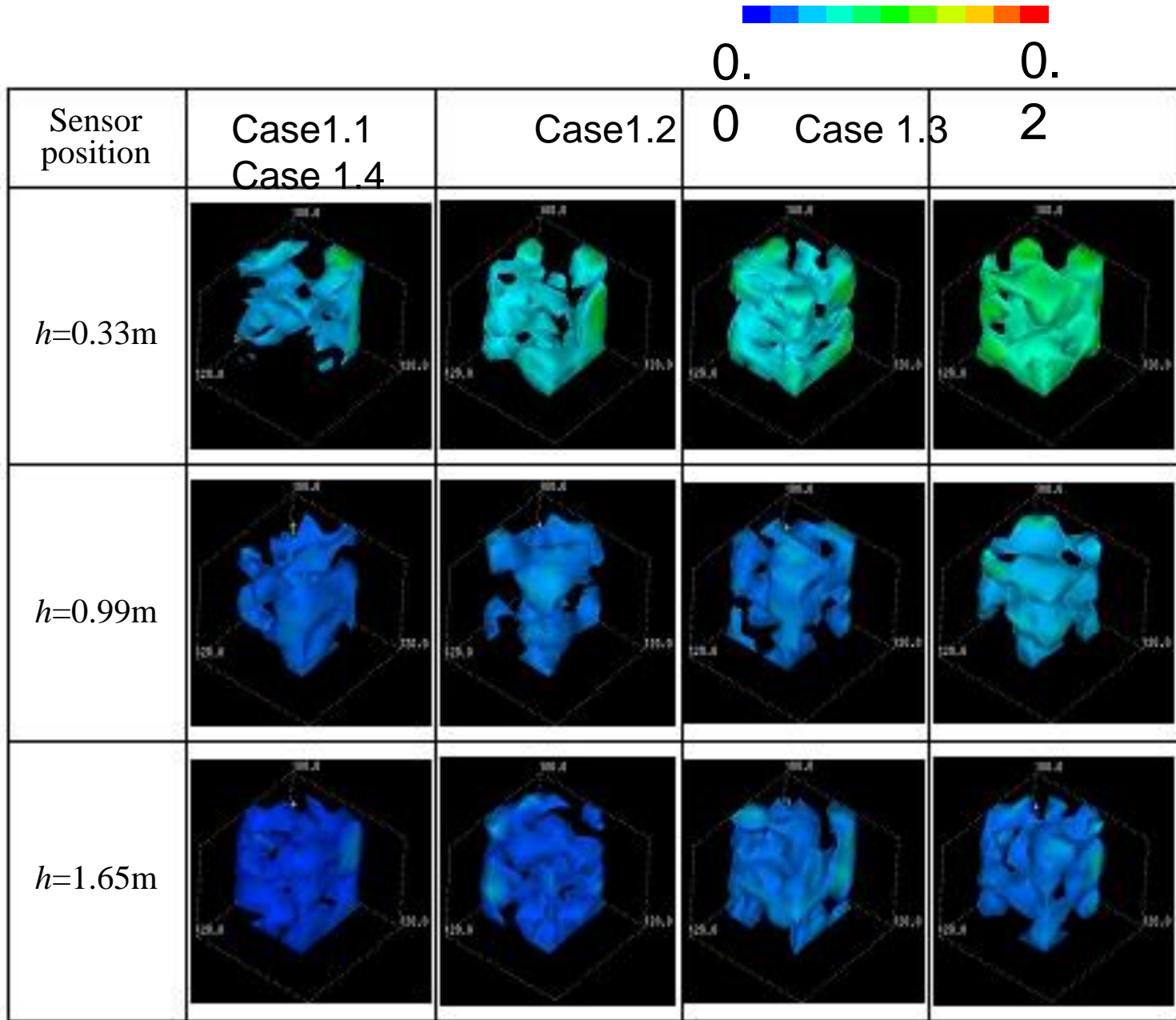
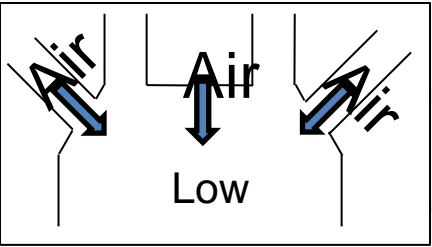
0.0

0.2

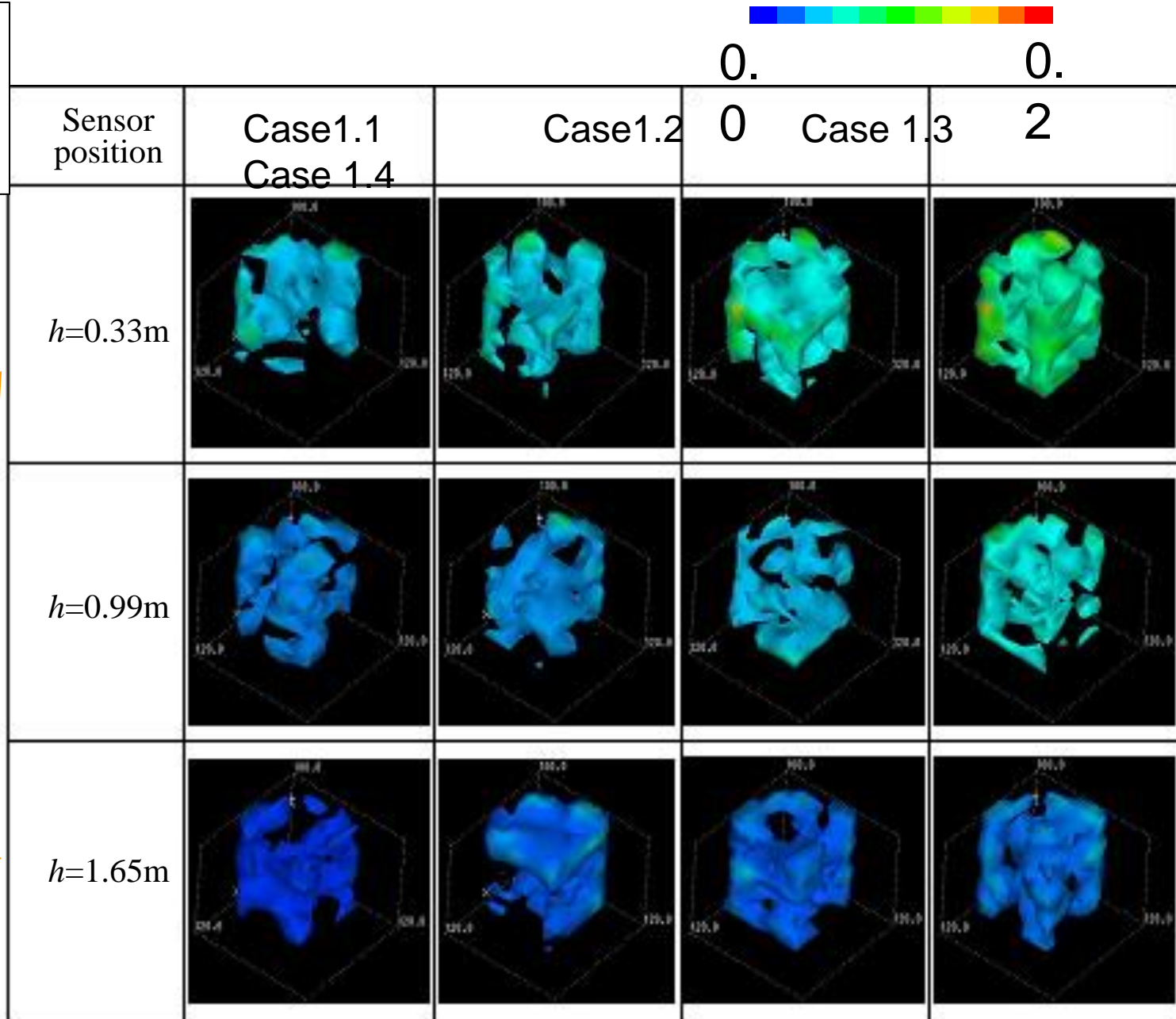
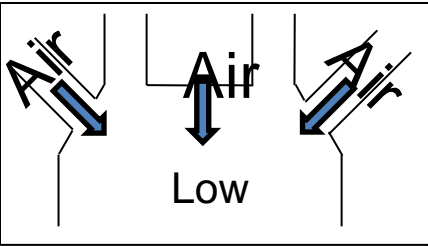


Sensor position	Case1.1	Case1.2	Case 1.3	Case 1.4
$h=0.33\text{m}$				
$h=0.99\text{m}$				
$h=1.65\text{m}$				

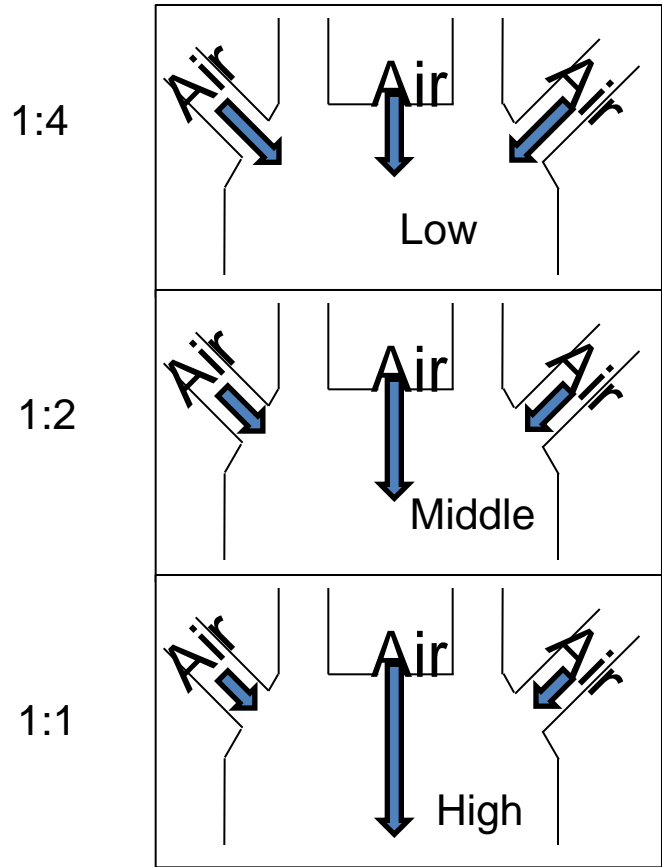
Time Mean Reconstructed Images (Centre : Side =1:2)



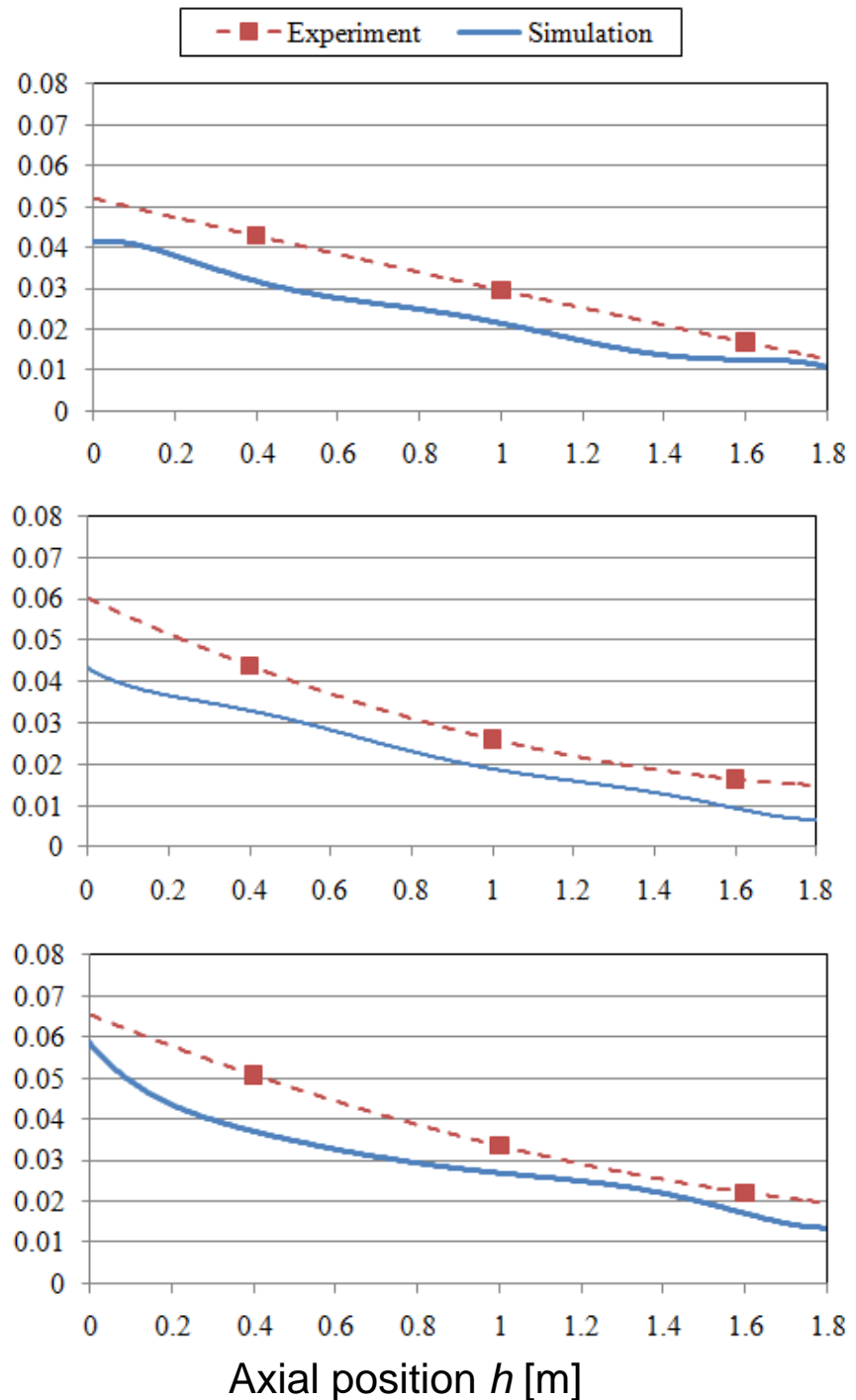
Time Mean Reconstructed Images (Centre : Side =1:1)



Axial Volume Fraction Profiles

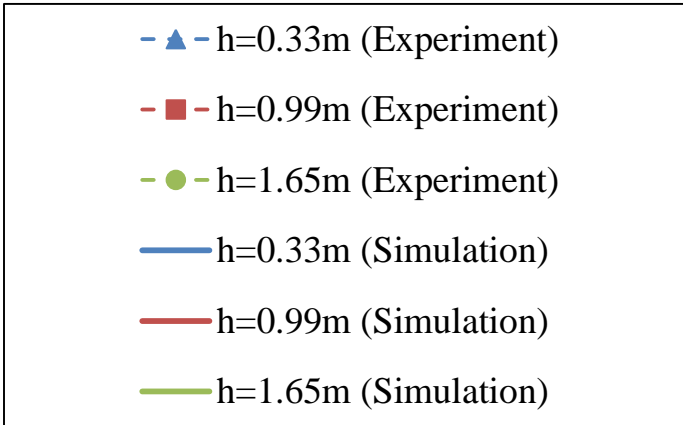
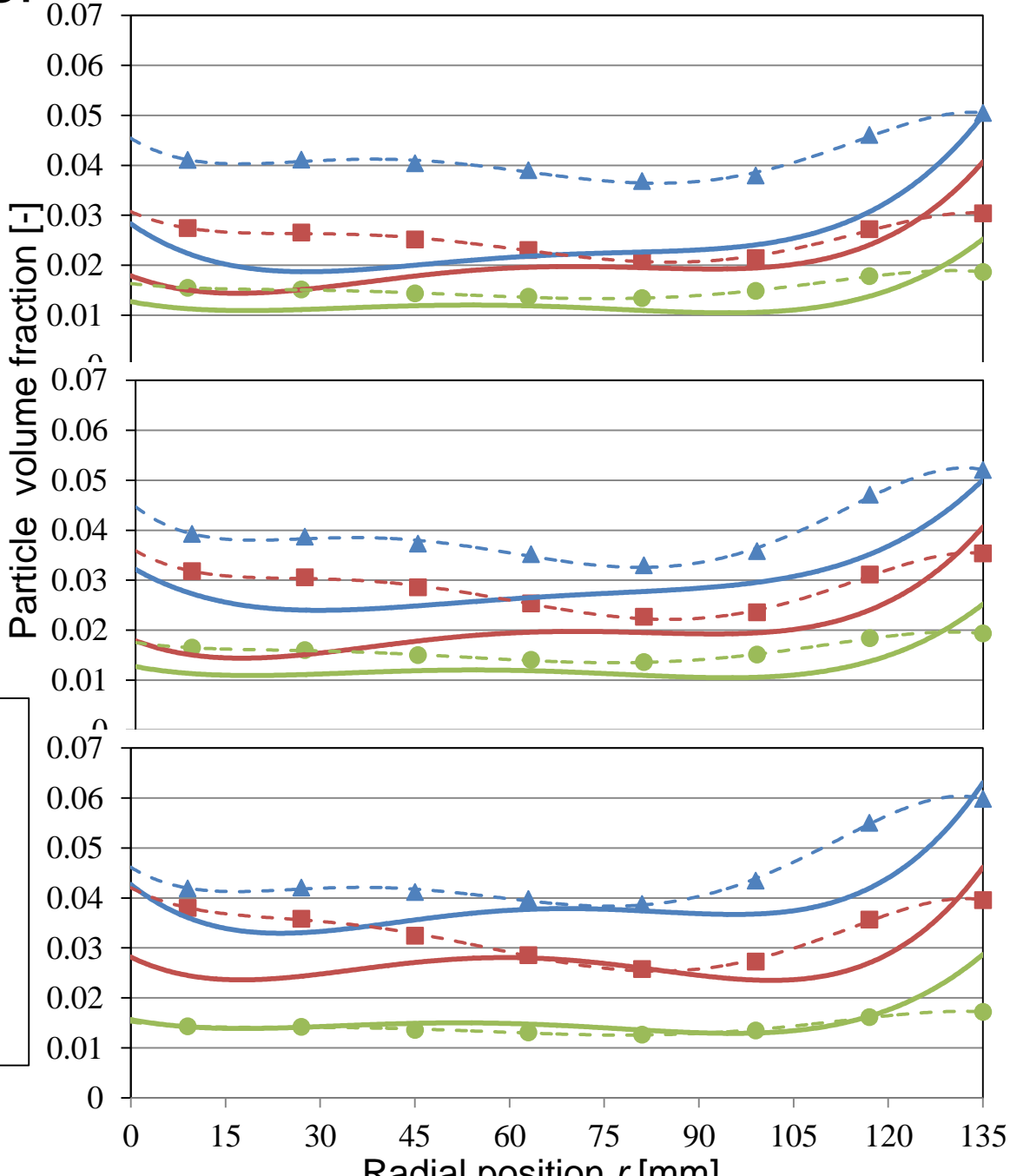
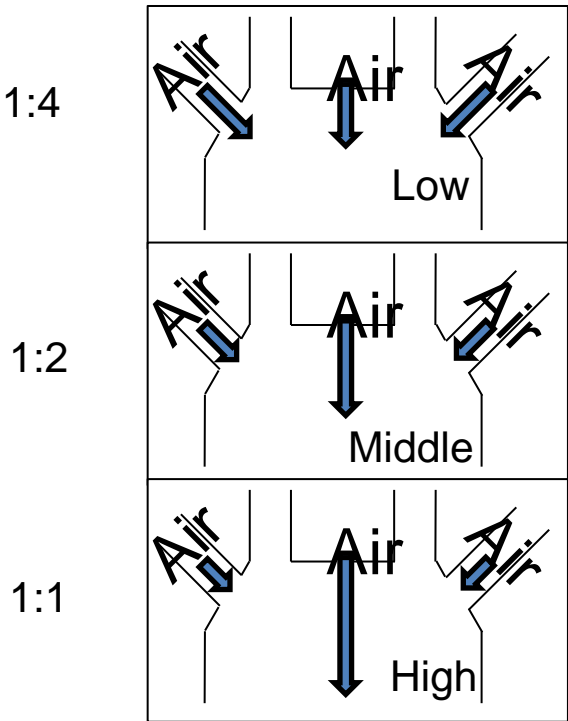


Particle volume fraction [-]

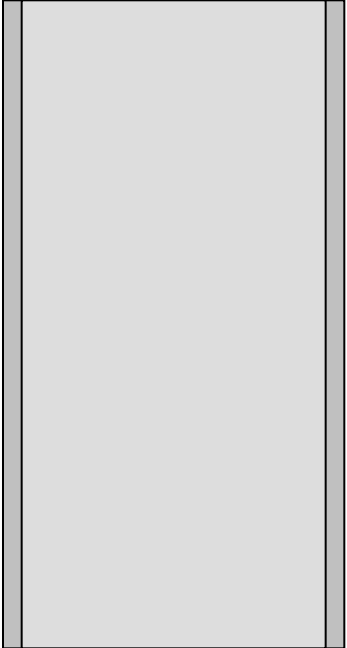
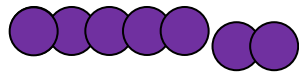


Particle volume fraction decreased as axial position goes downstream in both experiment and simulation.

Radial Volume Fraction Profiles



Discussion to Axial Profiles



First acceleration section ($V_p < V_a$)

Second acceleration Section ($V_p > V_a$)

Constant velocity section ($V_p = \text{constant}$)

$$Q_p = A \times V_p \times \alpha$$

$$Q_a = A \times V_a \times (1 - \alpha)$$

$$\frac{Q_p}{Q_p + Q_a} = \frac{\alpha \beta}{\alpha \beta + (1 - \alpha)} \quad \left(\beta = \frac{V_p}{V_a} \right)$$

Particle volume fraction

$$\alpha = \frac{Q_p}{Q_p + \beta Q_a}$$

α is inversely proportional to β .

Z. Wang et al. (1992)

- A : Sectional area of pipe
- Q_p : Particle flow rate
- Q_a : Air flow rate
- α : Particle volume fraction
- V_p : Particle velocity
- V_a : Air velocity
- β : Slip velocity

Governing Equations & Fluid Drag Force

Solid phase (Discrete phase)

$$m \frac{dv}{dt} = F_a + F_c + G$$

$$I \frac{d\omega}{dt} = T$$

Gas phase (Continuum phase)

$$\frac{\partial \varepsilon}{\partial t} + \nabla \cdot (\varepsilon \mathbf{u}) = 0$$

$$\frac{\partial (\rho_g \varepsilon_g \mathbf{u})}{\partial t} + \nabla \cdot (\rho_g \varepsilon_g \mathbf{u} \mathbf{u}) = -\varepsilon_g \nabla p + f_{a,i} + \varepsilon_g (\mu + \mu_e) \nabla^2 \mathbf{u}$$

Drag force

$$f_{a,i} = \frac{\beta}{\rho_g} (v_{pi} - u_i), \quad \text{Re} = \frac{|\vec{v}_p - \vec{u}| \rho_g d_p}{\mu}, \quad \beta = \begin{cases} \frac{\mu(1-\varepsilon)}{d_p^2 \varepsilon} [150(1-\varepsilon) + 1.75 R_e] & (\varepsilon \leq 0.8) \\ \frac{3}{4} C_D \frac{\mu(1-\varepsilon)}{d_p^2} \varepsilon^{-2.7} R_e & (\varepsilon > 0.8) \end{cases}$$

Ergun's equation, 1952

$$C_D = \begin{cases} \frac{24(1+0.15 \text{Re}^{0.687})}{\text{Re}} & (\text{Re} \leq 1000) \\ 0.43 & (\text{Re} > 1000) \end{cases}$$

Wen and Yu's equation, 1966

m : Mass of the particle, v : Translational velocity, ω : Rotational velocity, P : Pressure, I : Moment of inertia, F_a : Force acting on particle exerted by surrounding air, F_c : Contact force, G : Gravitational force, u : Velocity vector of air, T : Torque caused by the contact force and the moment of inertia of particle, ε : Volume fraction, ρ_g : Density of air, μ : Fluid viscosity, μ_e : Eddy viscosity, C_D : Drag coefficient for a single particle, d_p : Particle diameter, v_p : Particle velocity

Contact Force

Normal contact force

$$F_{cn} = k_n \Delta x_n - \eta_n \frac{dx_n}{dt}$$

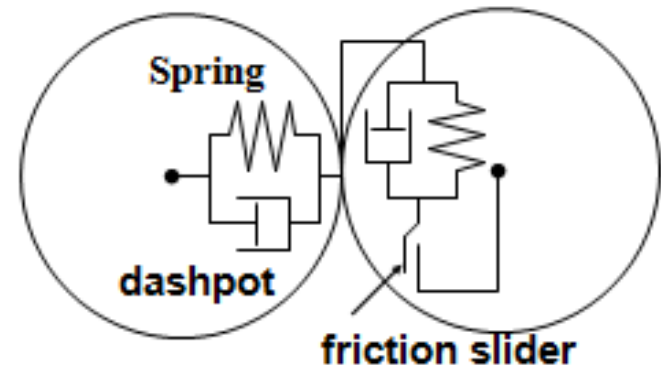


Fig. Models of contact force

Cundall and Strack 1979

$$F_{ct} = k_t \Delta x_t - \eta_t \frac{dx_t}{dt} \quad \text{if} \quad |F_{ct}| \leq \mu_f |F_{cn}|$$

$$F_{ct} = \mu_f |F_{cn}| \frac{x_t}{|x_t|} \quad \text{if} \quad |F_{ct}| > \mu_f |F_{cn}|$$

k_n & k_t : Stiffness of the springs in the normal and tangential direction

η_n & η_t : Coefficient of viscous dissipation in the normal and tangential direction

x_n & x_t : Particle displacement in the normal and tangential direction

μ_f : Friction coefficient.

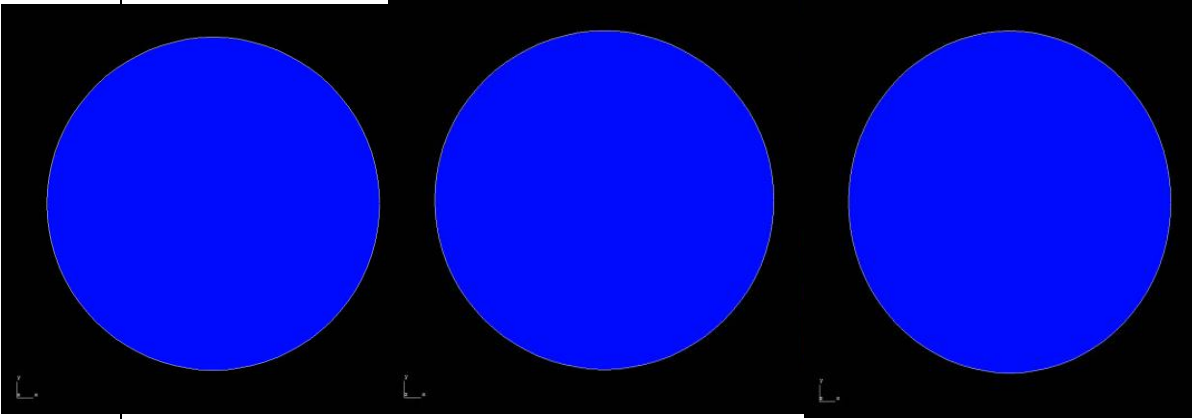
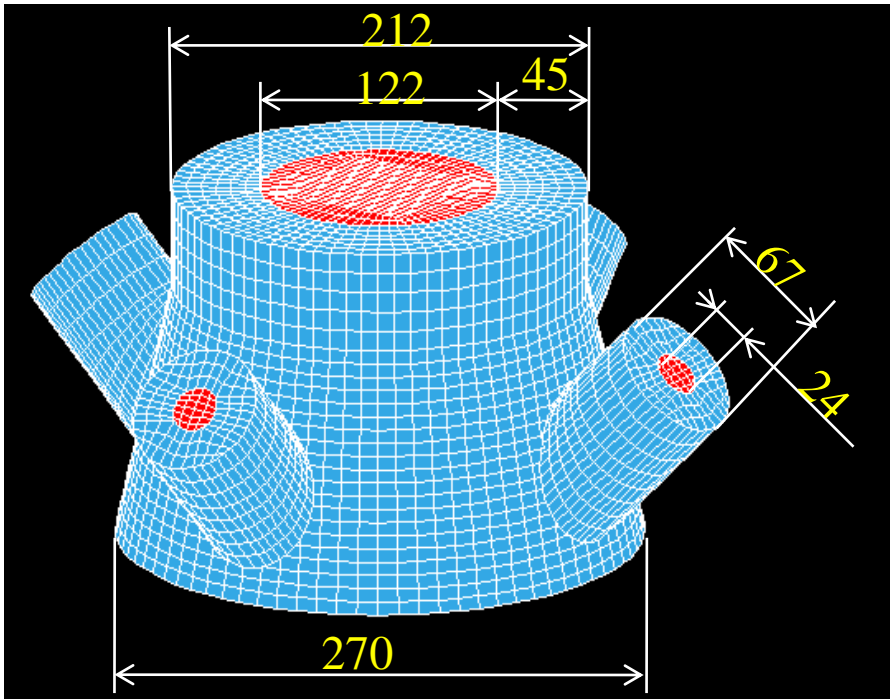
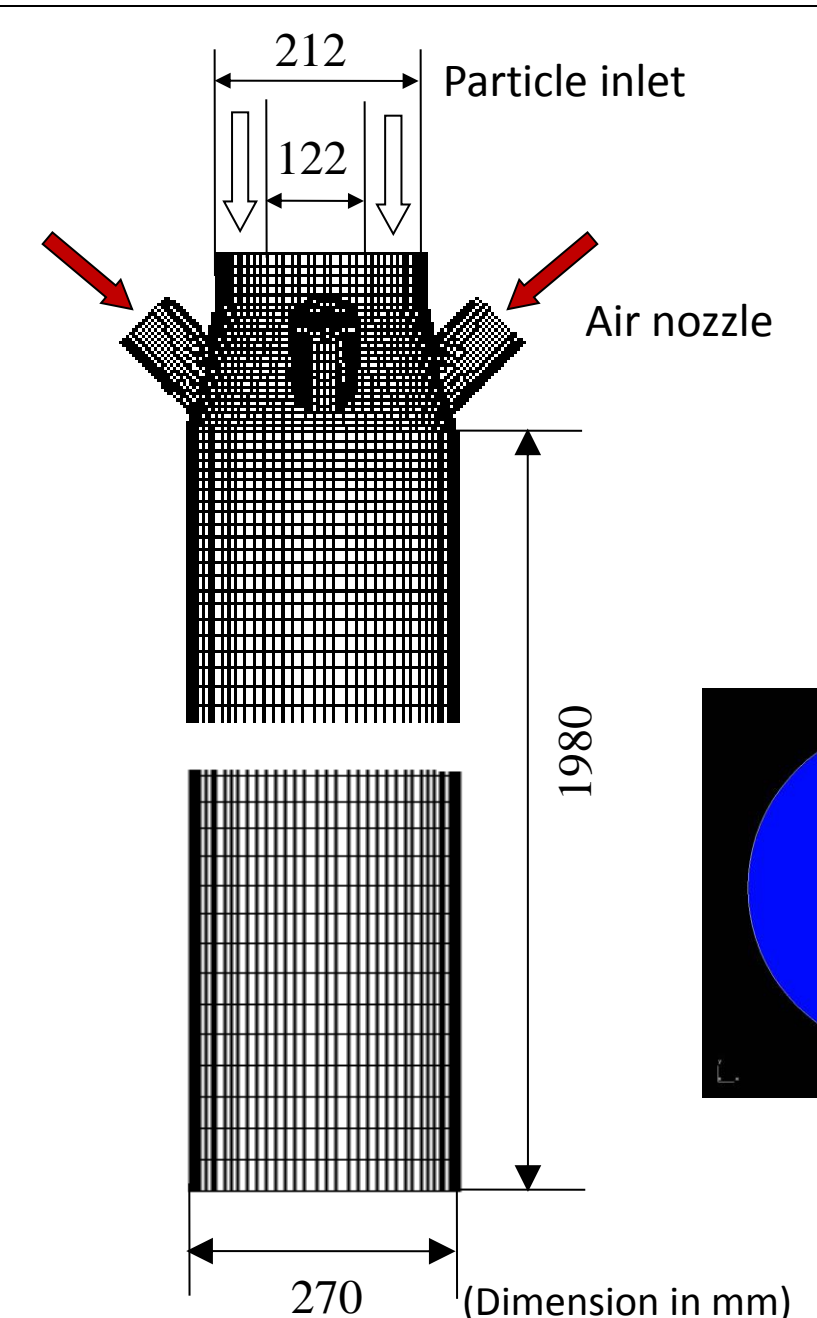
Simulation Conditions

T. Zhao and M.Takei, *Advanced Powder Technology, Elsevier*, (2008)
T.Zhao and M.Takei, *Powder Technology, Elsevier*, (2010)

Gas phase		Particle phase	
Fluid type	Air	Particle shape	spherical
Density(kg/m ³)	1.2	Density(kg/m ³)	1200
Bed geometry(m)	0.27 (diameter)	Particle diameter(mm)	0.3
	1.98(height)	Number of particles	328400
Superficial velocity (m/s)	20	Spring constant (N/m)	800
Viscosity(kg/ms)	2.0×10^{-5}	Friction coefficient	0.3
Acceleration of gravity (m/s ²)	9.8	Time step (s)	10^{-4}

Time step $\Delta t = \frac{2}{5} \pi \sqrt{\frac{(\pi d_p)^3 \rho_p}{6k_n}}$ (Y. Tsuji et al. 1992)

Calculation Domain and Calculation Results



$h=0.33\text{m}$ $h=0.99\text{m}$ $h=1.65\text{m}$
0.0% Powder concentration 5.0%

Fig. Simulation results of axial position

Calculated Profiles of Axial & Radial Volume Fraction

T.Zhao, M.Takei, *Flow Measurement and Instrumentation*, (2010)

T.Zhao, and M.Takei et al., *Advanced Powder Technology*, Elsevier, (2010)

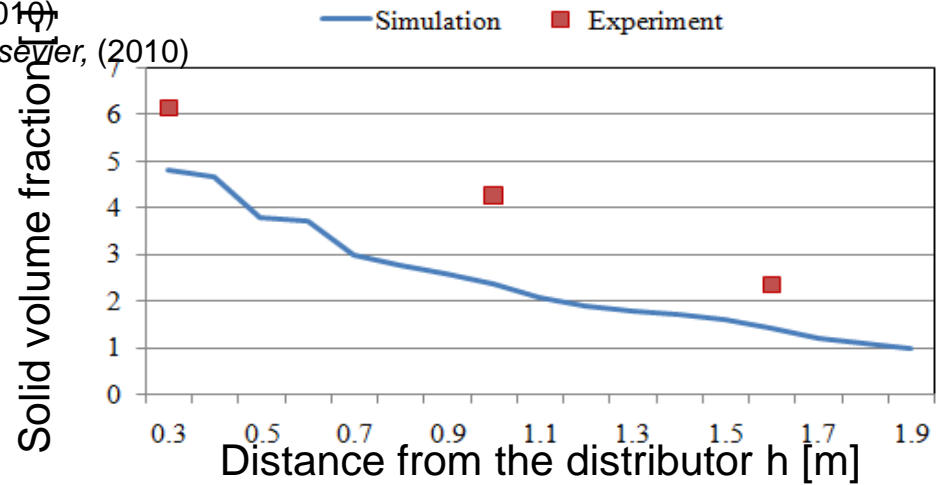
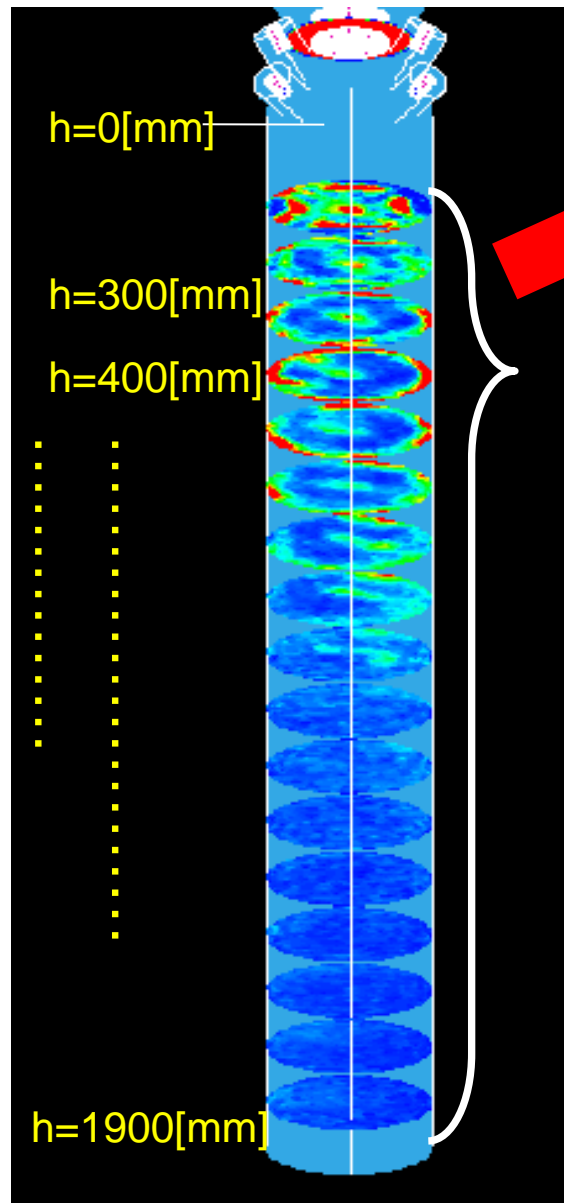


Fig. Profiles of axial volume fraction

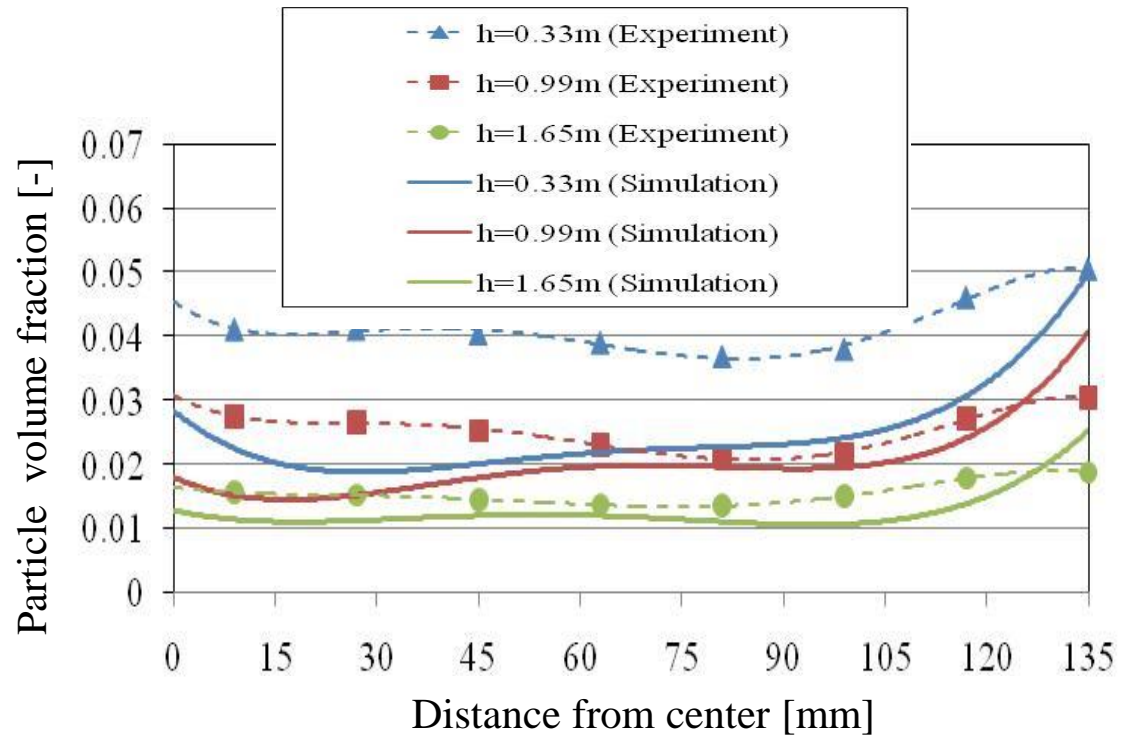


Fig. Profiles of radial volume fraction

COATING PROCESS IN DRUG PRODUCTION

Functional particle

Production by coating process

Nozzle spray of coating solvent to nucleus particles in fluidized bed

Dry of coating solvent around nucleus particles by hot air



Operational factors for uniform coating



Noninvasive monitoring technique to visualize the uniformity of particles fluidization during coating process

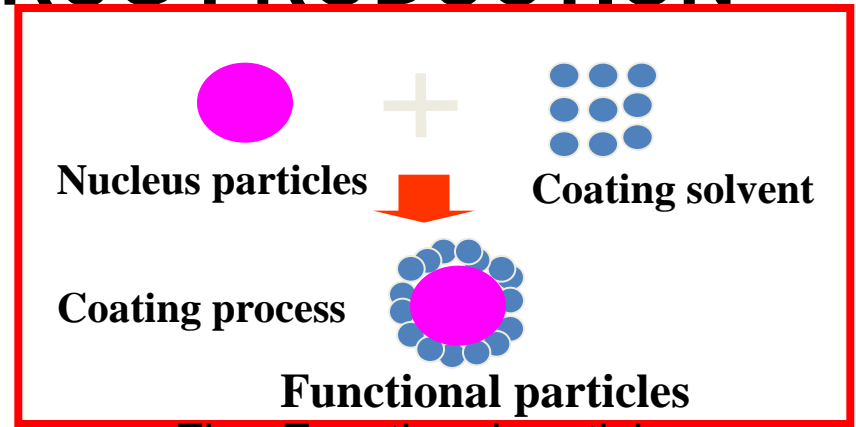


Fig. Functional particles

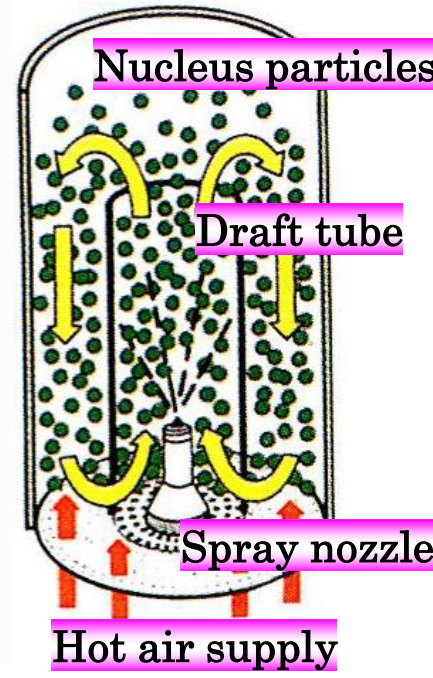
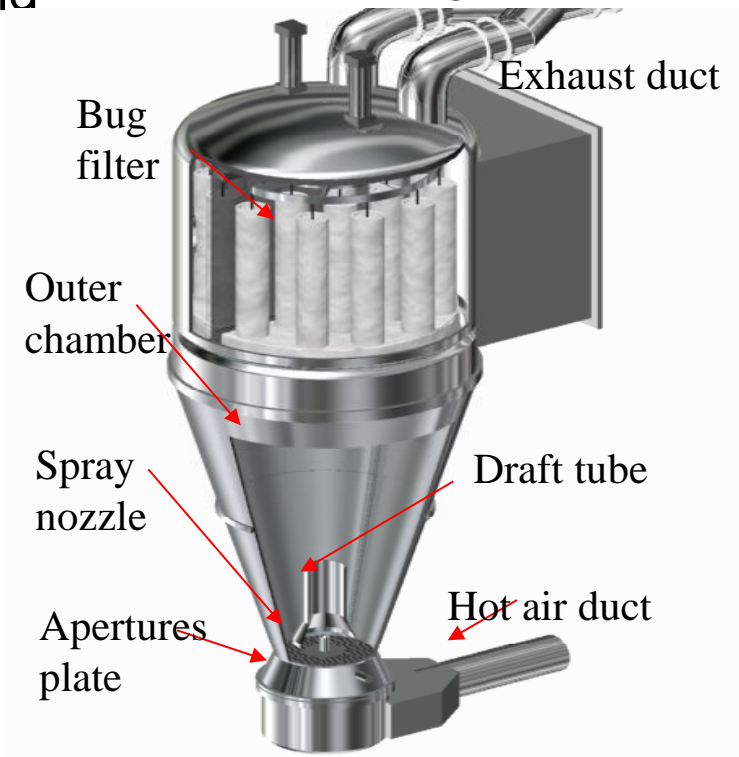


Fig. Coating process

INSTANTANEOUS CT IMAGES

Nucleus powder	Crystalline cellulose Asahi Kasei Corporation Celphia 203
Nucleus powder diameter	150 μ m
Density of powder	870 kg/m ³
Relative permittivity of Air	1.0006
Relative permittivity of Powder	2.1
Atomized coating liquid	HPC (Hydroxypropyl Cellulose) Shin-Etsu Chemical Co., Ltd.
Spray coating time	50 minutes
Sampling time	Every 5 minutes for several seconds

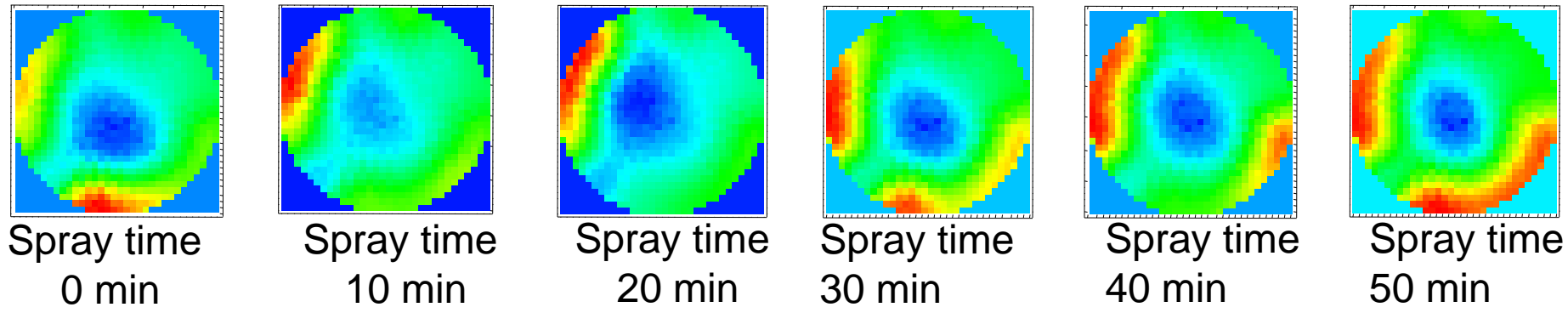



Fig. Instantaneous CT Images at each spray time 0.0  1.0
Concentration



The high concentration particle distribution is located near the tube

SPATIAL MEAN CONCENTRATION FROM IMAGE

M.Takei, et al., *Powder Technology, Elsevier, (2009)*

The spatial mean particle concentration at a time point

$$\overline{D}_p(t) = \frac{1}{(N_x N_y - N_{out})} \sum_{y=1}^{N_y} \sum_{x=1}^{N_x} \mathbf{E}_{xyt}$$

N_{out} : the pixel number outside the pipe

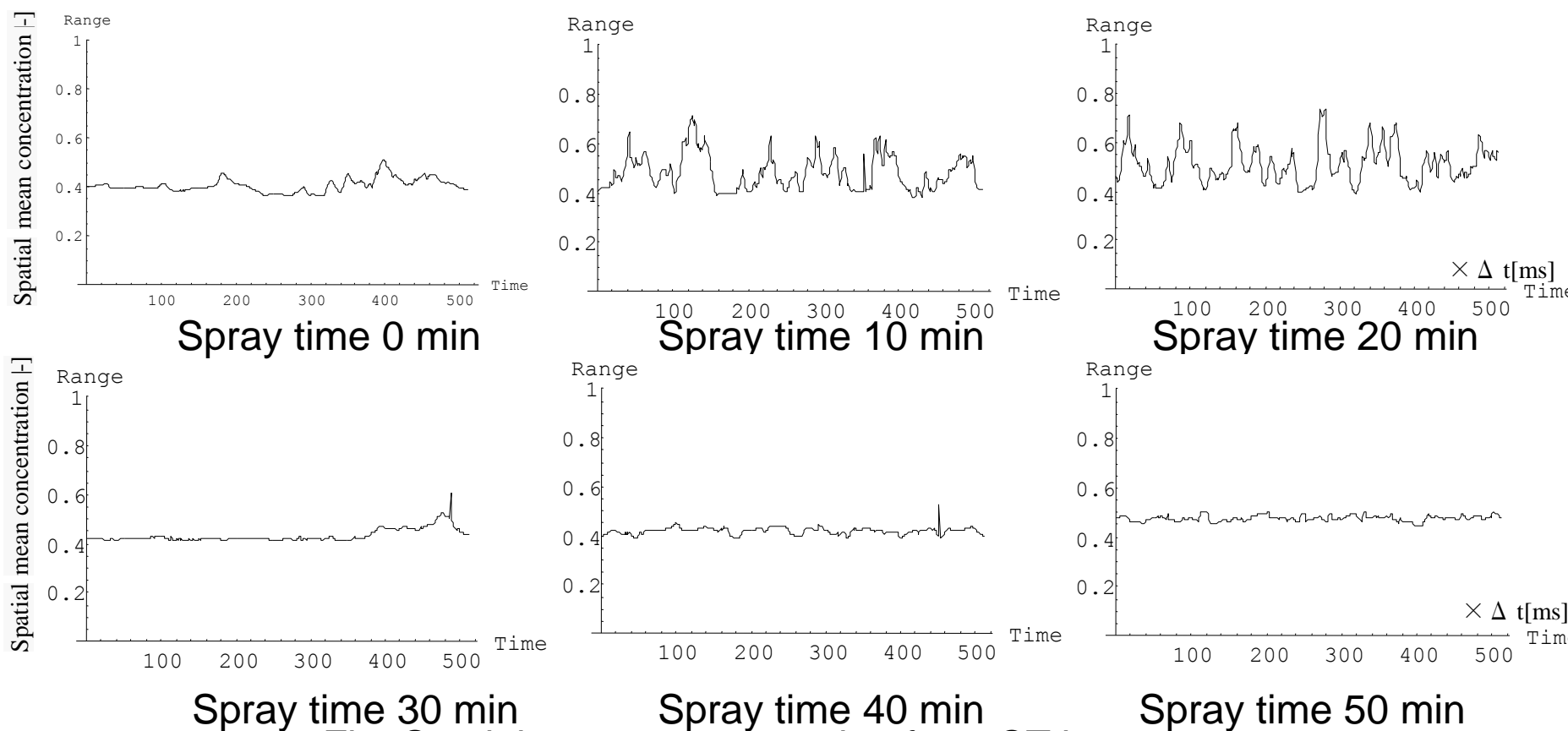
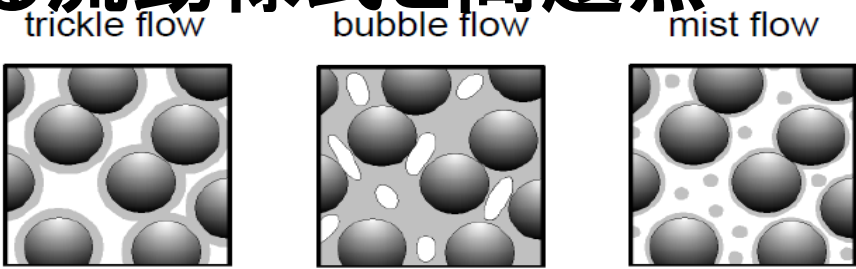
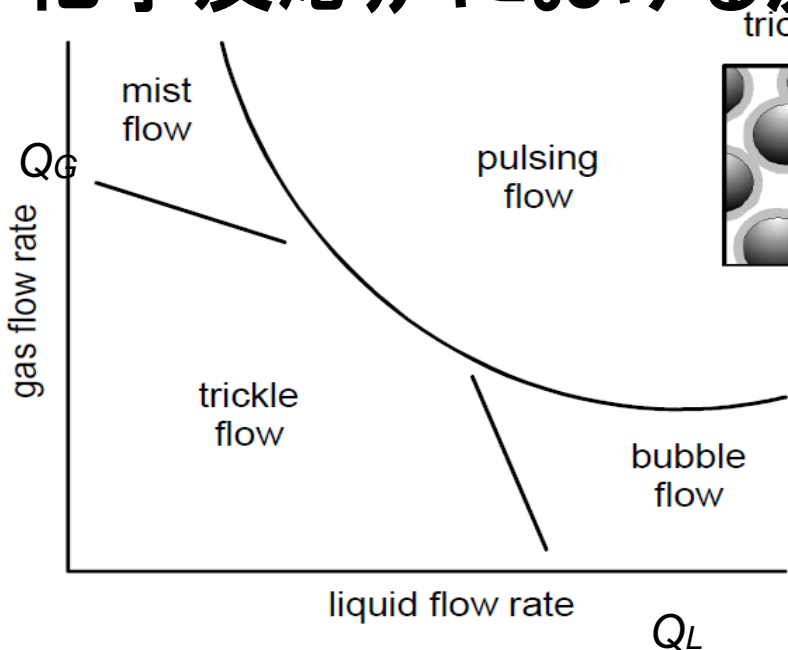


Fig. Spatial mean concentration from CT images.

CONTENTS

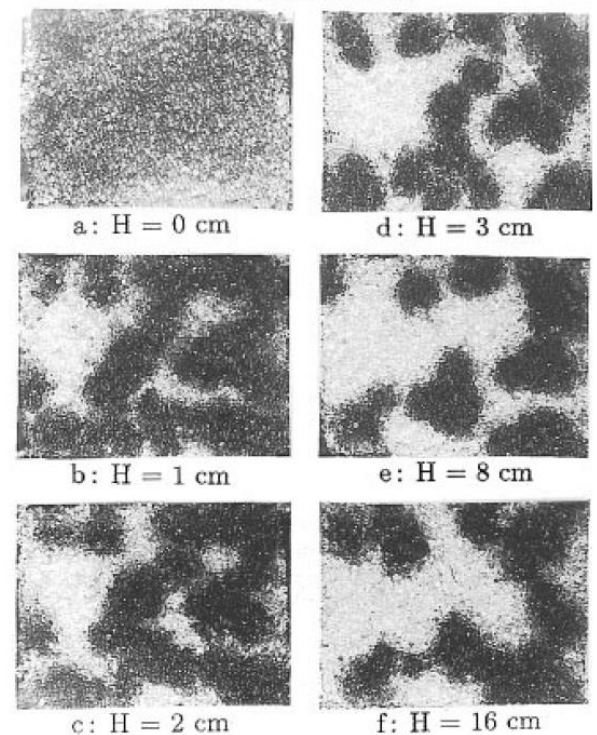
- PTの概要 ソフトフィールドとハードフィールド
 - ソフトフィールドPT
 - 電気PTの原理
 - プラントへの展開
 - 血流への展開
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 - Positron Emission Tomography (PET)
 - まとめ
- ①ECTの例 ②ERTの例
③温度分布計測の例

化学反応炉における流動様式と問題点



liquid phase
 gas phase
 solid phase

Ravindra, P.V. et al. (1997)



●問題点

液体の偏流(チャネリング)

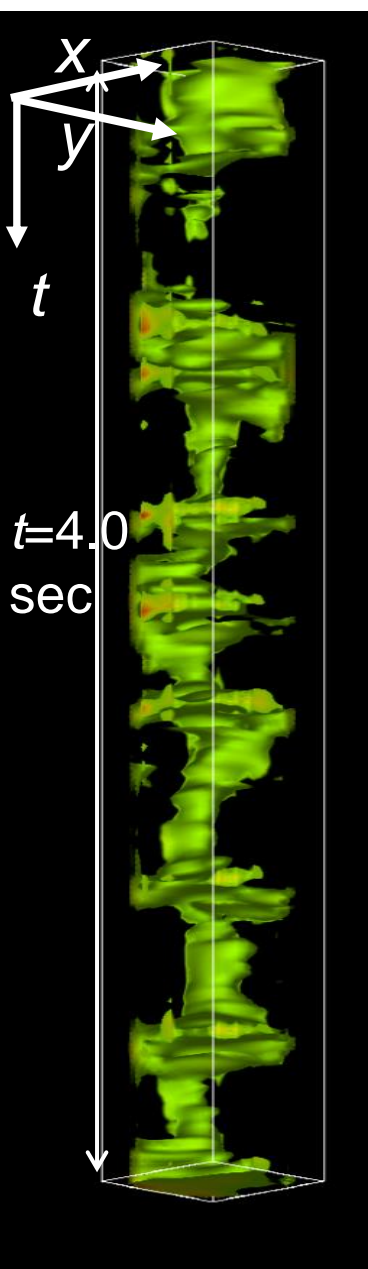
- 反応効率の低下
- 反応熱の蓄積

Q_L と Q_G に対する流動状態の把握が不十分

- 低パフォーマンス化

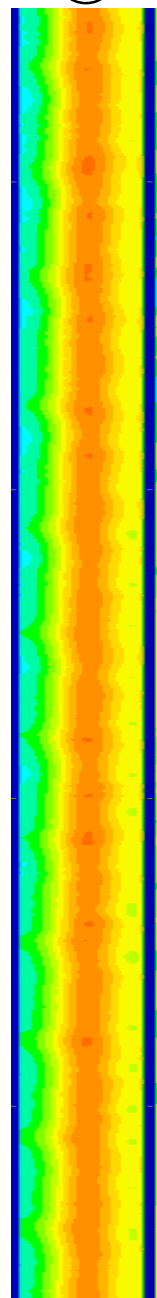
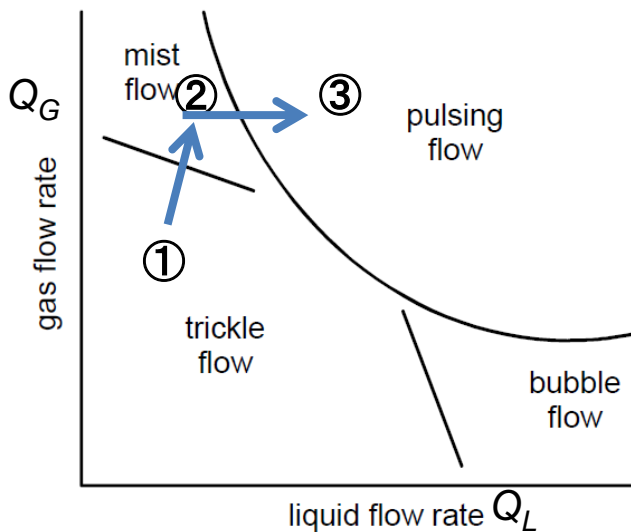
Fig.着色法による偏流の破壊可視化

流動様式の比較

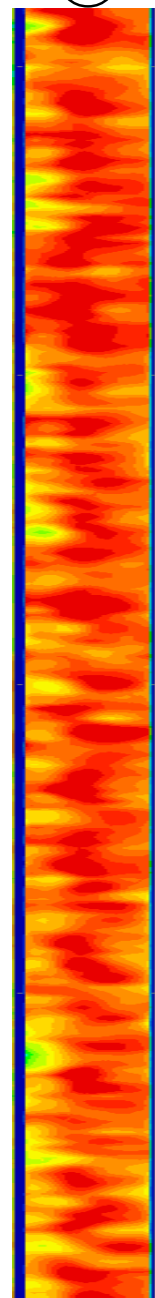


$(Q_L, Q_G) = (13\text{L/min}, 70\text{L/min})$

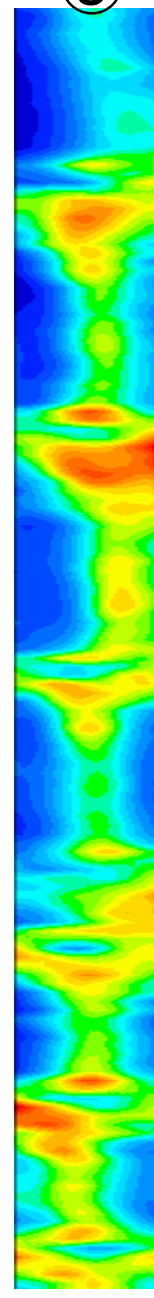
$z = 1020\text{ mm},$
 $d_p = 5\text{ mm},$



トリクル流

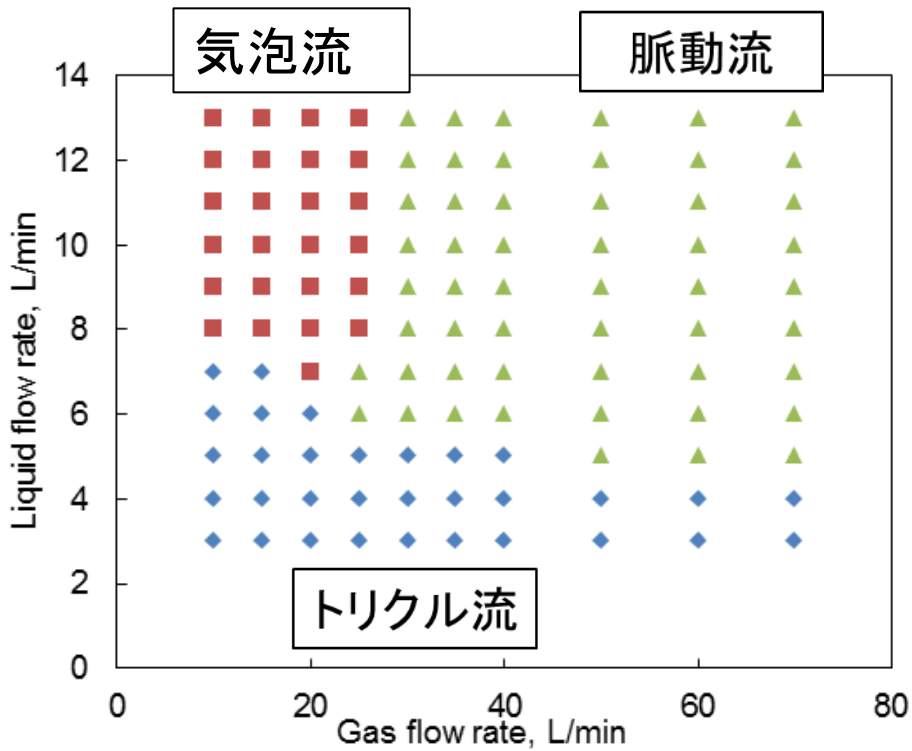
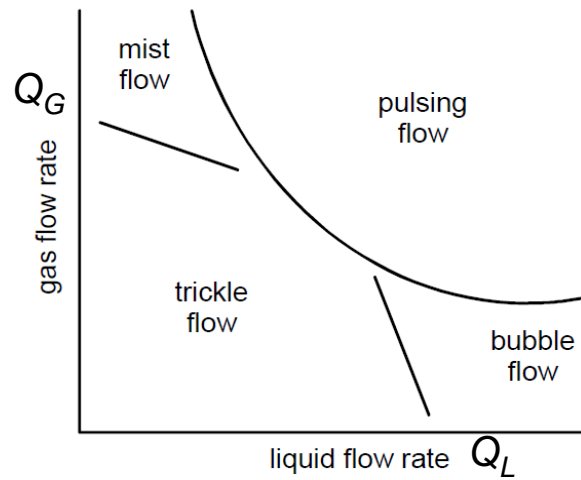


気泡流

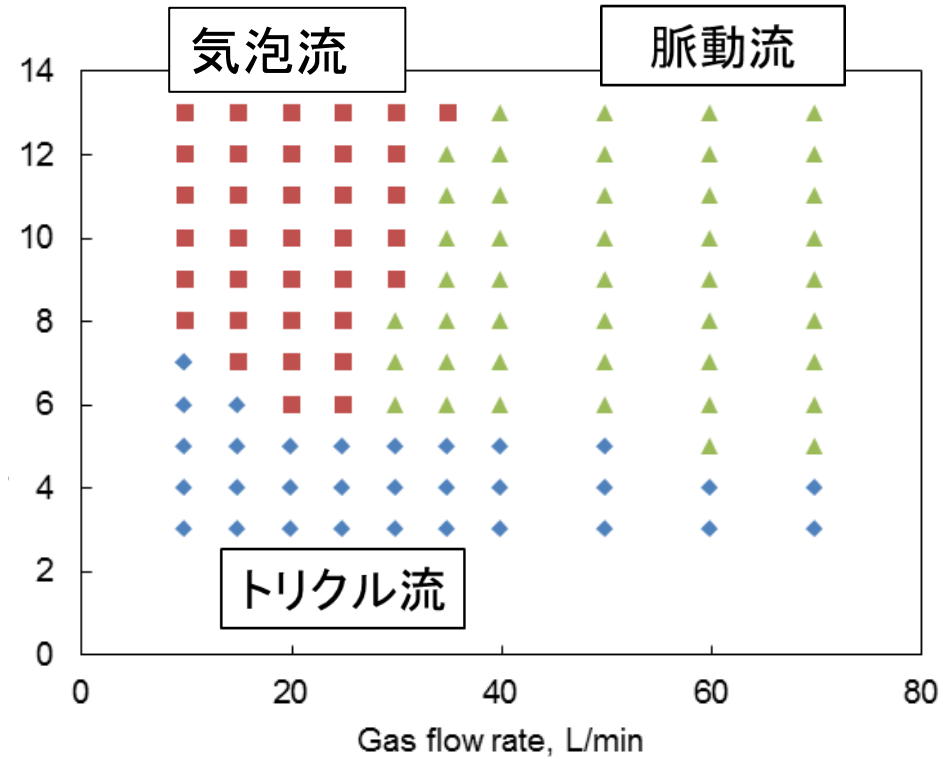


脈動流

状態図

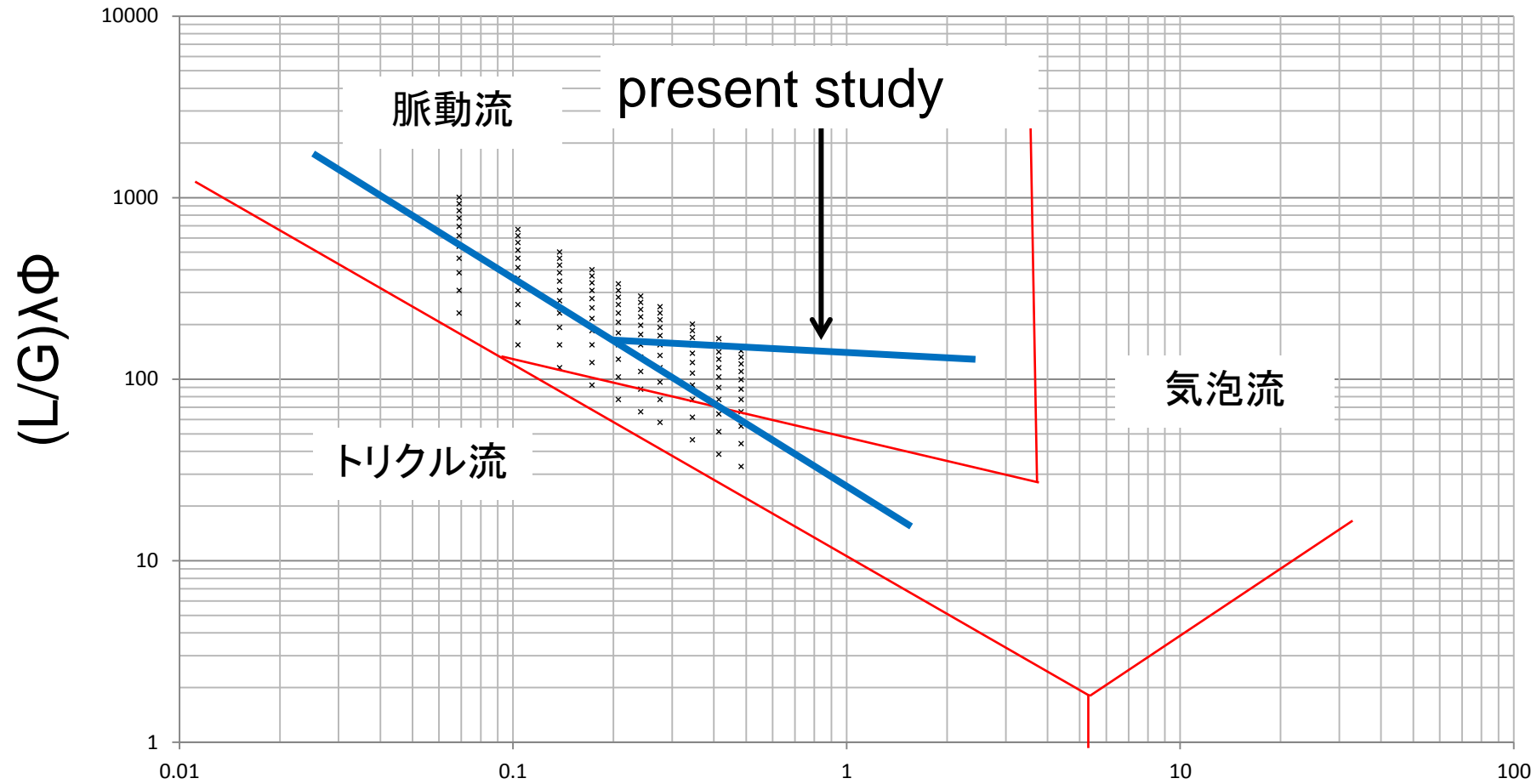


$d_p = 3 \text{ mm}$



$d_p = 5 \text{ mm}$

状態図の比較



G, L : ガス, 液の質量速度 $[\text{kg}/\text{m}^2\text{s}]$

$$\lambda = (\rho_G \rho_L / \rho_A \rho_W)$$

$$\phi = (\sigma_W \sigma_L) [(\mu_L / \mu_W) (\sigma_W / \sigma_L)^2]^{1/3}$$

ε : 充填層の空隙率 [-]

ρ_G, ρ_L : ガス, 液の密度 $[\text{kg}/\text{m}^3]$

ρ_A, ρ_W : 空気, 水の密度 $[\text{kg}/\text{m}^3]$

μ_L : 液の粘度 $[\text{kg}/\text{m} \cdot \text{s}]$, μ_W : 水の粘度 $[\text{kg}/\text{m} \cdot \text{s}]$

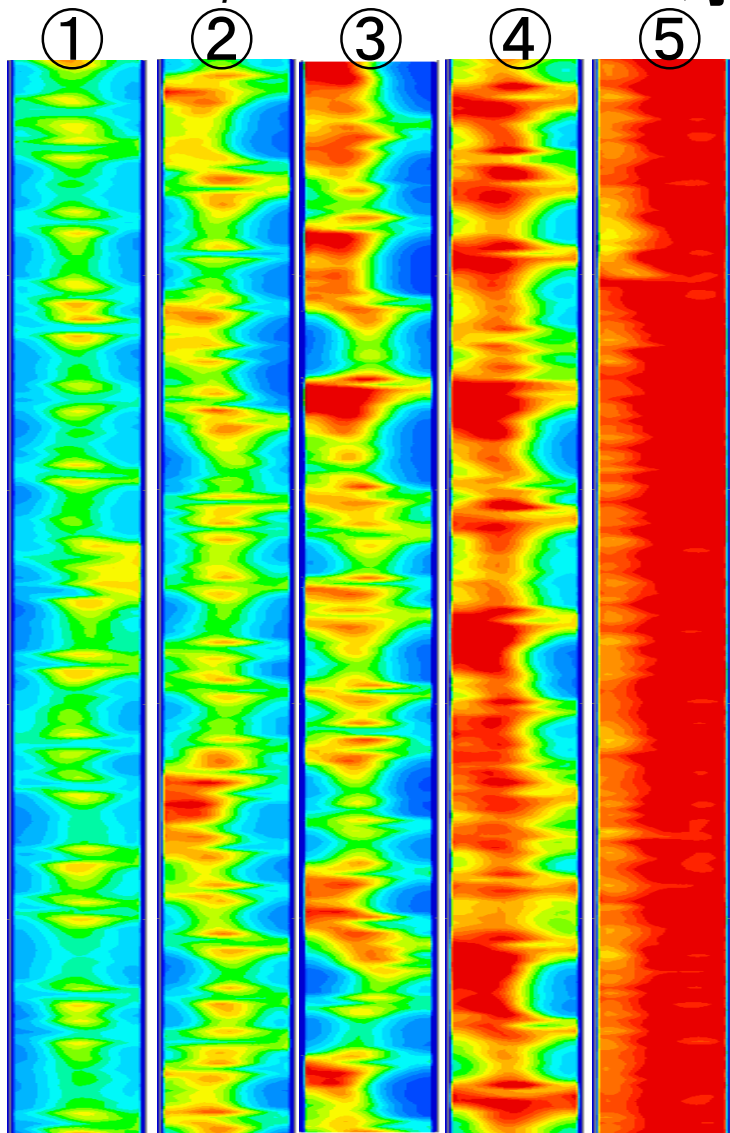
σ_L : 液の表面張力 $[\text{kg}/\text{m}^2]$, σ_W : 水の表面張力 $[\text{kg}/\text{m}^2]$

A. Gianetto et al., AIChE J 24,(6)1087(1978)

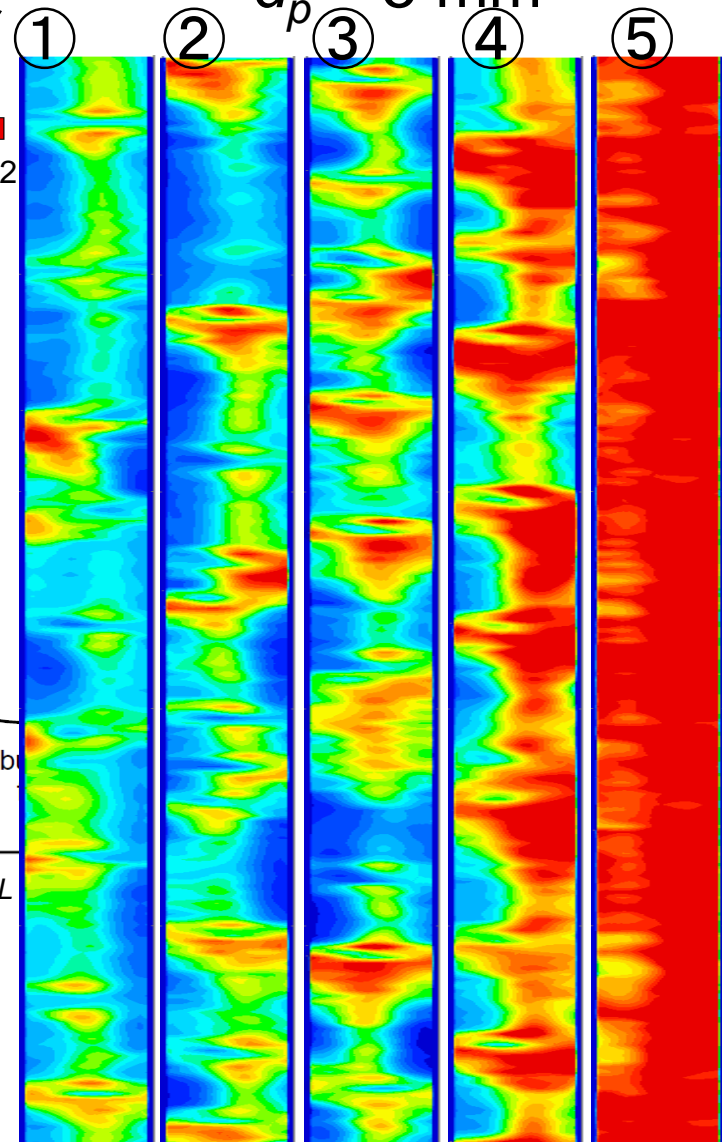
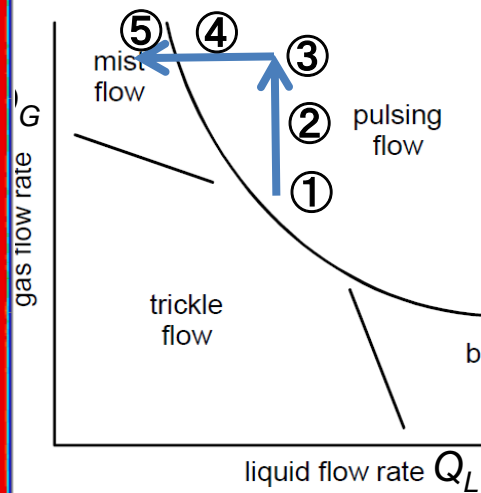
$d_p = 3 \text{ mm}$

水平断面画像

$d_p = 5 \text{ mm}$



(Q_L, Q_G) (Q_L, Q_G) (Q_L, Q_G) (Q_L, Q_G) (Q_L, Q_G)
7, 100 11, 100 15, 100 15, 60 15, 20



(Q_L, Q_G) (Q_L, Q_G) (Q_L, Q_G) (Q_L, Q_G) (Q_L, Q_G)
7, 100 11, 100 15, 100 15, 60 15, 20



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- ①ECTの例 ②ERTの例
③温度分布計測の例

PT法による濃度・温度分布の画像再構成

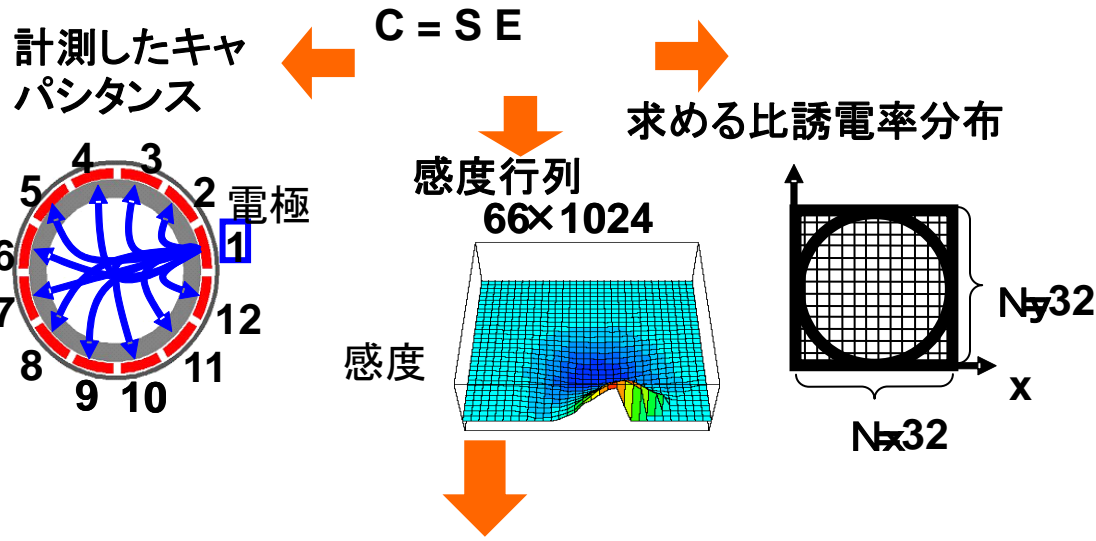
$$C_{i,j} = -\frac{\epsilon_0}{V_c} \oint_{r \in \Gamma_j} \epsilon(\mathbf{r}) \nabla V_i(\mathbf{r}) \cdot d\mathbf{r} \quad \nabla \cdot [\epsilon(\mathbf{r}) \nabla V(\mathbf{r})] = 0$$

($i = 1, 2, \dots, 11; j = i + 1, \dots, 12$)

$C_{i,j}$: 電極*i*と*j*間のキャパシタンス, ϵ_0 : 真空の誘電率, V_c : 電極にかける電圧, \mathbf{r} : 位置ベクトル, ϵ : 比誘電率, $V(\mathbf{r})$: 位置*r*における電位, Γ : 電気力線がカバーする領域

逆問題による比誘電率分布の計算

デバイ式による比誘電率から温度分布の計算



$$\frac{\epsilon - 1}{\epsilon + 2} = \frac{\rho N_A}{3 \epsilon_0 M} \left(\frac{\mu^2}{3 k_B T} \right)$$

$$T = \left(\frac{\epsilon + 2}{\epsilon - 1} \right) \left(\frac{\rho N_A \mu^2}{3 \epsilon_0 M 3 k_B} \right)$$

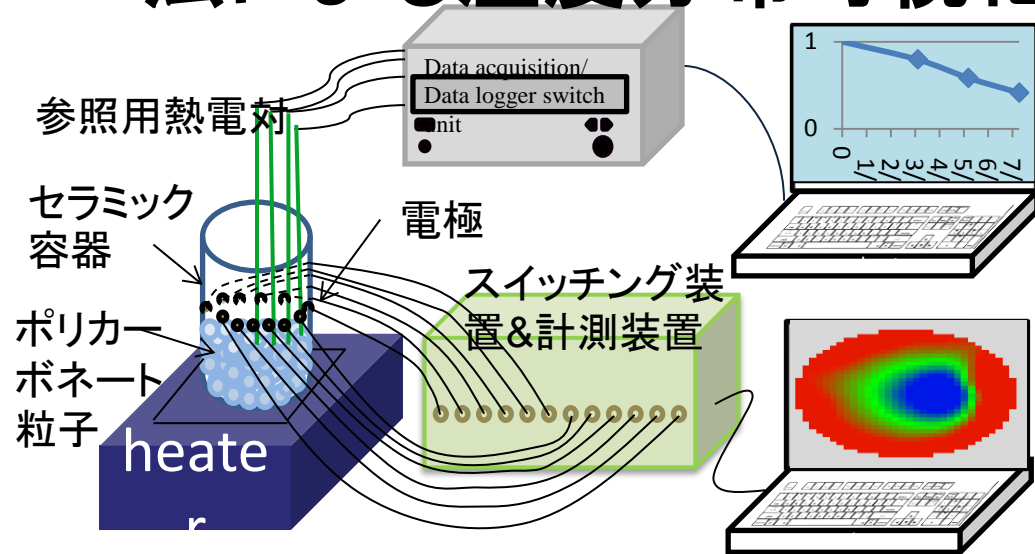
$$T = f(\epsilon)$$

不適切逆問題 未知数 > 式数

ϵ_0 : 真空の誘電率[F/m], M : モル質量[kg/mol],
 ρ : 密度[kg/m³], N_A : アボガドロ定数[l/mol],
 T : 温度[K], k_B : ボルツマン定数[J/K],
 μ : 永久双極子モーメント[D], ϵ : 比誘電率[-]

画像再構成アルゴリズム
 近似的な比誘電率(濃度)分布

PT法による温度分布可視化計測



- ポリカーボネート粒子のPTセンサ内充填+下部中心より加熱溶解
- デバイ式により誘電率分布から温度分布の画像再構成
- 温度分布の3D(2D+時間)可視化計測に成功
- 従来技術(熱電対)と比較して数%の誤差

図 温度分布可視化計測の装置

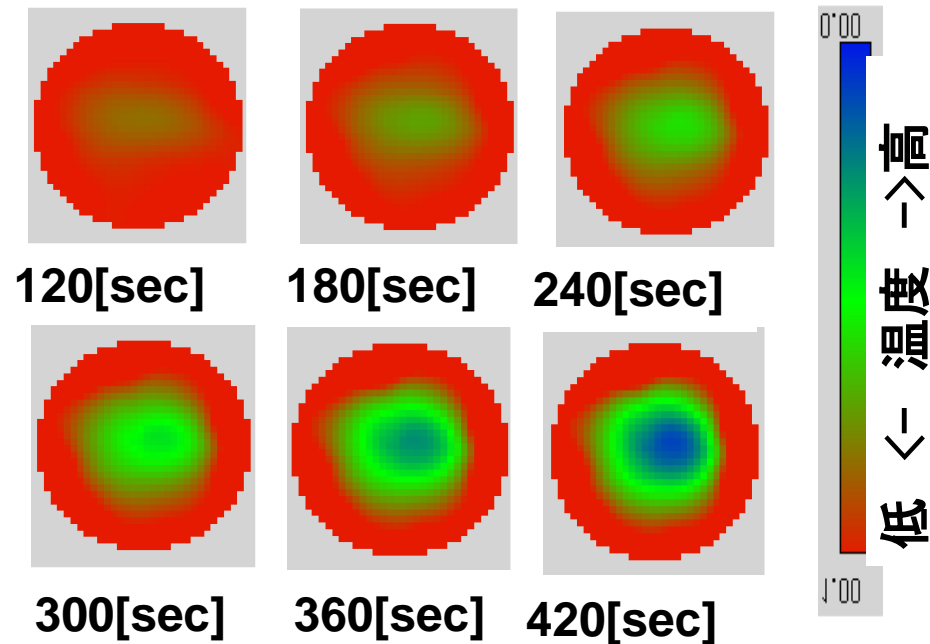


図 温度分布の時間変化画像

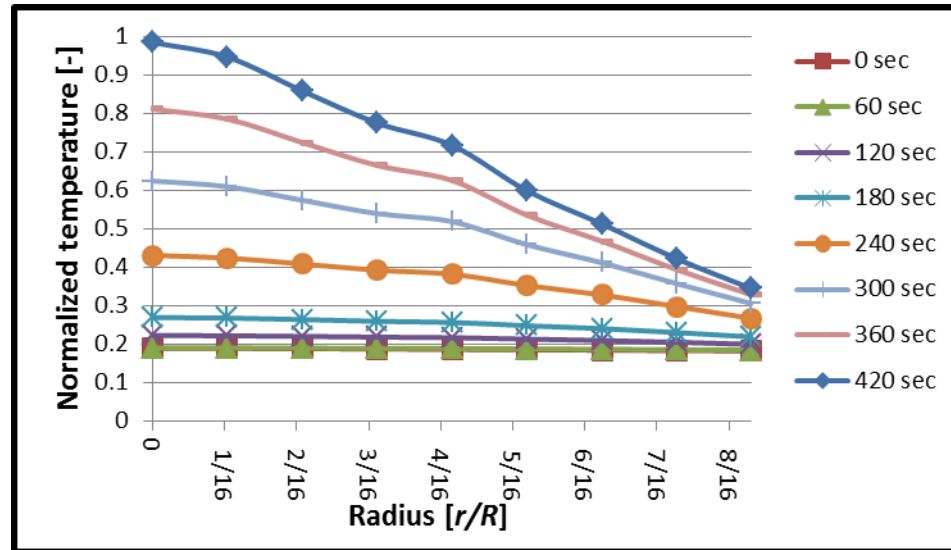


図 PT法による温度分布の時間変化

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背景と従来技術の問題点

日本人の死因:30% 循環器系疾患

人工臓器の実用化

人工臓器による
血栓症リスクの増大

大量の抗凝固剤投与
患者の血栓に対する不安

血栓症の予測(いつ、どこで、どれだけの血栓)の可能性

しかしながら

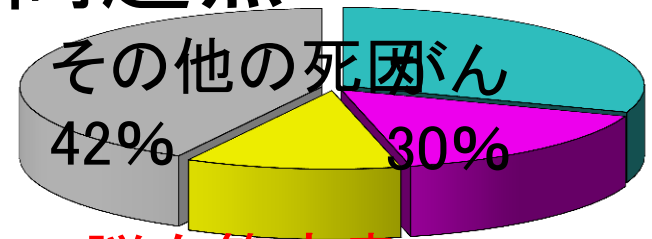
1) 血栓検出計測技術の未熟性

血栓オンライン計測が不可能

30万人 人工透析患者
在宅人工透析が進まない理由

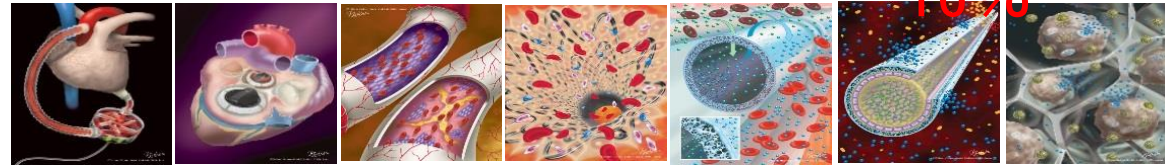
2) 人工臓器と血液との界面マルチフィジックスが不明

血栓未来予測が不可能



脳血管疾患12% 心疾患16%

図 日本人の死因 (厚生労働省:人口動態統計の概況より)



人工心臓 人工弁 人工血管 スtent 人工肺 人工腎臓 人工肝臓

補助人工心臓の例

体内植え込み型補助人工心臓の薬事承認

2011年4月1日より発売
「EVAHEART」「DuraHeart」

血栓が生じやすい
脳梗塞などの合併症

血栓症の未来予測技術の確立

トータルソリューションの研究開発

- ① 血栓 *Insitu* (その場) 検出技術
- ② 血栓 *Insilico* (シミュレーション) 予測技術
- ③ 血栓 *In vitro* (精密制御体外実験) 検証

補助人工心臓
を装着して自宅
療養・職場復帰

千葉大学病院でも
症例多数あり

そこで、私たちの提案!!

送血管

上行大動脈

左心室

脱血管

補助人工心臓インペラ

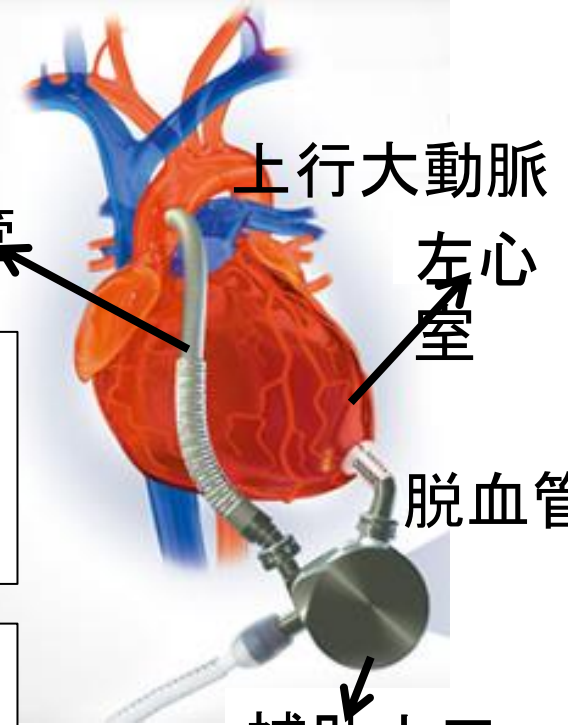
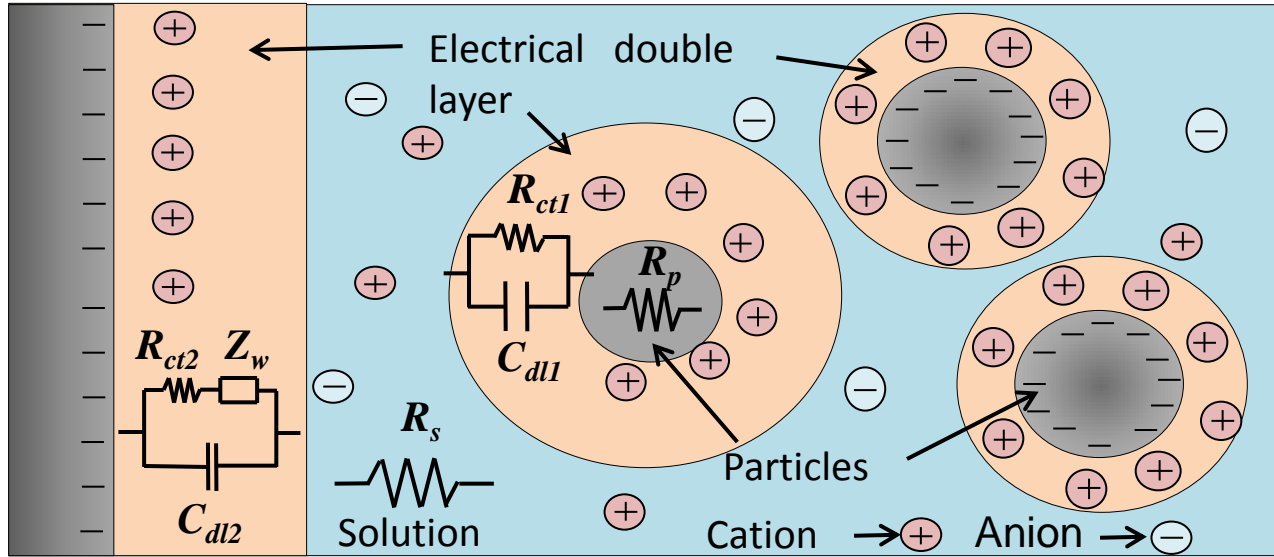


図 血栓が生じた人工心臓インペラ

血流におけるインピーダンス計測

電気二重層



R_{ct1} : 粒子界面電気二重層
電荷移動抵抗

C_{ct1} : 粒子界面電気二重層
容量

R_{ct2} : 電極界面電気二重層
電荷移動抵抗

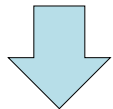
C_{ct2} : 電極界面電気二重層
容量

R_p : 粒子抵抗 R_s : 溶液抵抗

Z_w : ワールブルグインピーダンス

電気二重層

溶液中の粒子は多くの場合帯電

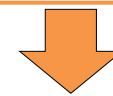


溶液中の対イオンが集まり、
界面にイオンの層が形成(電気二重層)

- ・コンデンサのような電気容量
- ・緩和周波数

インピーダンストモグラフィ

- ・単一周波数
- ・インピーダンス値のみ計測



周波数をスイープして様々な電気成分を計測

誘電スペクトル

⇒電子分極

⇐配向分極⇒

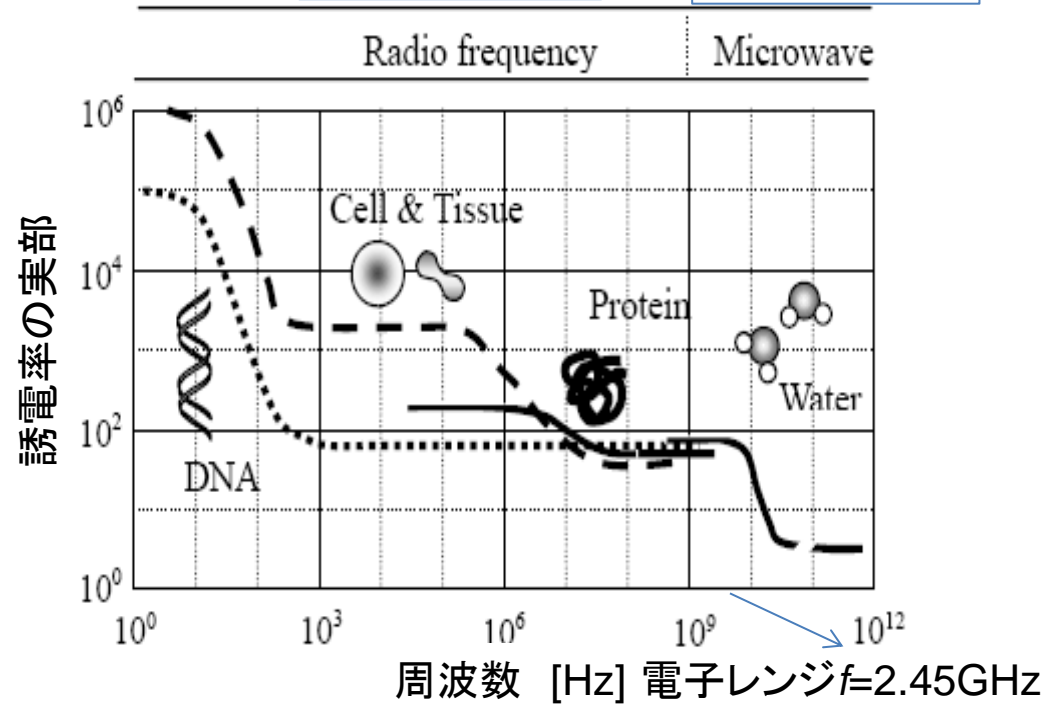
⇒イオン分極

●電束密度と分極

$$D = \epsilon_0 E + P$$

$$P = Nm = N\alpha F$$

D : 電束密度[C/m²], ϵ_0 : 真空の誘電率[F/m], E : 電場[V/m], P : 分極[C/m²], N : 単位体積当たりの分子数[-], m : 誘起双極子モーメント[Cm], F : 有効電場[V/m], ϵ : 誘電率[F/m], α : 分子の分極率 [Cm²/V], μ : 永久双極子モーメント [Cm]



浅見耕司 <http://www003.upp.so-net.ne.jp/asami/DS.pdf>より

配向分極(極性分子)

Clausius-Mossotti式

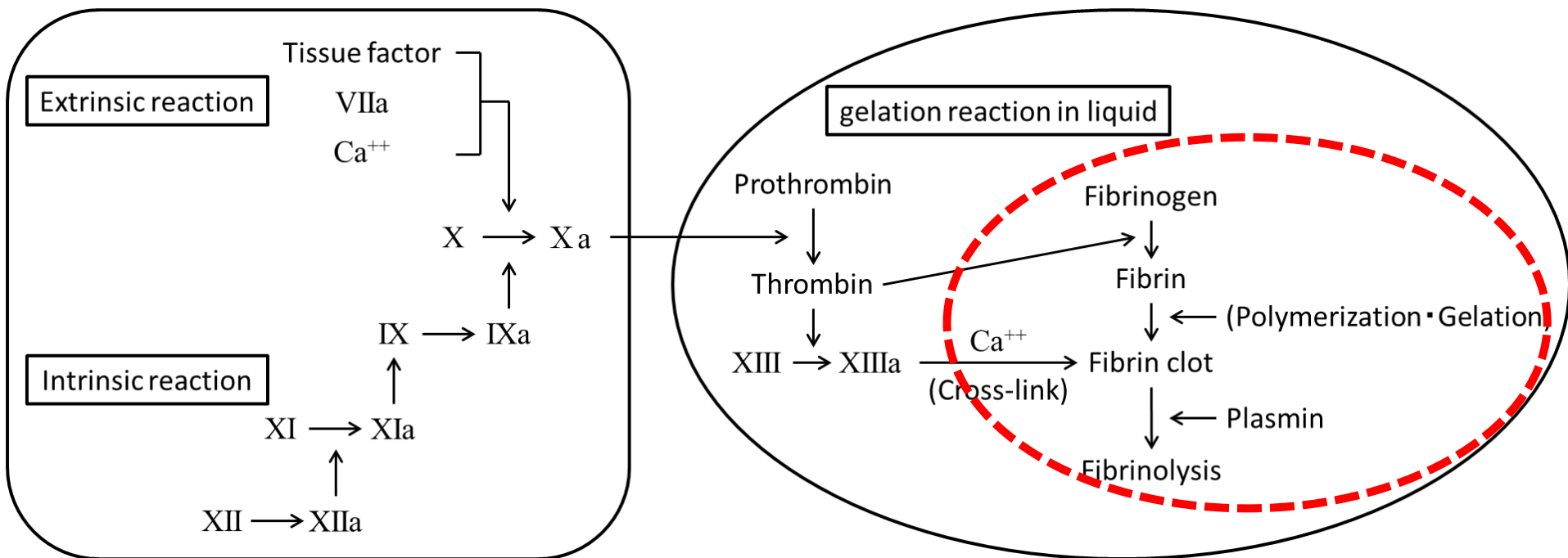
$$\frac{\epsilon - 1}{\epsilon + 2} \frac{M_W}{\rho} = \frac{N_A \alpha}{3\epsilon_0}$$

Debye式

$$\frac{\epsilon - 1}{\epsilon + 2} \frac{M_W}{\rho} = \frac{N_A}{3\epsilon_0} \left(\alpha_e + \frac{\mu^2}{3k_B T} \right)$$

M_W : 分子量, N_A : Avogadro数, k_B : Boltzmann定数, T : 絶対温度, ρ : 密度

血液凝固過程と電気的特性



● 低測定周波数 ⇒ 血漿の抵抗率変化

#1. フィブリン・クロット(フィブリンのゲル化)形成時における血漿タンパク(プロトロンビンとフィブリノーゲン)量と抵抗率との関係の知見

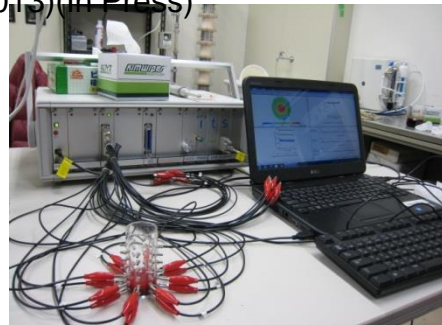
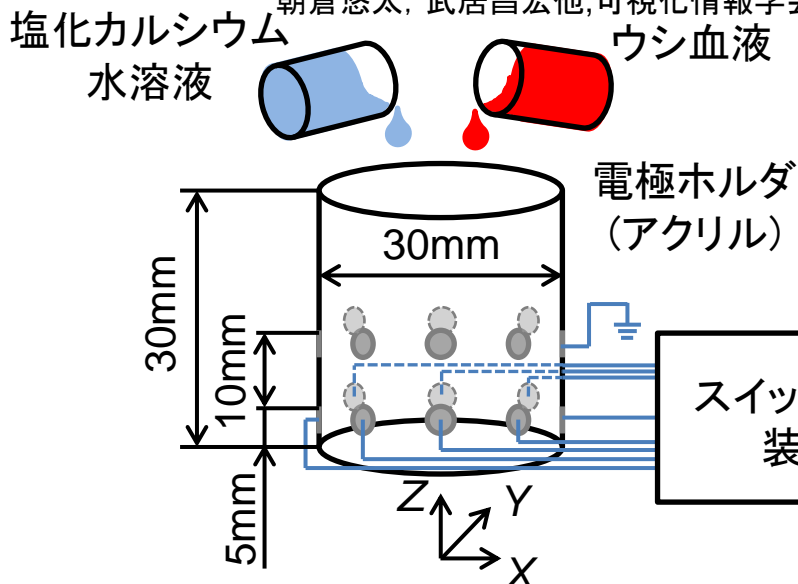
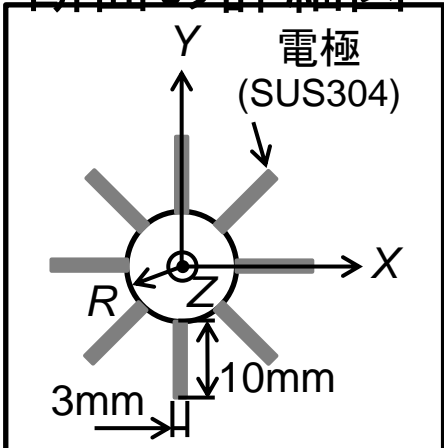
● 高測定周波数 ⇒ 赤血球膜のキャパシタンス(リアクタンス)変化

#2. 赤血球の凝集(血栓形成)により赤血球膜のリアクタンス変化の知見

血栓 *In situ* 検出の血栓形成過程の可視化

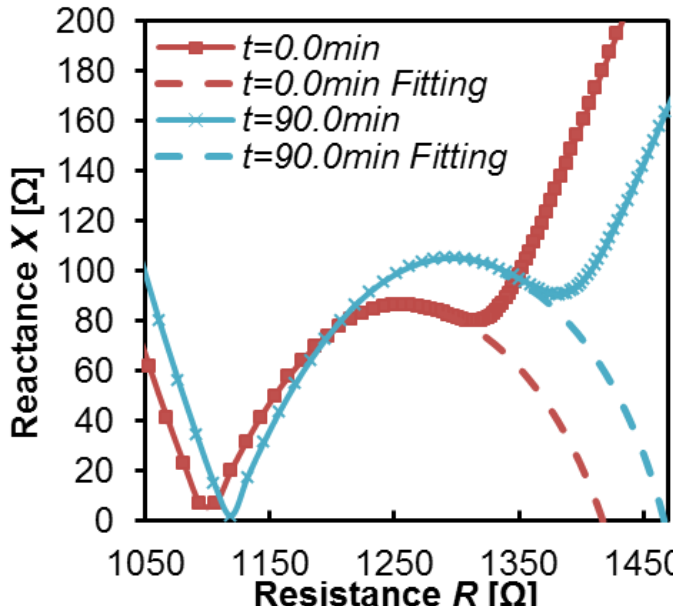
武居, (社) 日本人工臓器学会2012年度 Grant
 朝倉悠太, 武居昌宏他, 可視化情報学会論文集(2013)(In Press)

断面の詳細図



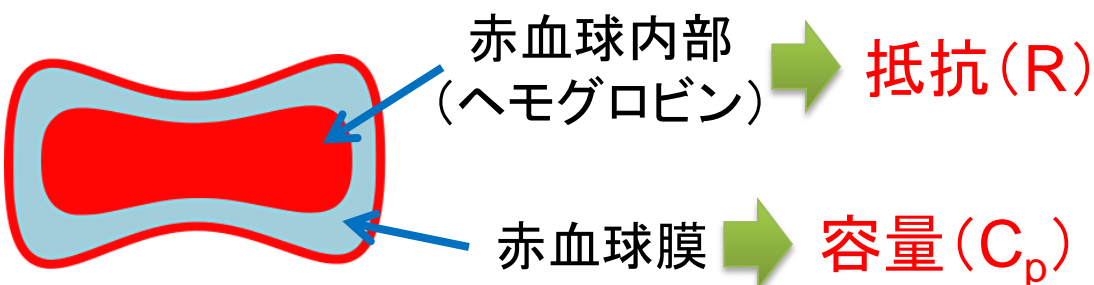
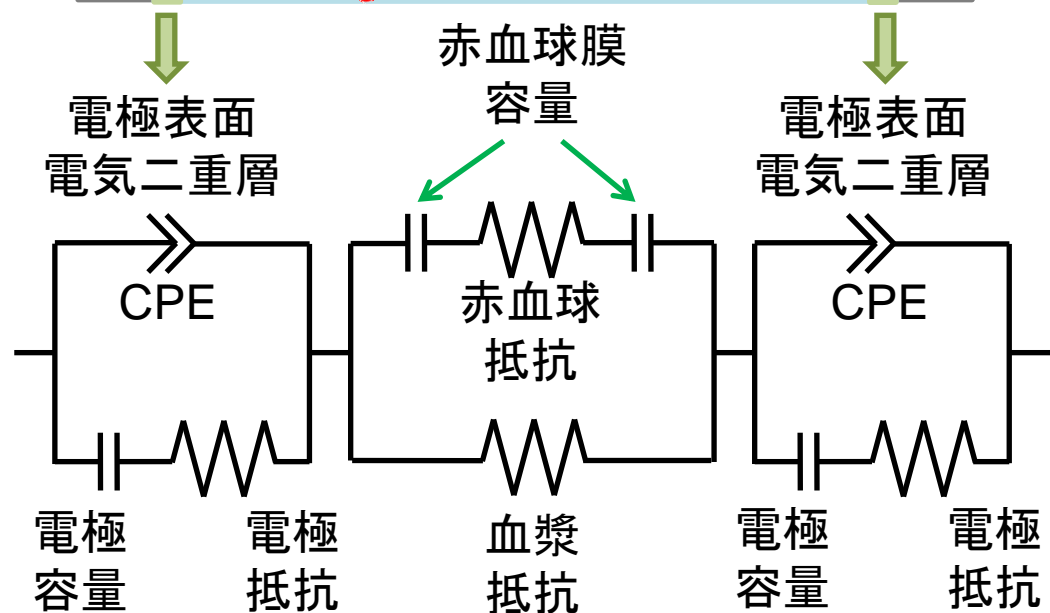
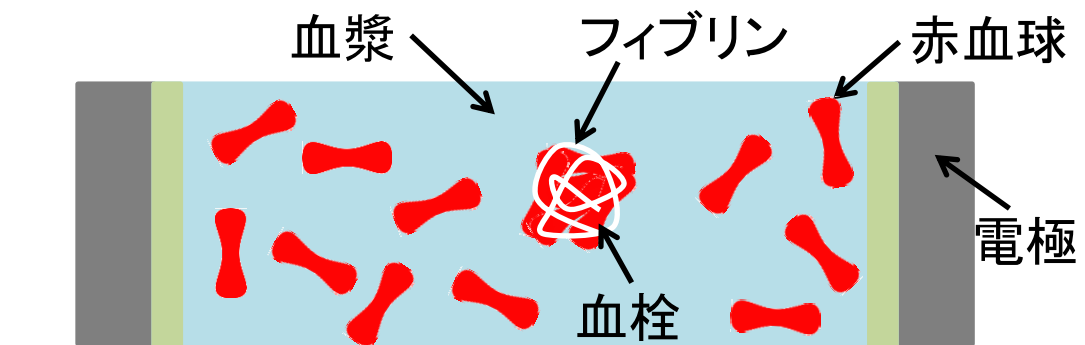
	t [min]	0.0	10.0	20.0	30.0	40.0	50.0	60.0	70.0	80.0	90.0
RBCs	Plasma 63%										
	Plasma 90%										
	Plasma 99%										
	Plasma 100%										

血栓形成過程のPT可視化画像

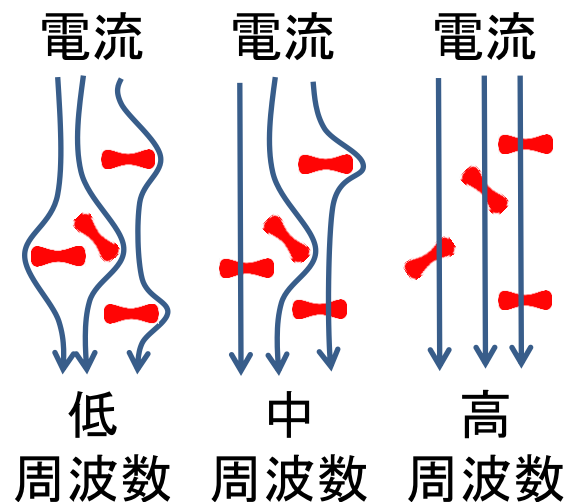
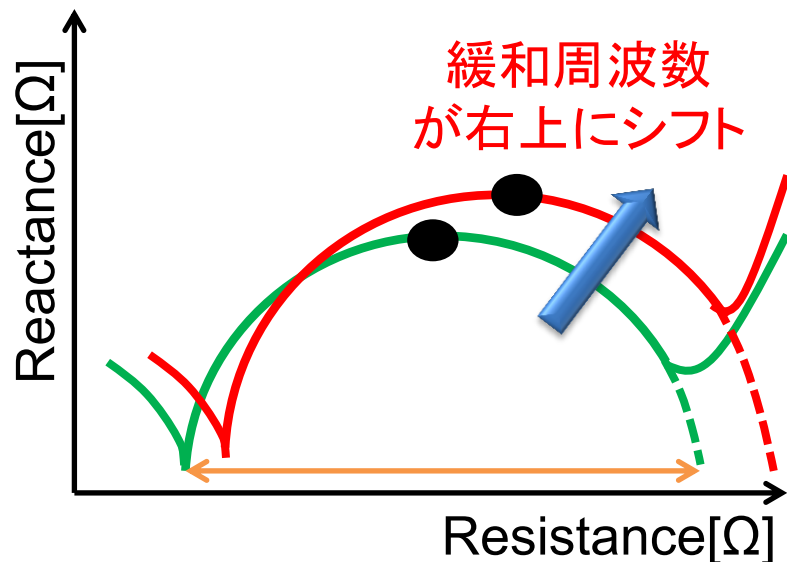


血栓形成過程のCole-Cole plot

赤血球膜のリアクタンスの時間変化

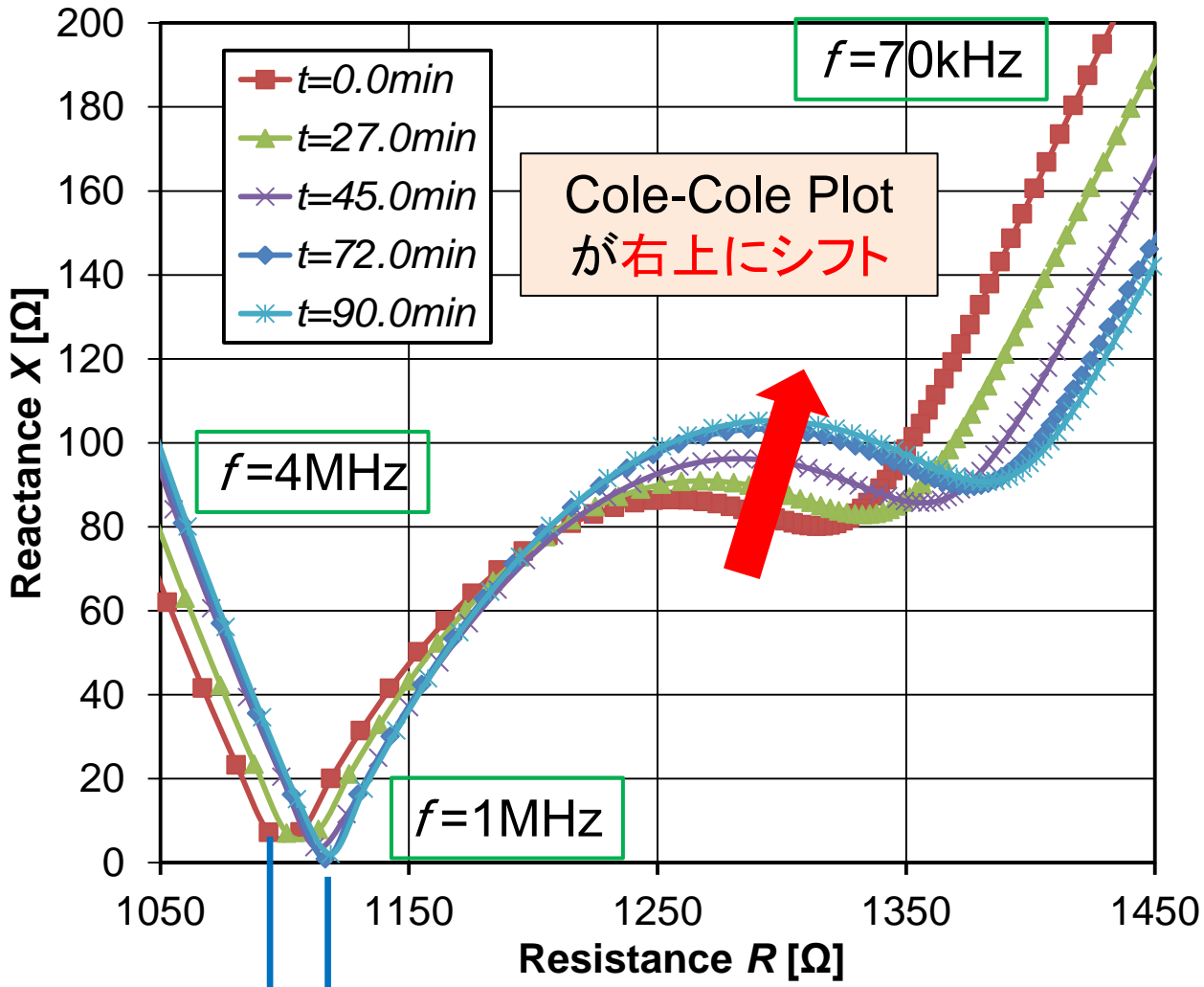


Cole-Cole Plot

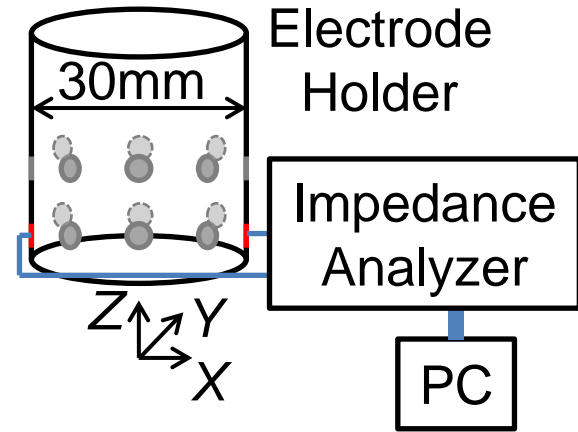


赤血球膜のリアクタンスの時間変化

(Plasma 63%+30%CaCl₂)



20Ω → 血漿凝固によって抵抗が増加



印加電圧 V	1[V]
測定周波数 f	70kHz ~ 4MHz
測定時間 t	90min
測定点数	60 Point

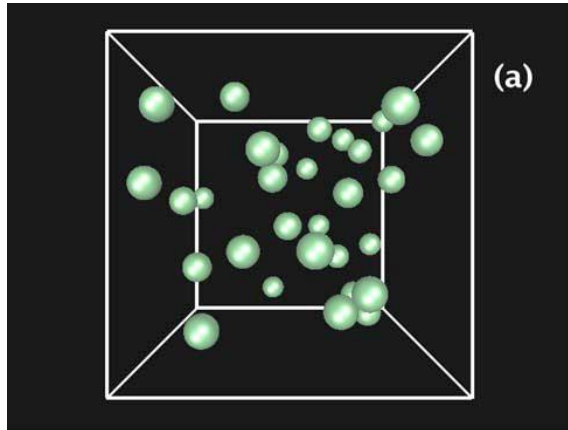
Cole-Cole Plotがシフト
赤血球の凝集(血栓形成)により赤血球膜のCが減少しXが増加

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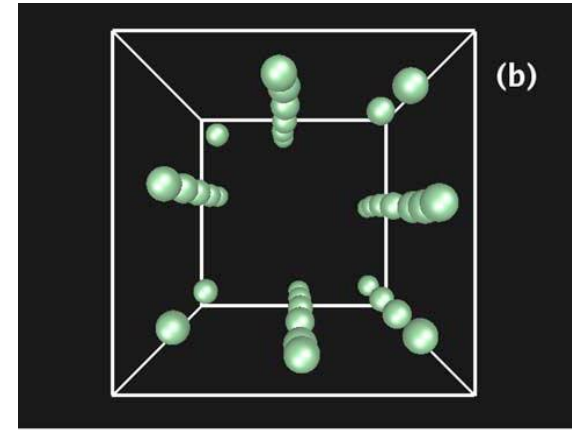
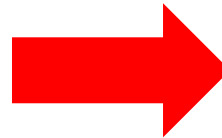
- PTの概要 ソフトフィールドとハードフィールド
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Previous Study on Particle Migration

B. Chun et al. *Physics of fluids* (2010)



Upstream
Uniform particles distribution



Downstream at $Re=100$,
Migrate 8 equilibrium positions, Linear chains

Migration

Reynolds number Re , Particle Reynolds number Rep ,
Initial particle concentration ξ , Particle size d_p
Downstream position z



How to measure 3D particle concentration?

Typical measurement technique

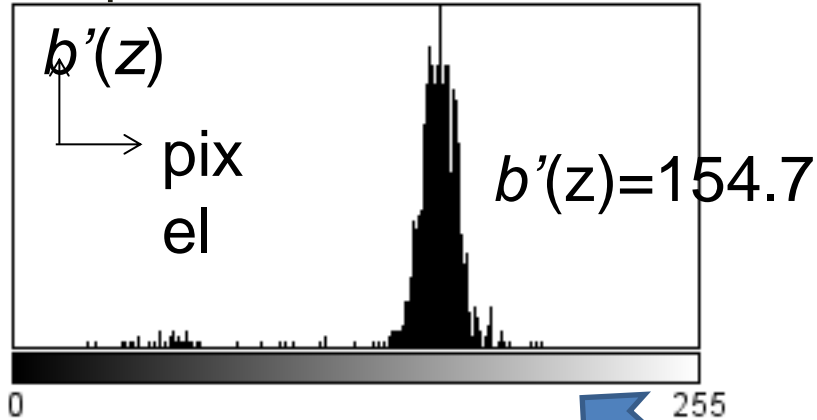
Brightness from the 2D horizontal image by microscope

Brightness Fluctuation by Particle Migration

Brightness fluctuation $b'(z)$

$$b'(z) = \frac{\sqrt{(b(z) - \langle b(z) \rangle)^2}}{\langle b(z) \rangle}$$

Upstream cross-section



Downstream cross-section

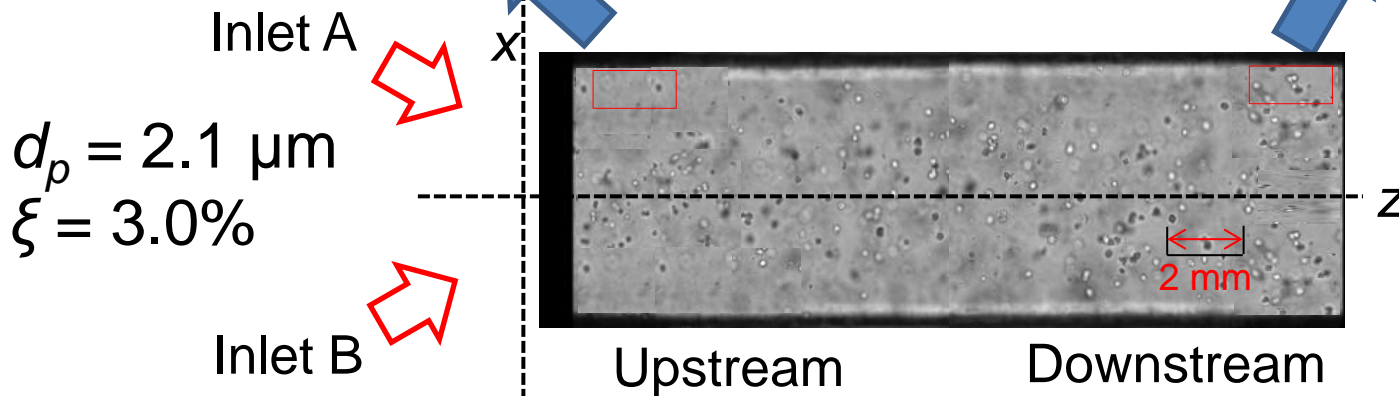
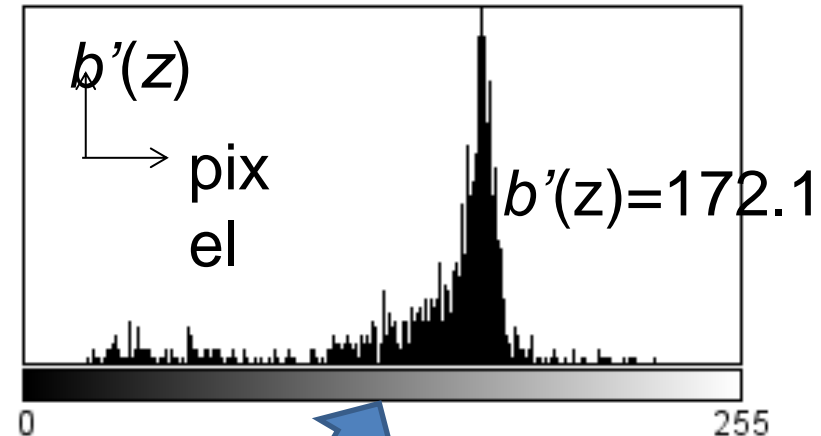


Fig. Histograms of brightness at upstream and downstream by microscope

How to measure in dense particle phase?

Previous Studies of Multi-capacitance Sensing

Multi-capacitance sensing: High speed switching of electrodes

Process tomography: Imaging from multi capacitance data

T. York et al. *Sensors and Actuators A* (2006)

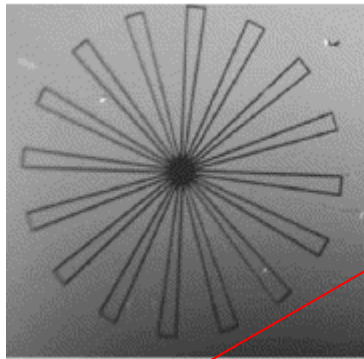
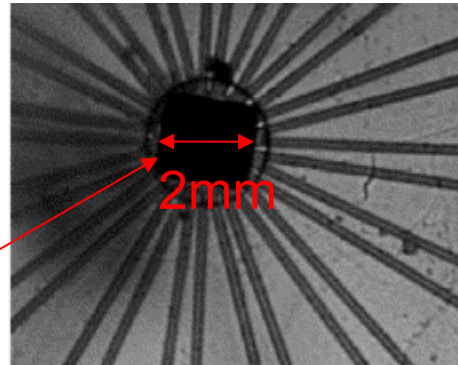


Fig. Hole type mini sensor

- 2 mm diameter
- 12 electrodes



T. Sun et al. *Biosensors and Bioelectronics* (2010)

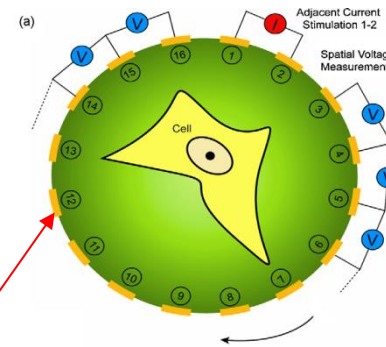
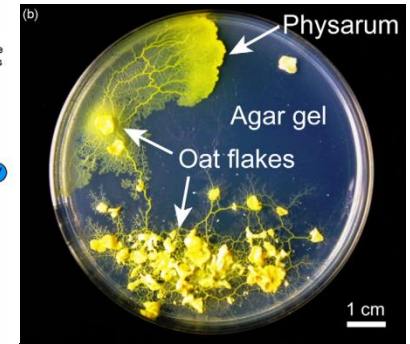


Fig. EIT for imaging single cell in culture in a circular electrode pattern

- 6 mm diameter
- 16 electrodes



Our research originality: Multilayer microchannel by MEMS

- 0.25 μm x 200 μm electrode size
- 700 μm diameter of diamond shape cross-section
- 5 cross-sections with 12 electrodes per one cross-section
- 60 layered electrodes

Microchannel with 60 Layered Electrodes

N. T. A. Othman et al. *Flow Measurement and Instrumentation* (2013)
 Z.Liu, M.Takei et al., *Heat and Mass Transfer*, Springer, (2007)

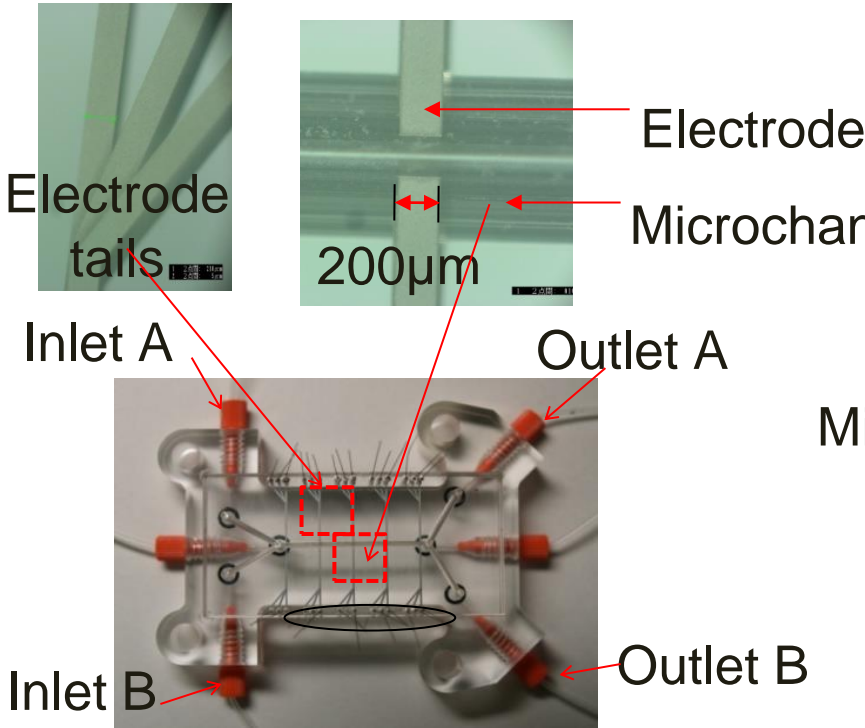


Fig. 60 electrodes of microchannel

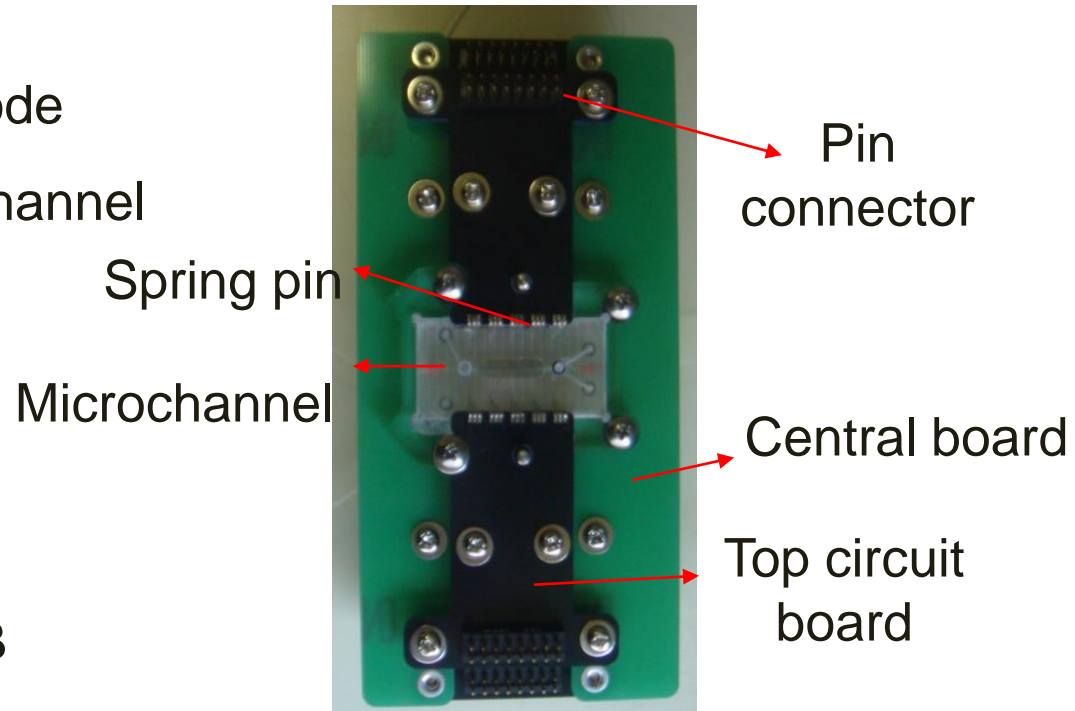
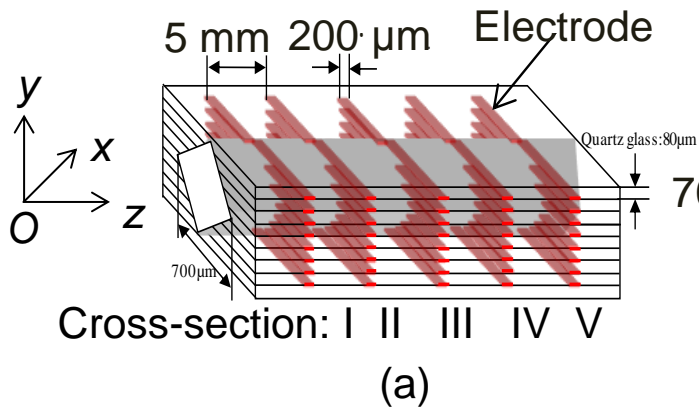
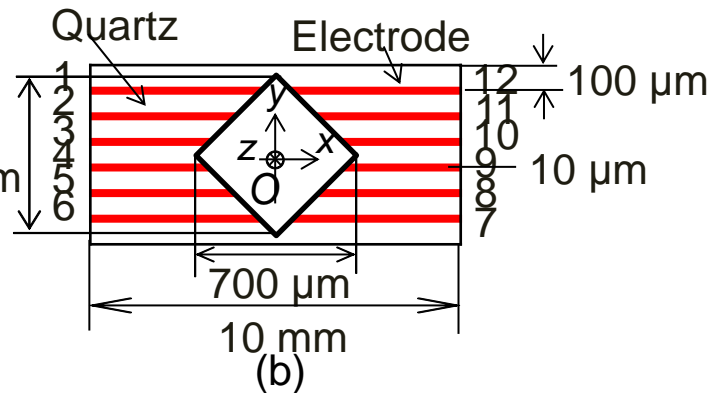


Fig. Microchannel with connector



(a)



(b)

(c)

Fig. (a) 3D microchannel, (b) Cross-sectional and (c) Micro CT microchannel

Fabrication Process of Microchannel

Electrode : Platinum ($2.5\mu\text{m} \times 200\mu\text{m}$)

Substrate of Microchannel : Quartz

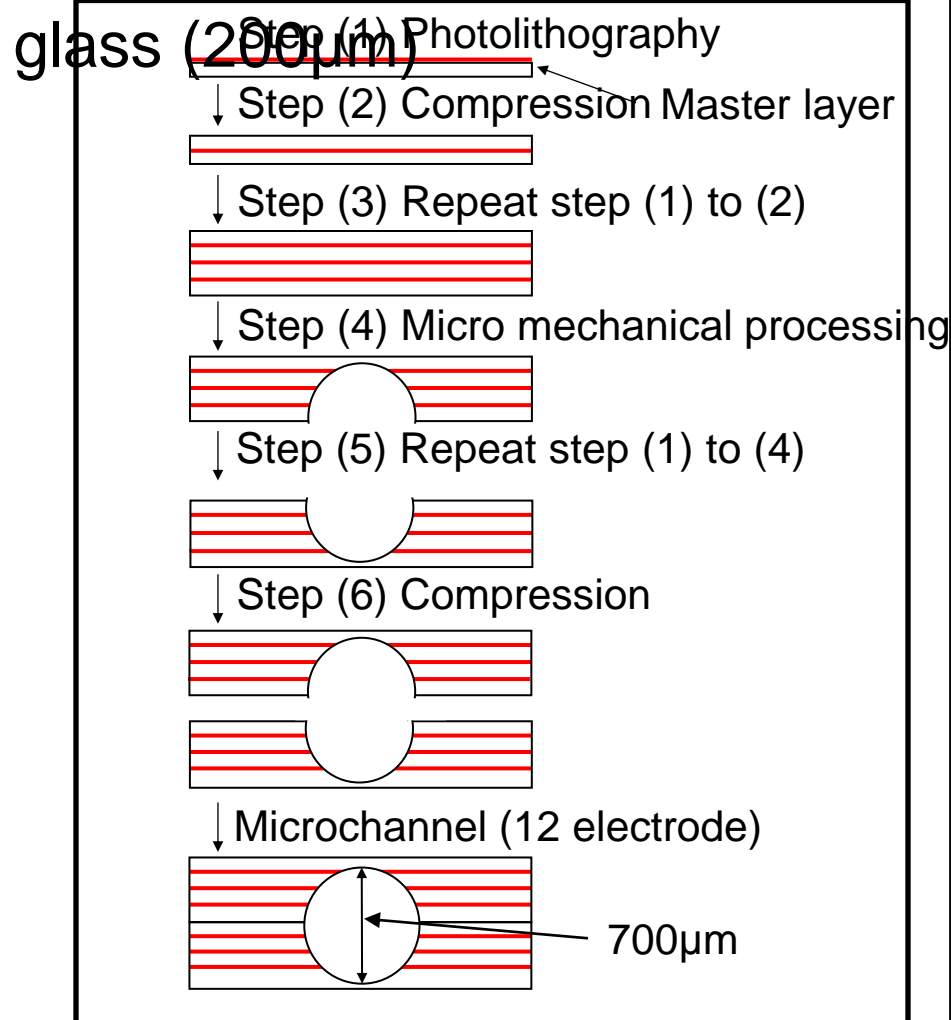


Fig. Cross-section

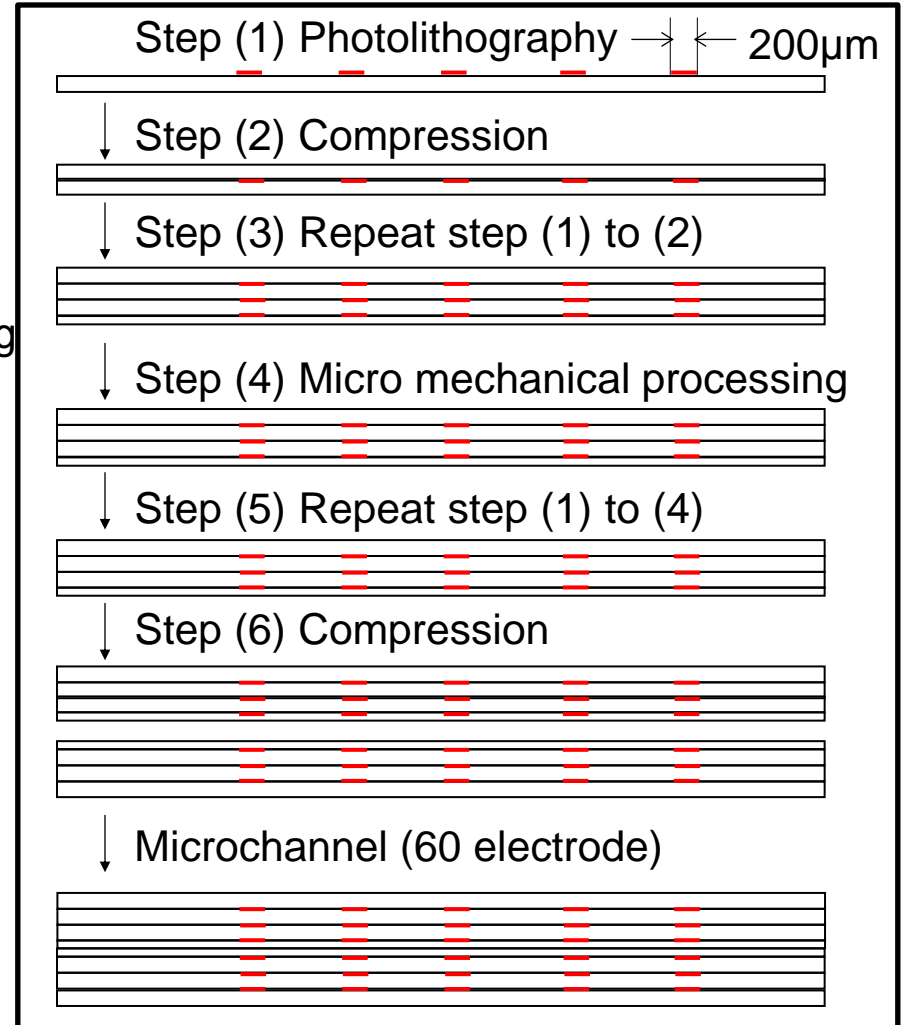
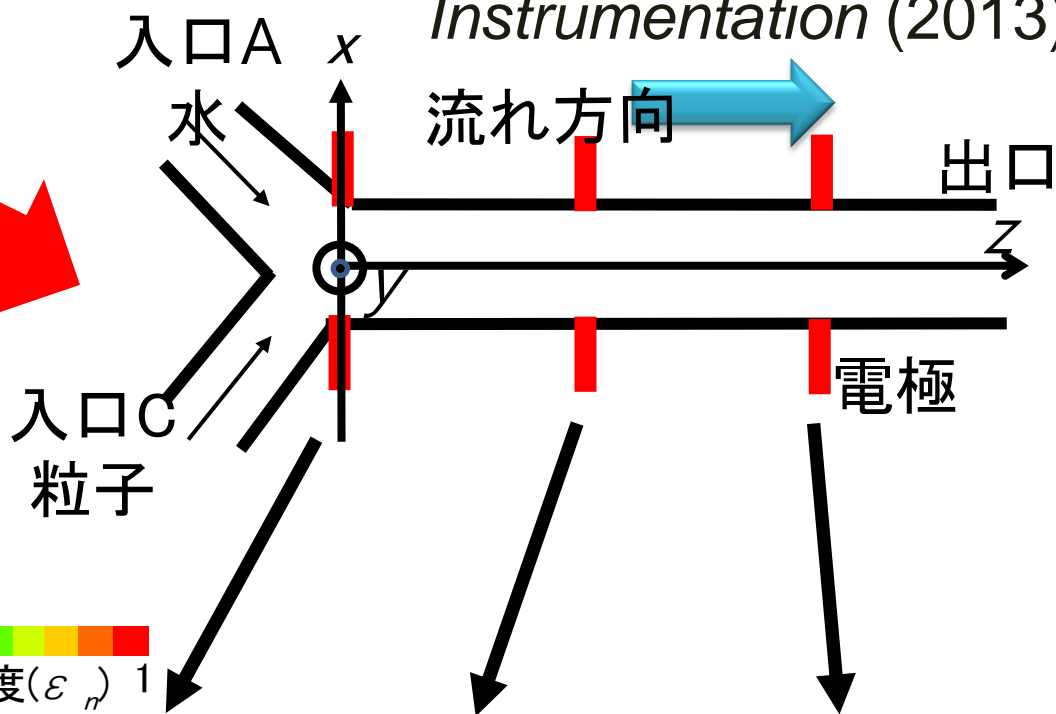
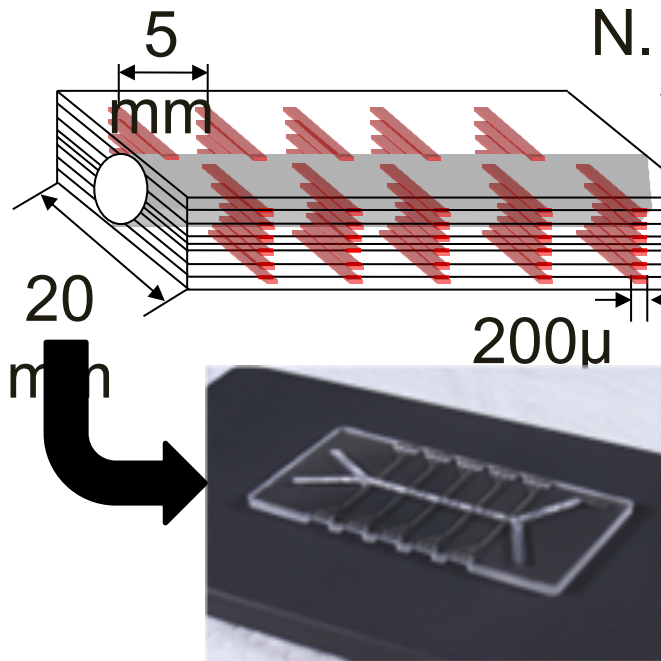


Fig. Radial-section

PT法のマイクロ流路への応用

N. T. A. Othman et al. *Flow Measurement and Instrumentation* (2013)

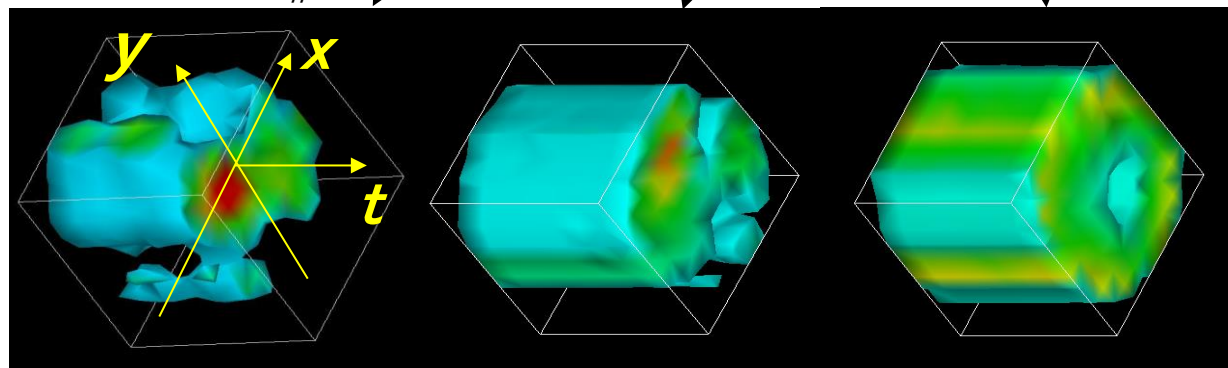


各電極間の電気量の
超高速計測(1 μ s)

0 粒子の濃度(ϵ_n) 1

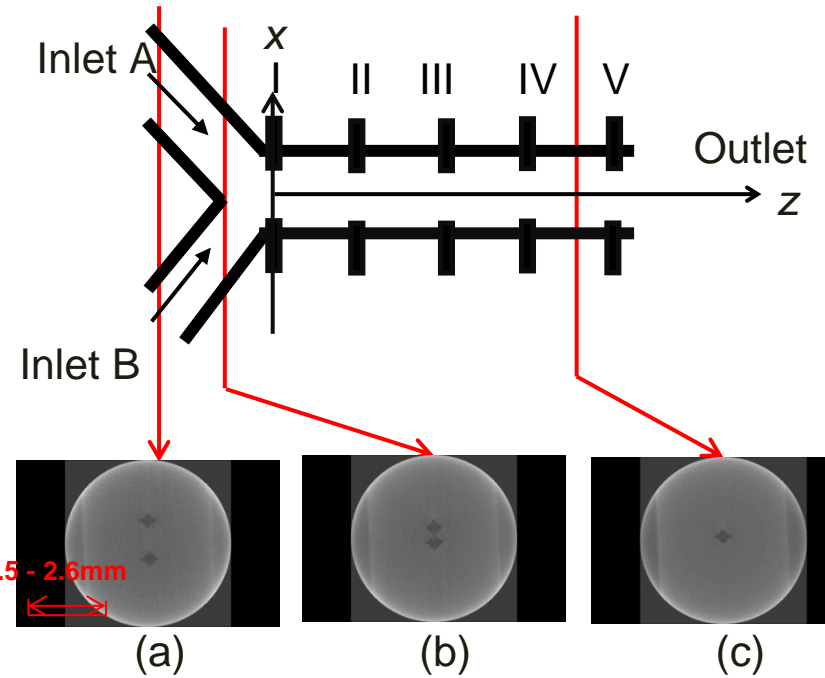
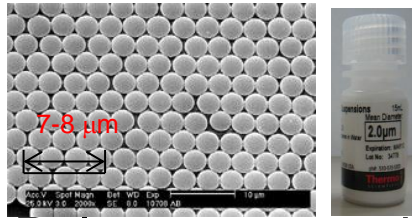
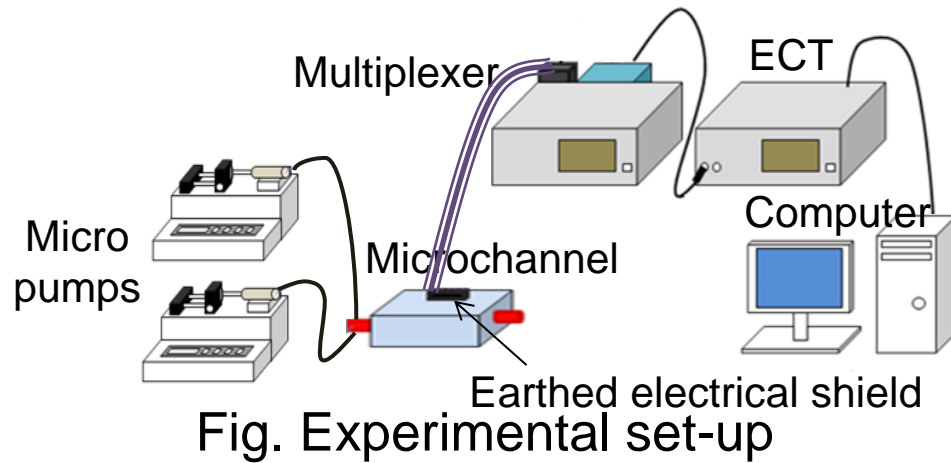
画像再構成

微粒子の濃度分布
の3Dイメージング



垂直断面 I 垂直断面 II 垂直断面 III
図 PT法による微粒子の3D拡散現象のイメージング

Experimental Set-up, Method and Condition #1



Properties of experimental condition

Inlet A and B	Deionized water and particle															
Initial particle concentration ξ [%]	3.0, 5.0 and 10.0															
Particle diameter d_p [μm]	1.3, 1.5 and 2.1															
Cross-section position z [mm] $z^* = z/D$ [-] with $D = 700 \mu\text{m}$ Numbering of cross-section [-]	<table style="width: 100%; text-align: center;"> <tr> <td>$z=0$</td> <td>$z=5$</td> <td>$z=10$</td> <td>$z=15$</td> <td>$z=20$</td> </tr> <tr> <td>$z^*=0$</td> <td>$z^*=7.1$</td> <td>$z^*=14.3$</td> <td>$z^*=21.4$</td> <td>$z^*=28.6$</td> </tr> <tr> <td>I</td> <td>II</td> <td>III</td> <td>IV</td> <td>V</td> </tr> </table>	$z=0$	$z=5$	$z=10$	$z=15$	$z=20$	$z^*=0$	$z^*=7.1$	$z^*=14.3$	$z^*=21.4$	$z^*=28.6$	I	II	III	IV	V
$z=0$	$z=5$	$z=10$	$z=15$	$z=20$												
$z^*=0$	$z^*=7.1$	$z^*=14.3$	$z^*=21.4$	$z^*=28.6$												
I	II	III	IV	V												

Experimental Conditions #2

Liquid phase (non-conductive liquid)		Micro particle phase (dielectric particle)	
Fluid	Deionized water	Particle shape (Duke Scientific Co., USA)	Polystyrene Spherical
Density, ρ^L [kg/m ³]	1000	Density, ρ^P [kg/m ³]	1050
Flow Reynolds number Re	4.0	Particle Reynolds number Rep	0.42
Relative permittivity, ϵ^L	15.0	Relative permittivity, ϵ^P	2.55
Resistivity, ρ^L [Ω m]	1.8×10^5	Resistivity, ρ^P [Ω m]	2.8×10^5
Conductivity, σ^L [S/m]	5.5×10^{-6}	Conductivity, σ^P [S/m]	1.0×10^{-6}
Flow rate, v [μ L/s]	1.0		

Properties of multi capacitance sensing

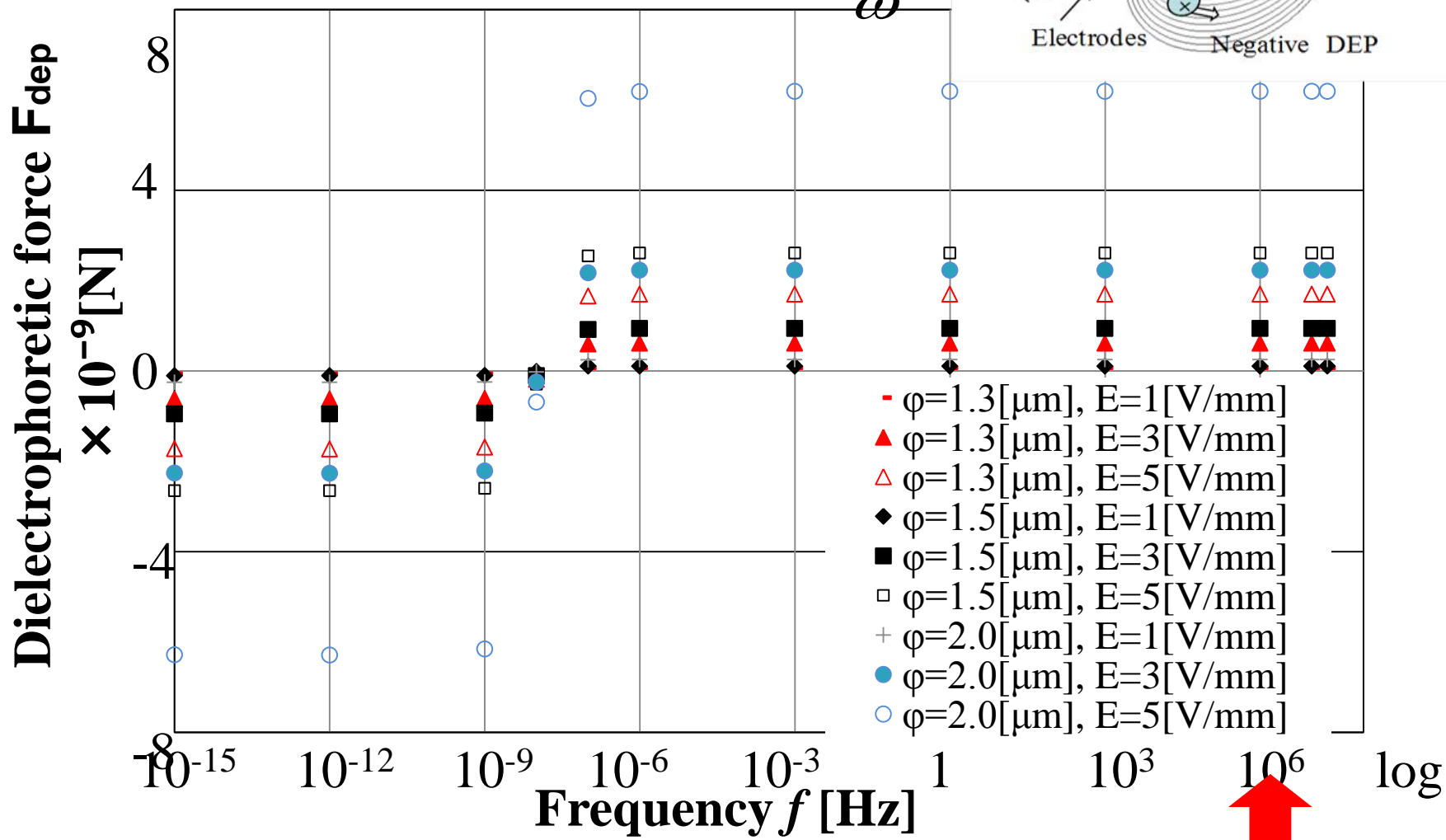
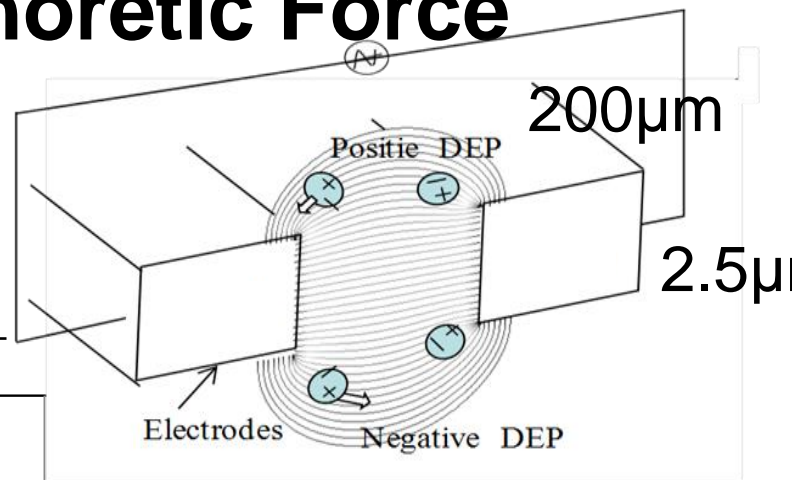
Measurement frequency [MHz]	12.5
Voltage [V]	4.5
Electric fields, E [V/mm] where $E = -\nabla V(l)$	2.0 - 5.0
Sampling time, t [seconds]	100
Data measurement [frame/seconds]	820

Negligible Dielectrophoretic Force

$$F_{\text{dep}} = 2\pi \left(\frac{d}{2}\right)^3 \varepsilon_m \operatorname{Re}[K(\omega)] |\nabla \mathbf{E}|^2$$

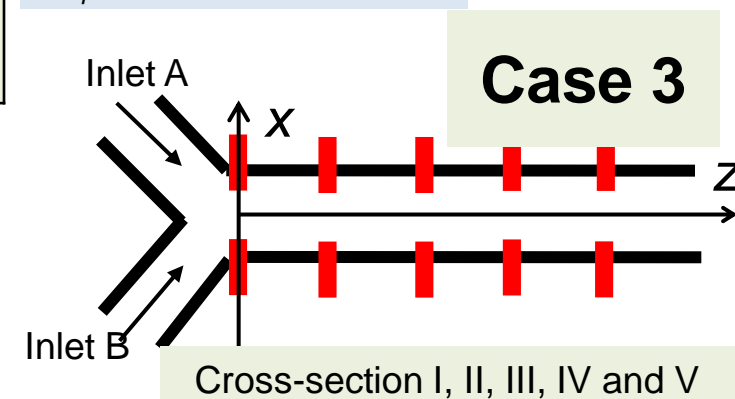
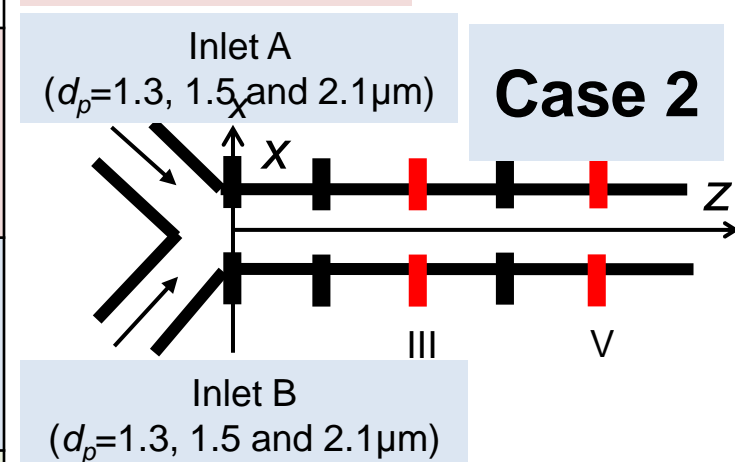
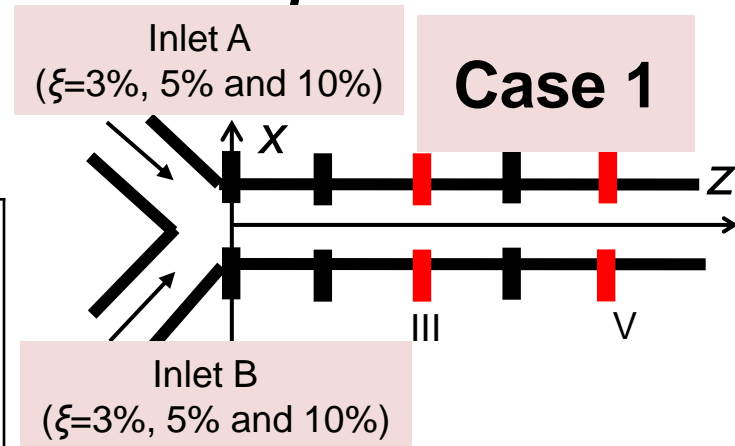
$$K(\omega) = \frac{\varepsilon_p^* - \varepsilon_m^*}{\varepsilon_p^* + 2\varepsilon_m^*} \quad \varepsilon_p^* = \varepsilon_p - j \frac{\sigma_p}{\omega}$$

$$\varepsilon_m^* = \varepsilon_m - j \frac{\sigma_m}{\omega}$$

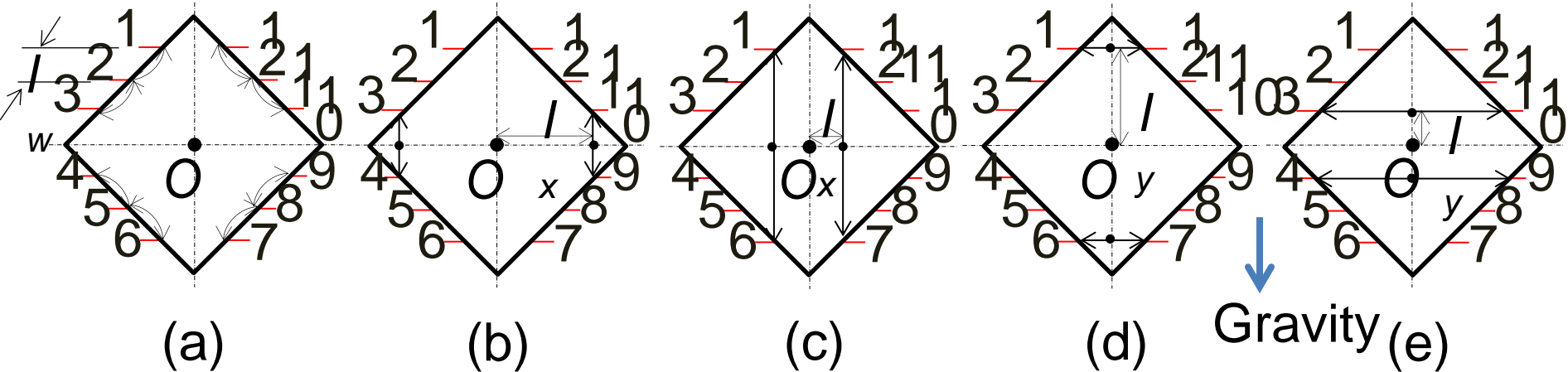


Experimental Conditions #3 --- ξ , d_p and z ---

#	Initial concentration ξ [%]	Particle diameter d_p [μm]	Cross-sectional measurement position z				
			I	II	III	IV	V
1	3.0	2.1			✓		✓
	5.0				✓		✓
	10.0				✓		✓
2	3.0	1.3			✓		✓
		1.5			✓		✓
		2.1			✓		✓
3	10.0	2.1	✓	✓	✓	✓	✓



Configuration Electrode Pair Areas



(a) Adjacent pair (b) Vertical wall (c) Vertical center (d) Horizontal wall (e) Horizontal center

Adjacent pair	Electrode pair, i-j	1-2	2-3	4-5	5-6	7-8	10-11
	Distance between electrode, l_w [μm]		120	120	120	120	120
Vertical pair	Electrode pair, i-j	3-4	2-5	1-6	7-12	8-11	9-10
	Distance electrode from x-axis, l_x [μm]	-300	-180	-60	60	180	300
Horizontal pair	Electrode pair, i-j	1-12	2-11	3-10	4-9	5-8	6-7
	Distance electrode from y-axis, l_y [μm]	-300	-180	-60	60	180	300

Capacitance Measurement Circuit

Conventional circuit

Technical Report of Agilent Technology LCR meter

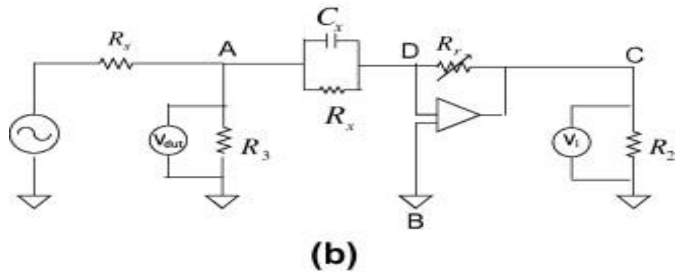
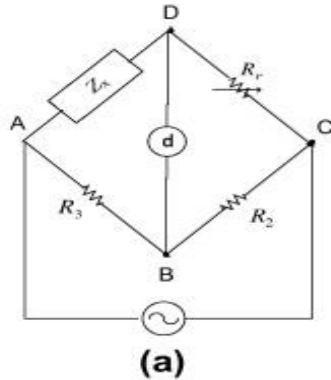


Fig. Equivalent circuit for the capacitance measuring module: (a) Bridge method and (b) Auto balancing bridge method

Equivalent circuit not measure capacitance directly but from reactance.

Direct measurement circuit

W Q Yang, et al., Meas. Sci. Technol. (1997)

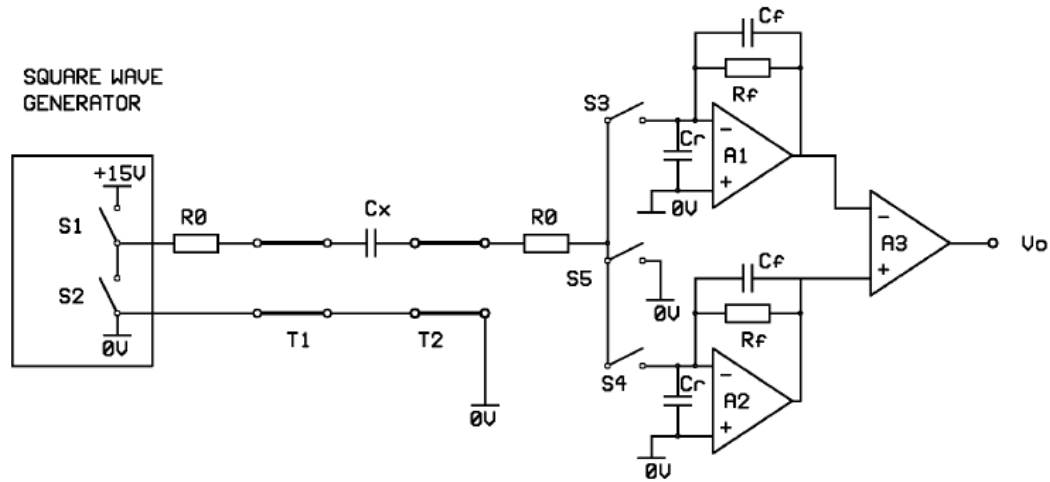
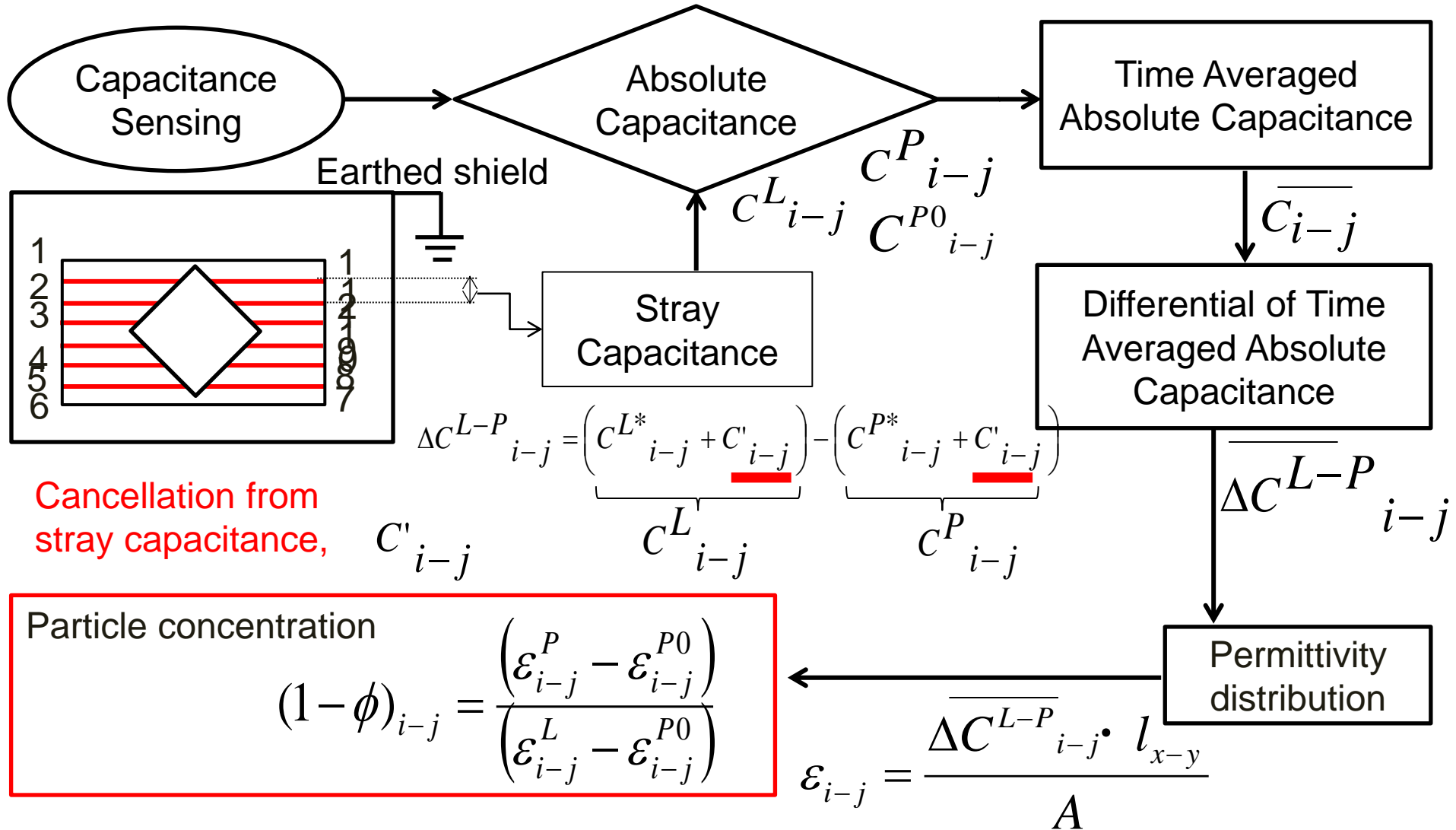


Fig. Direct capacitance measurement circuitry for a single plane of electrodes

- Very small changes in inter-electrode capacitances; order of 10^{-17} Farads (0.01 fF)
- Small capacitances between opposing electrodes (10fF)
- Larger capacitances between adjacent electrodes (500fF) at

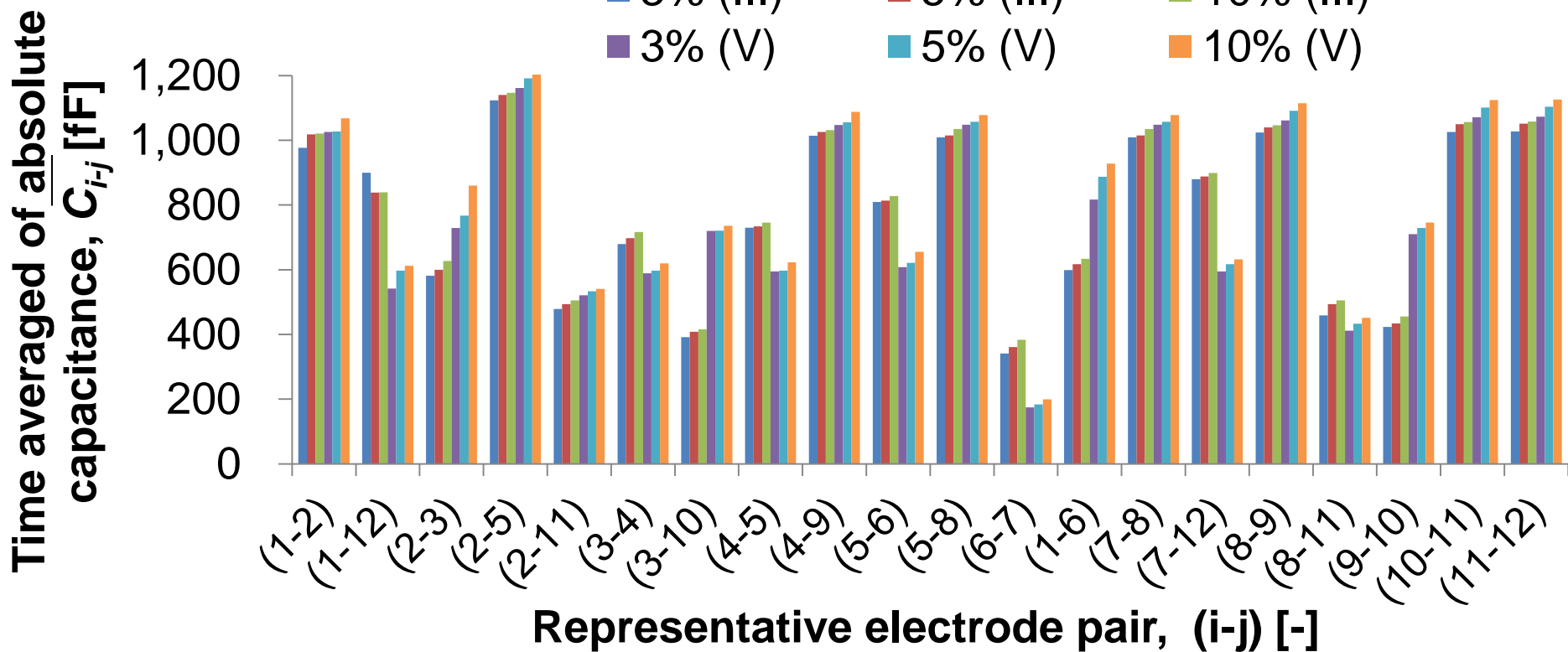
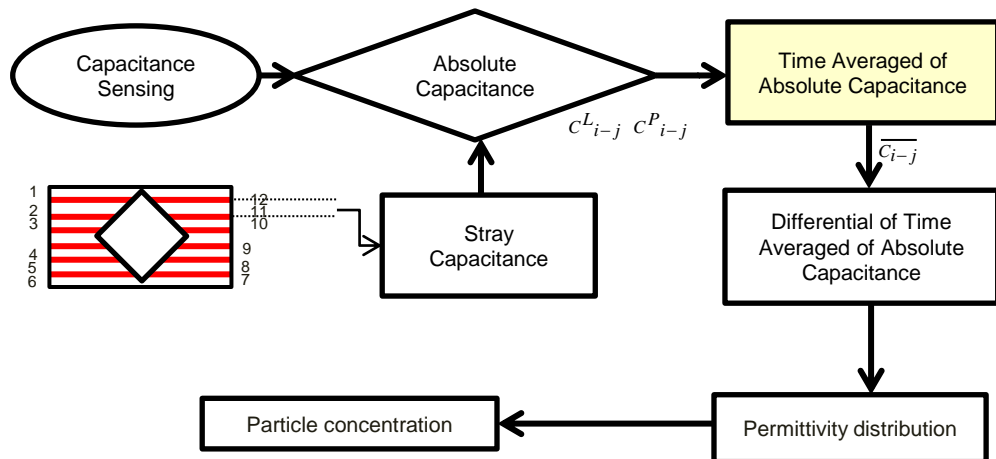
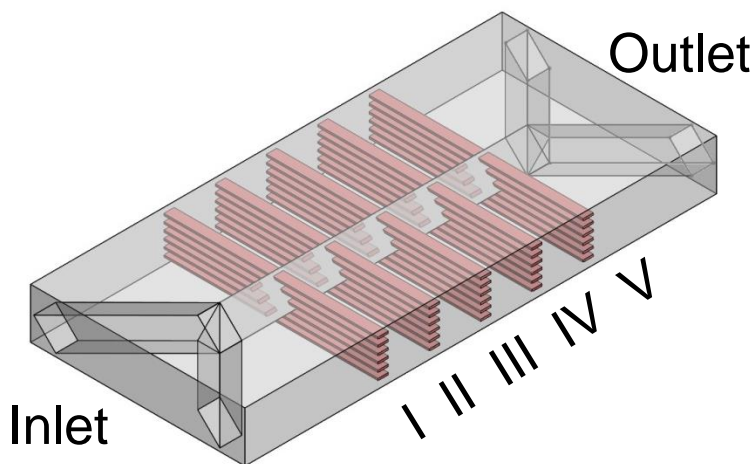
Calculation Process on Particle Concentration



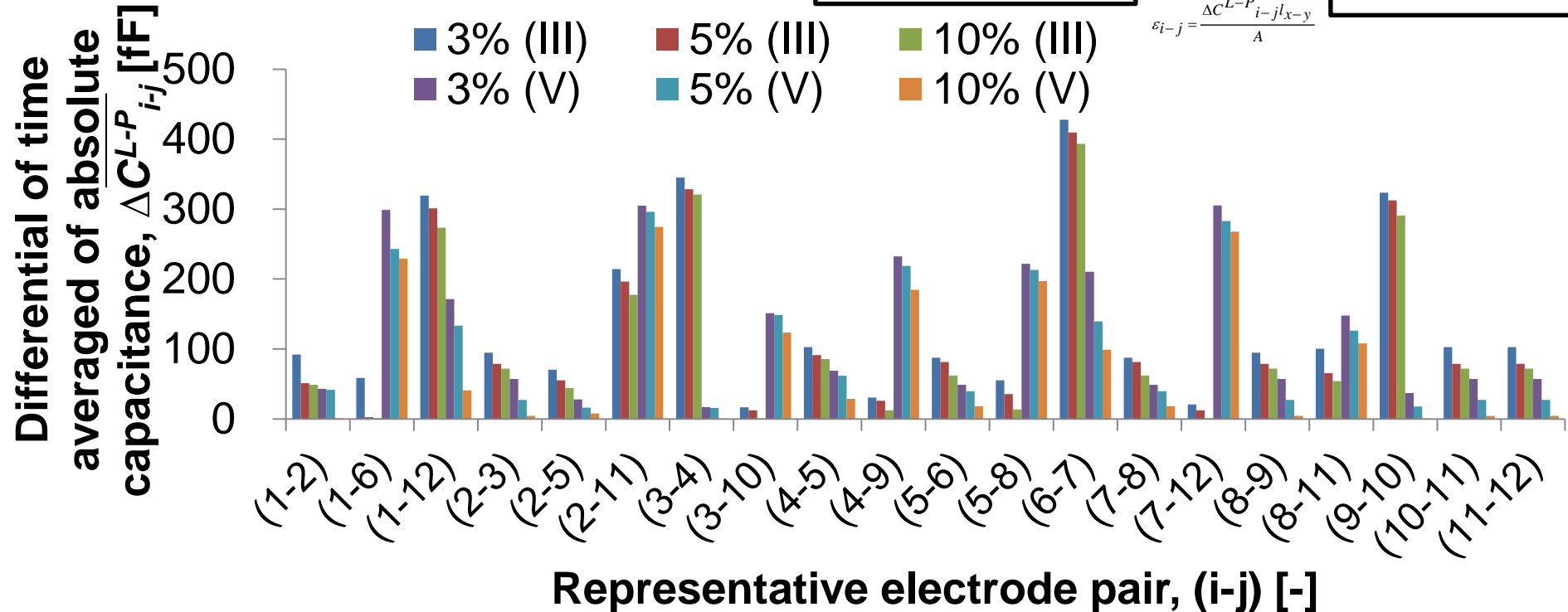
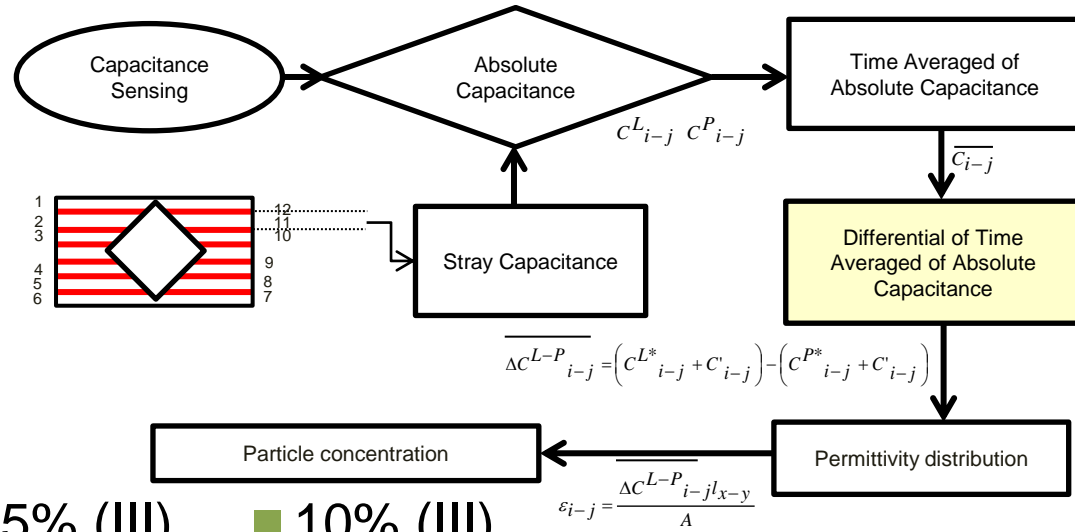
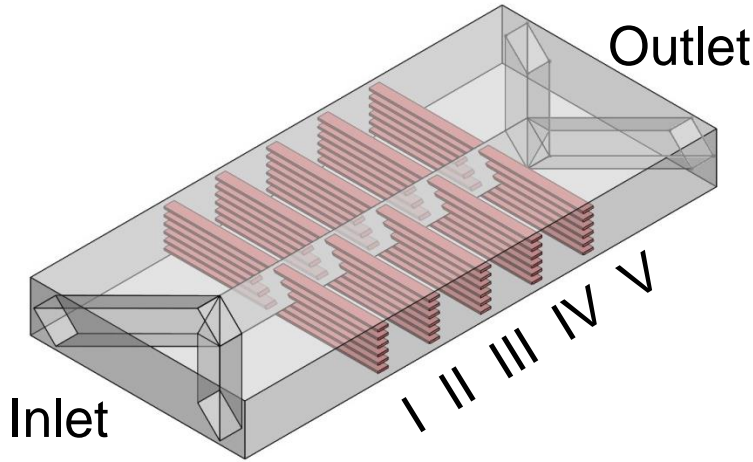
Symbol: C = capacitance, ε = permittivity, $(1 - \phi)$ = particle concentration, l_{x-y} = distance between electrode pair, A = area of electrode, i = source electrode and j = detector electrode

Superscript: L = deionized water flow, $P0$ = static particle, P = particle flow, C^* = actual capacitance value and C' = stray capacitance

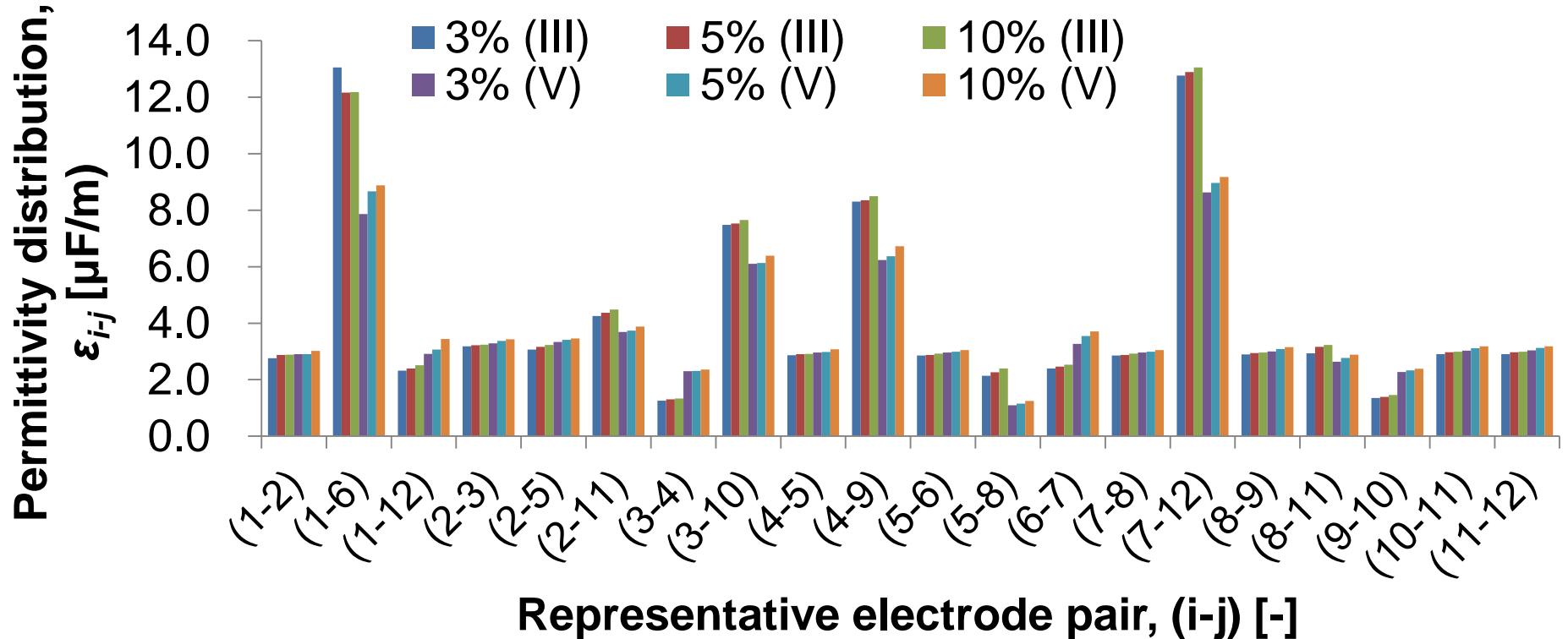
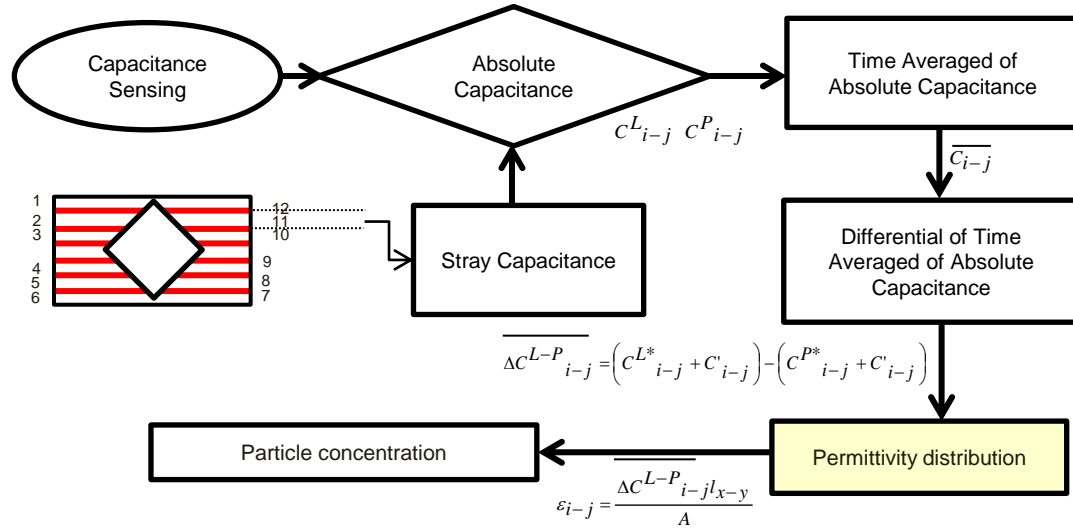
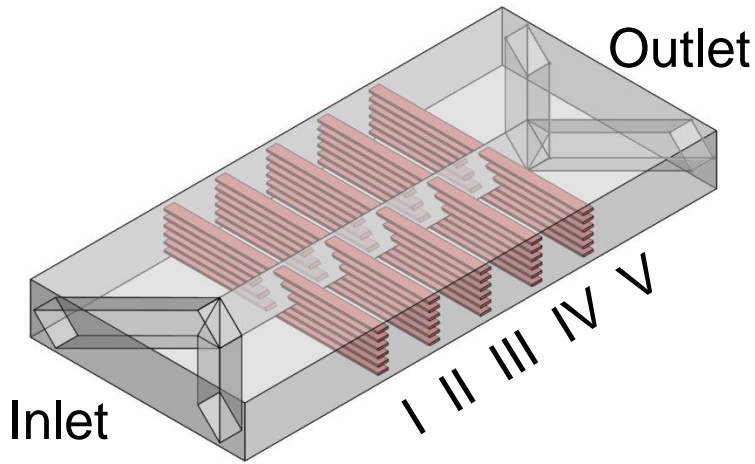
Time Averaged Absolute Capacitance in Case 1



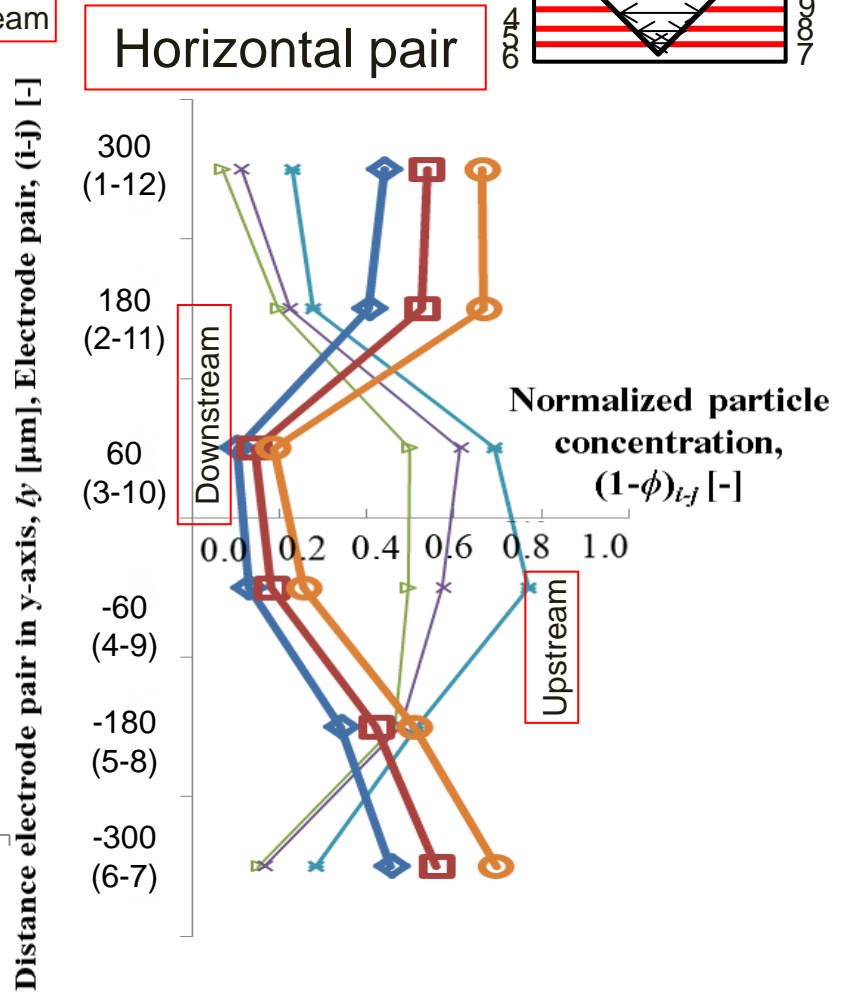
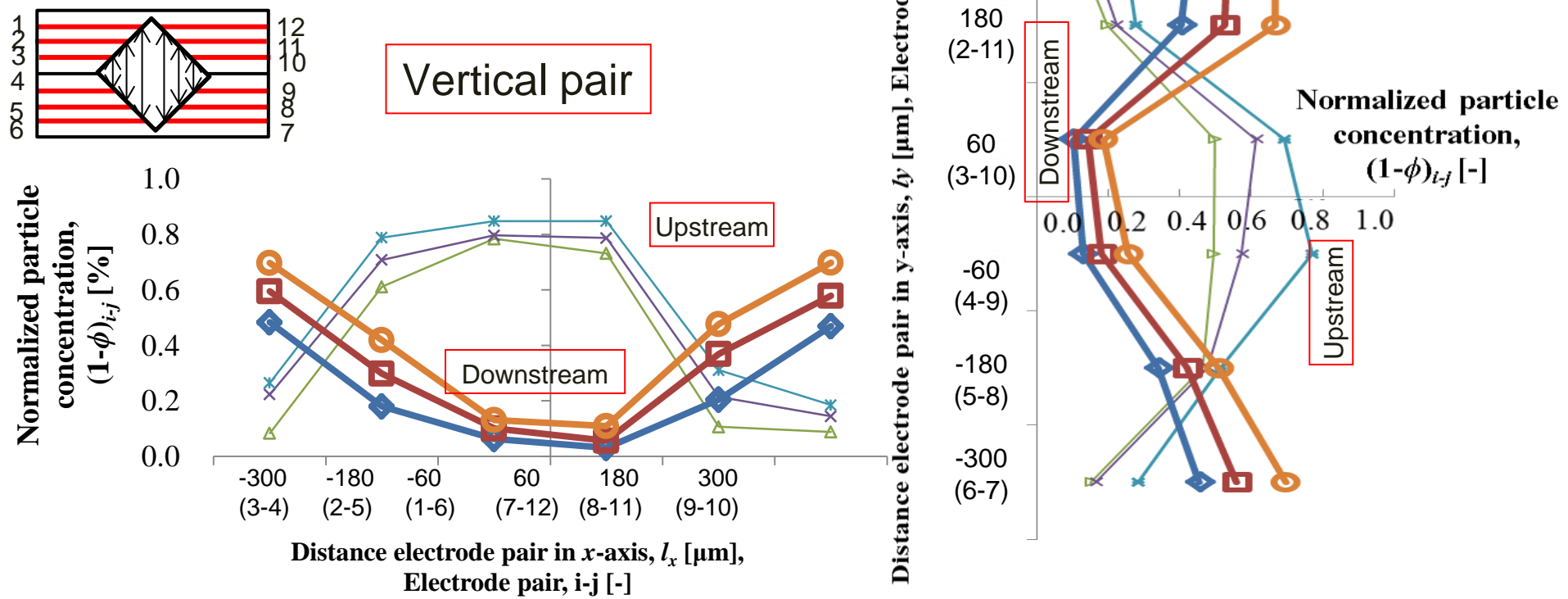
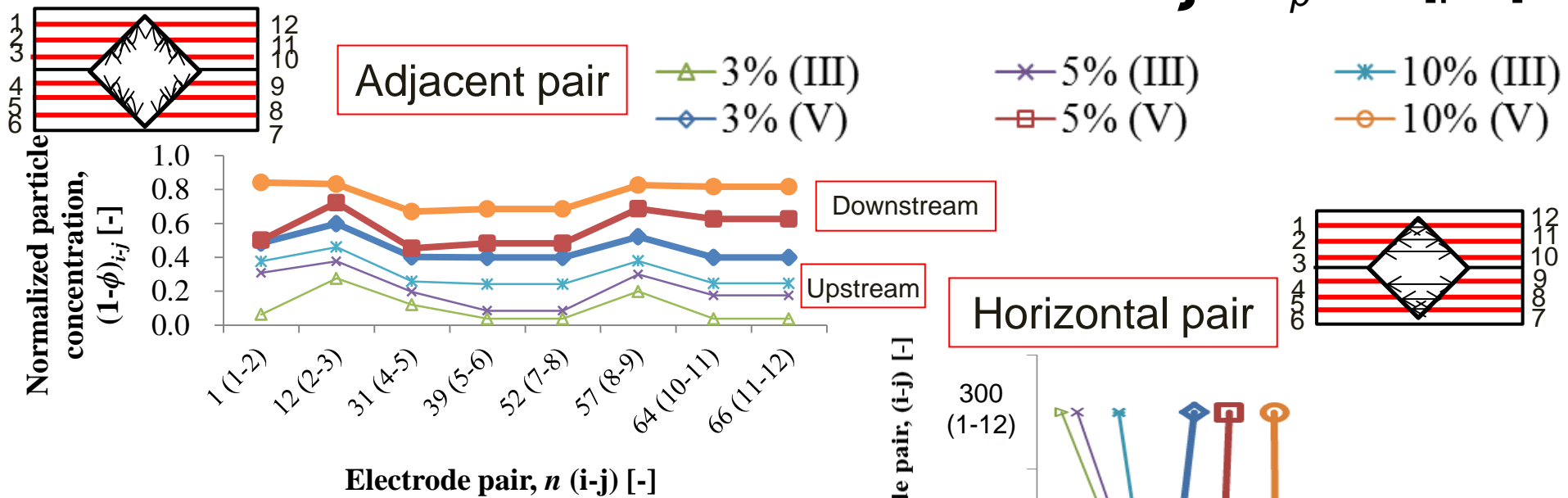
Differential of Time Averaged Absolute Capacitance in Case 1



Permittivity Distribution in Case 1

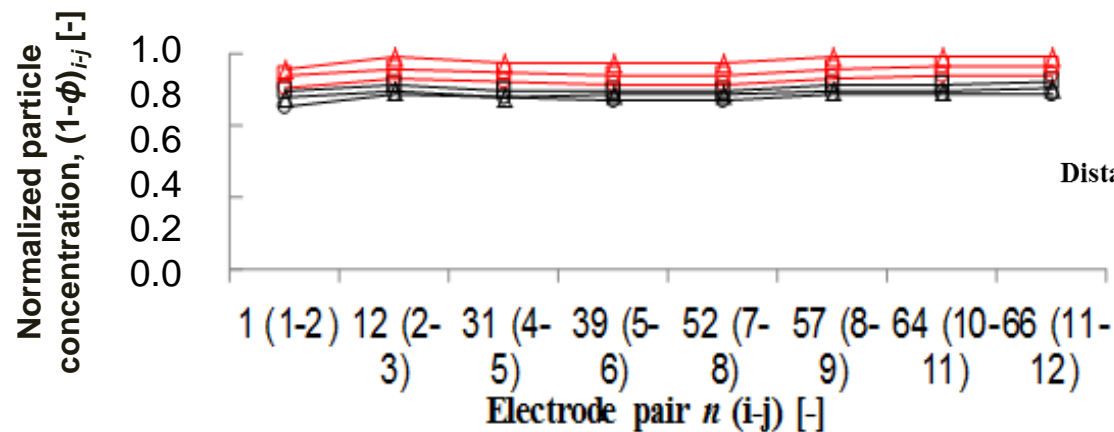


Particle Concentration : Effect of ξ $d_p = 2.1 [\mu\text{m}]$



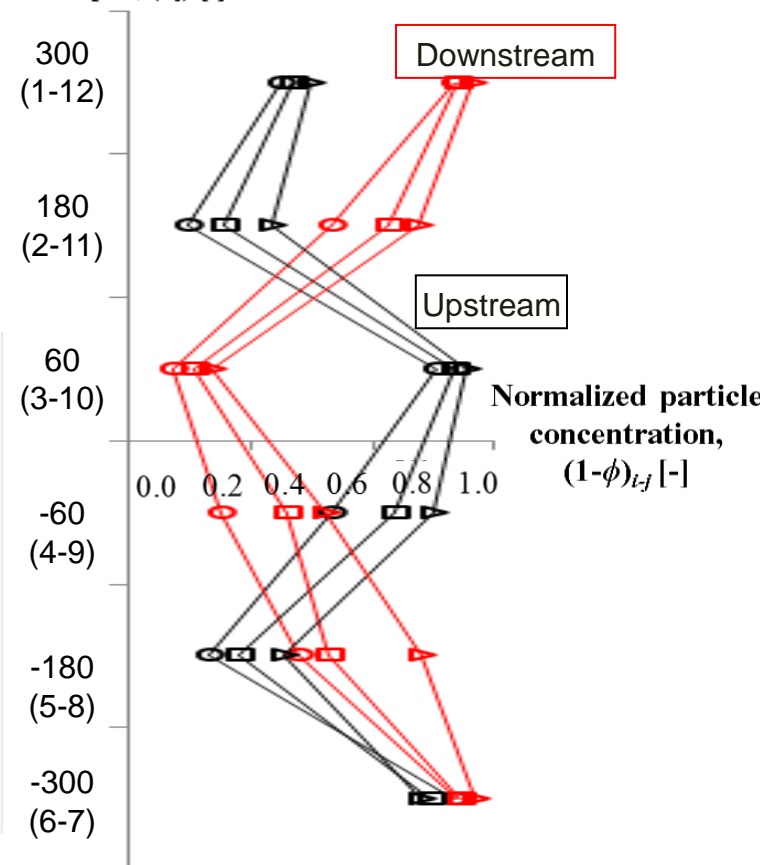
Particle Concentration : Effect of d_p $\xi=3.0[\%]$,

Adjacent pair

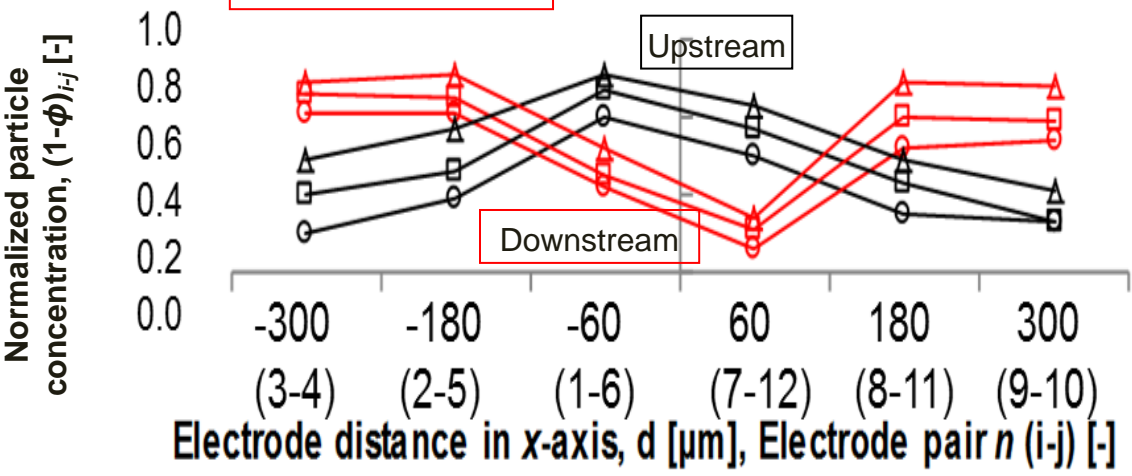


Horizontal pair

Distance electrode pair in y-axis, l_y [μm],
Electrode pair, (i-j) [-]

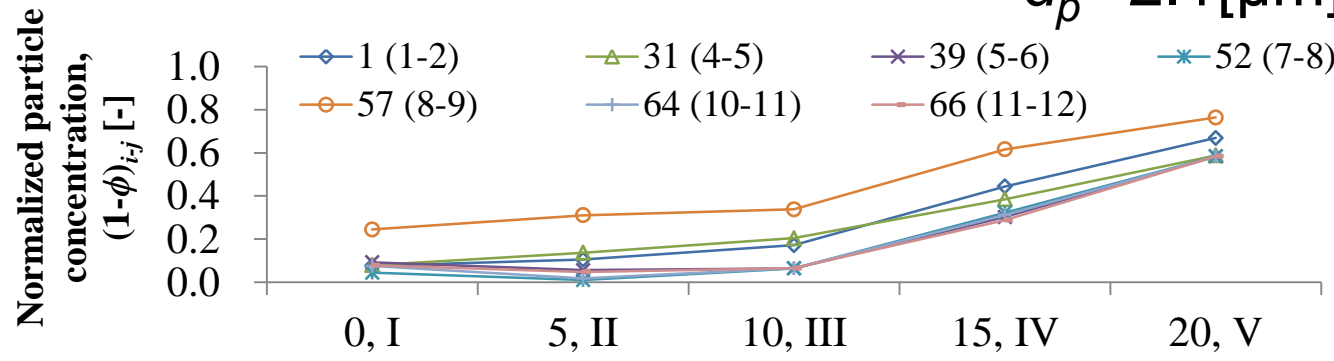


Vertical pair

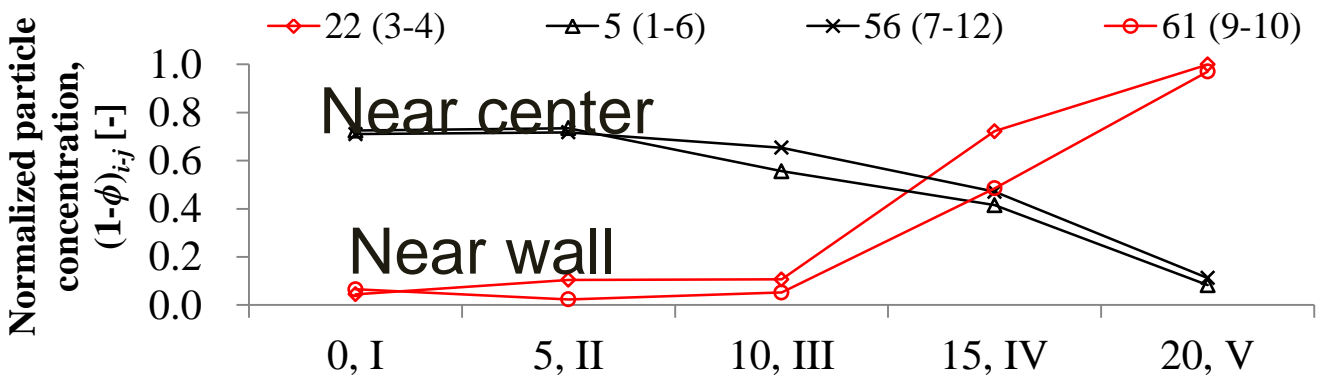


Particle Concentration : Effect of z $\xi=10.0[\%]$, $d_p=2.1[\mu\text{m}]$

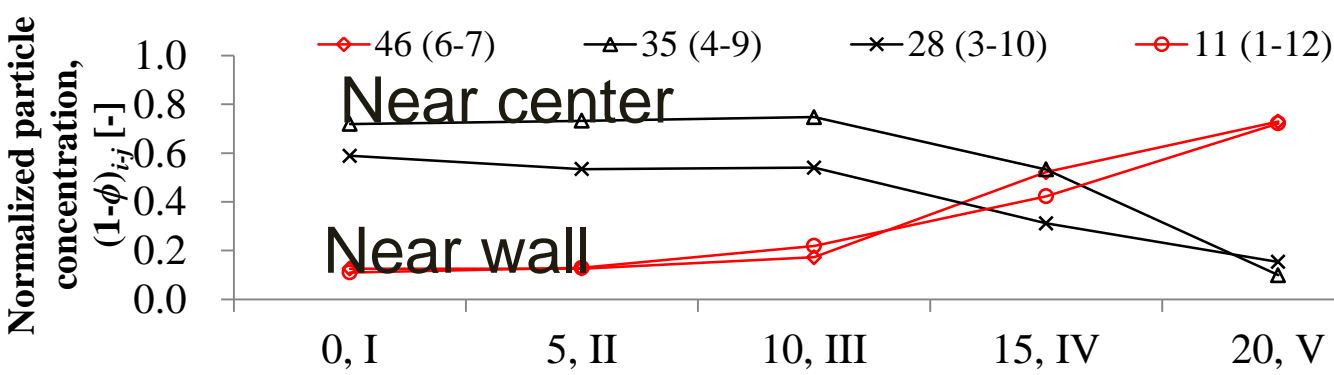
Adjacent pair



Vertical pair



Horizontal pair



Position from inlets, z [mm], Cross-section [-]

Mass Conservation in ξ

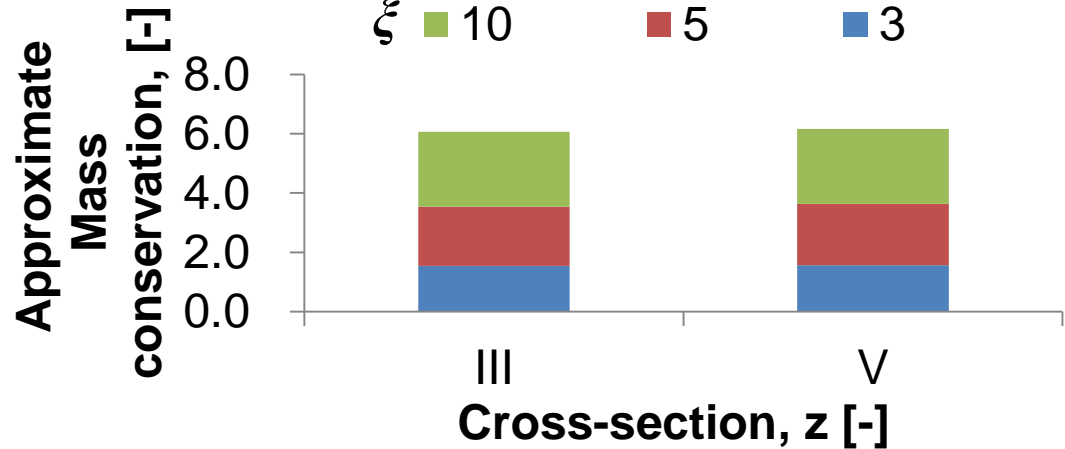
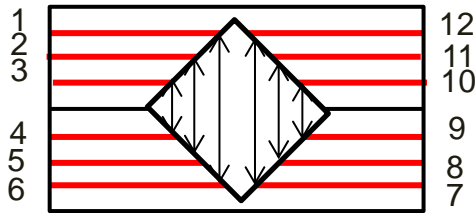
Mass Conservation [kg/s]

$$\iint \rho_p(1 - \phi)u_p dx dy$$

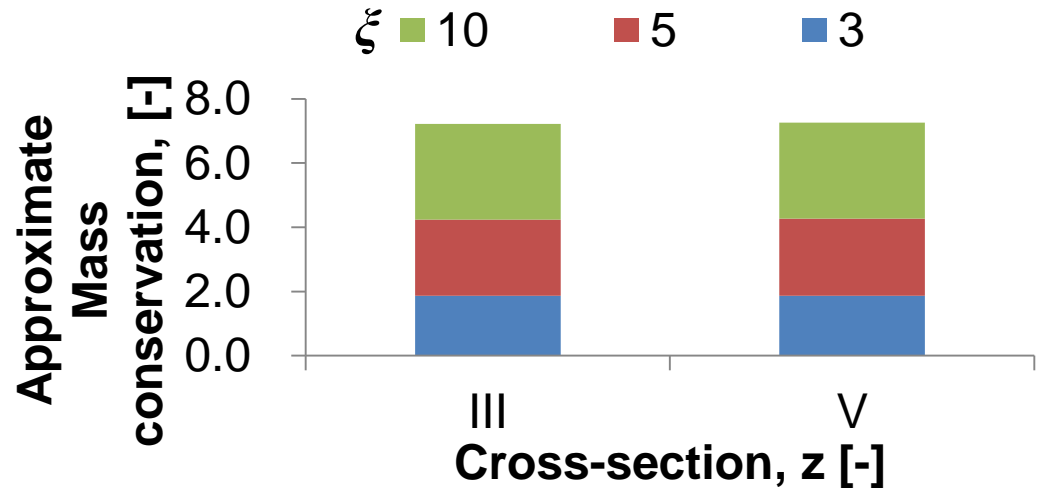
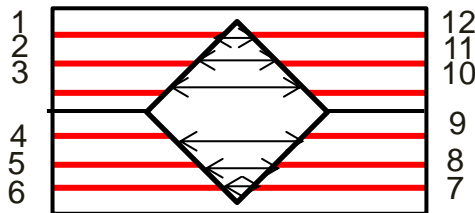
Approximate Mass Conservation [-]

$$\Sigma[\rho_p(1 - \phi)]_{i-j}$$

Vertical pair



Horizontal pair



Particle Migration Ratio Φ --Effect of ξ and z --

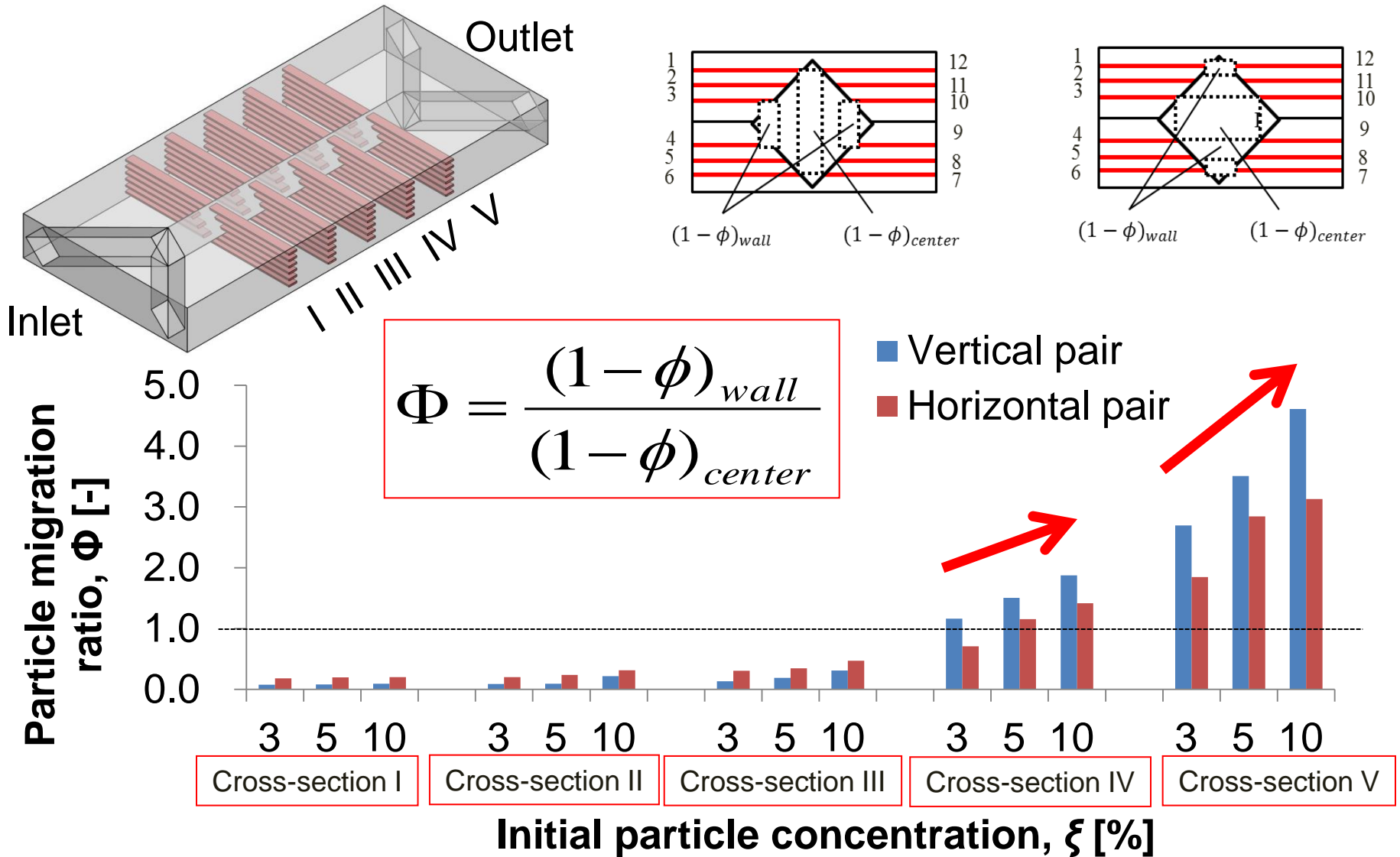


Fig. Particle migration ratio at cross-section I to V, at vertical and horizontal pair for $\xi=3.0, 5.0$ and 10.0%

Particle Migration Ratio Φ -- Effect of d_p --

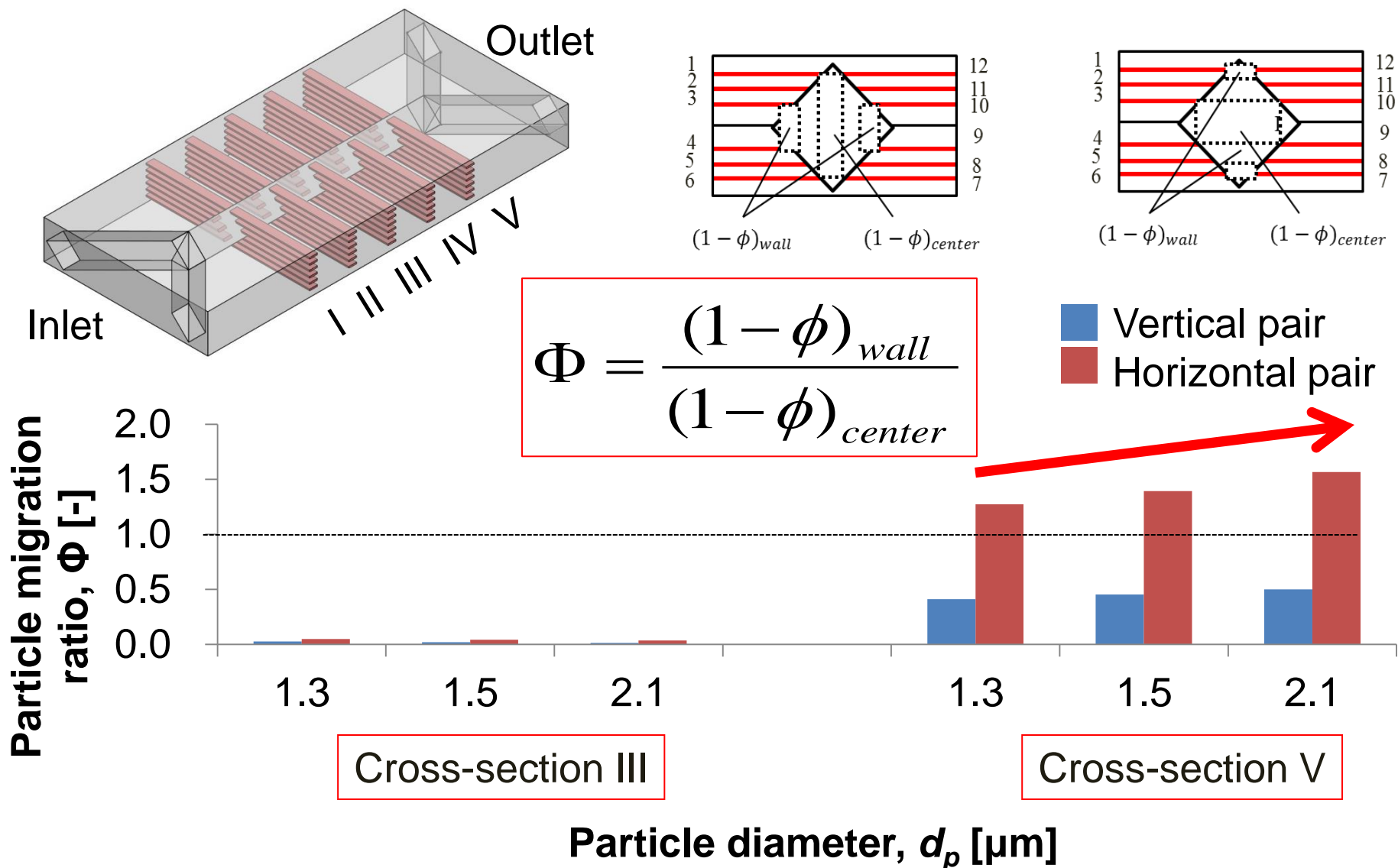
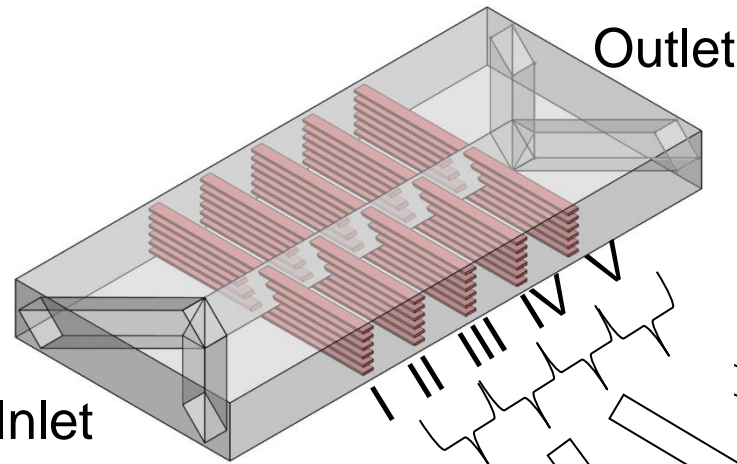


Fig. Particle migration ratio at cross-section III and V, at vertical and horizontal pair for $d_p=1.3 \mu\text{m}$, $1.5 \mu\text{m}$ and $2.1 \mu\text{m}$

Streamline Migration Ψ --Effect of ξ and z --

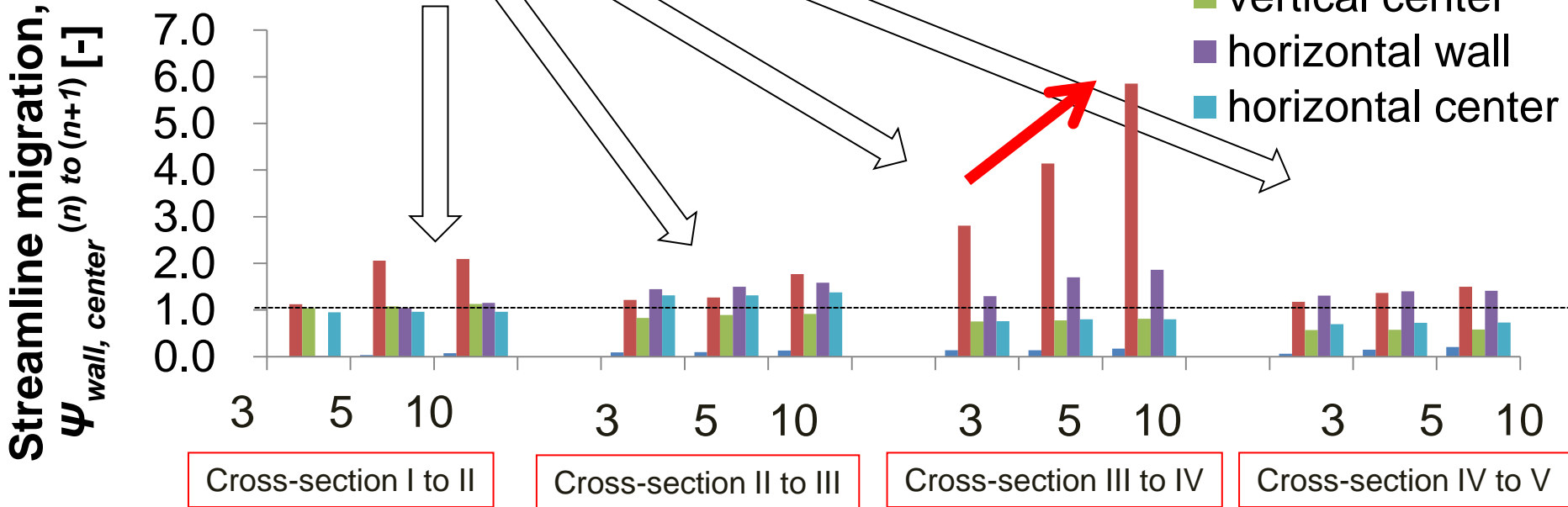
downstream



$$\Psi_{wall,center}^{(n)to(n+1)} = \frac{(1-\phi)_{wall,center}^{(n+1)}}{(1-\phi)_{wall,center}^{(n)}}$$

upstream

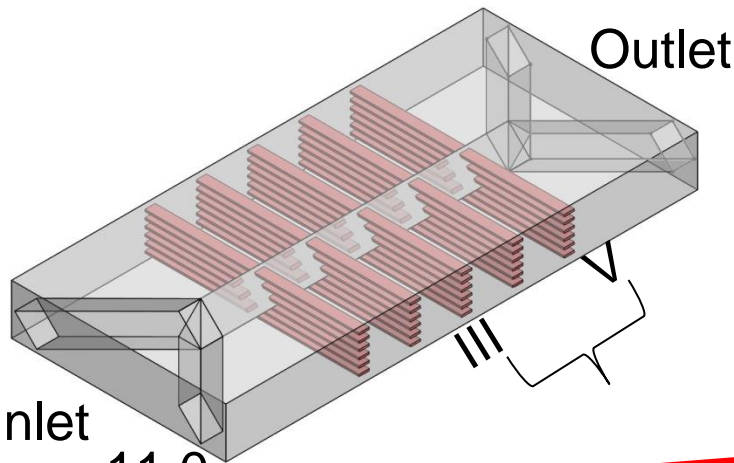
- adjacent
- vertical wall
- vertical center
- horizontal wall
- horizontal center



Initial particle concentration, ξ [%] , streamline transition, z [mm]

Fig. Streamline migration ratio at adjacent, wall and center of vertical and horizontal pair from cross-section I to V at $\xi=3.0, 5.0$ and 10.0%

Streamline Migration Ψ -- Effect of d_p --



$$\Psi_{wall,center}^{(n)to(n+1)} = \frac{(1 - \phi)_{wall,center}^{(n+1)}}{(1 - \phi)_{wall,center}^{(n)}}$$

downstream

upstream

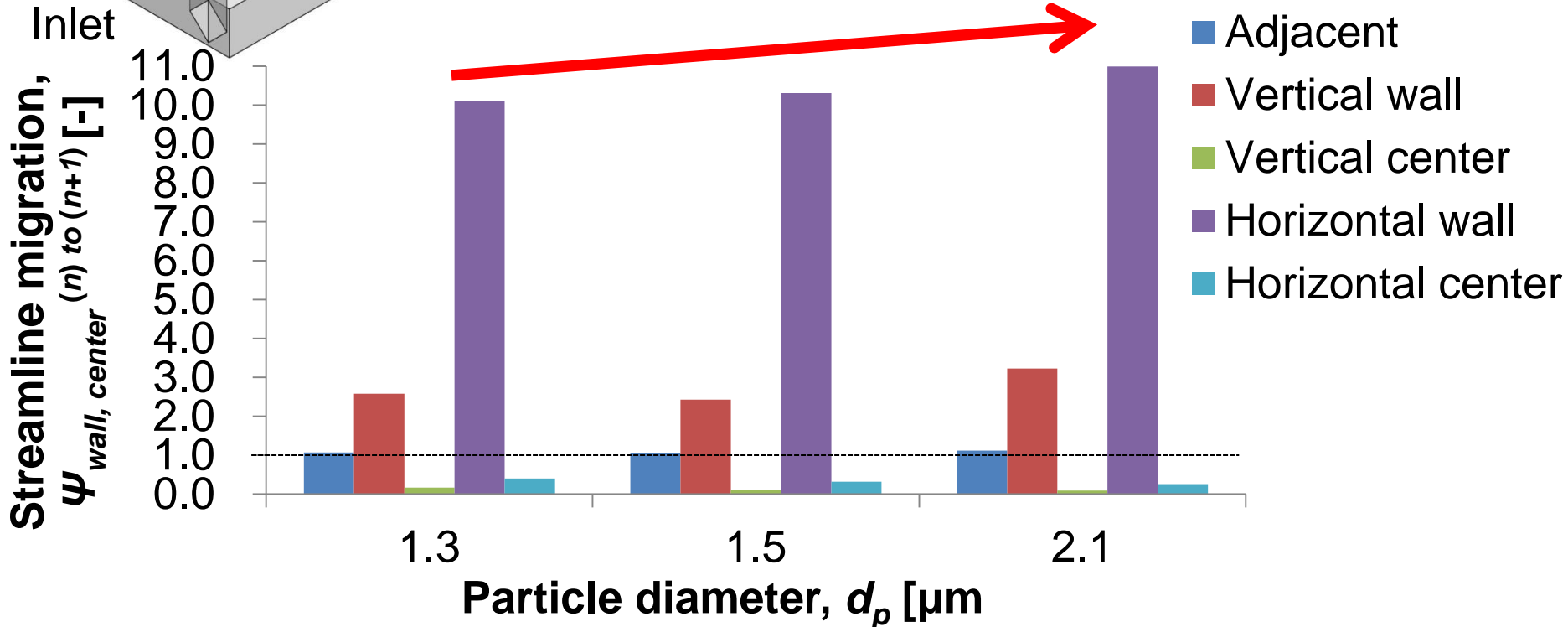


Fig. Streamline migration ratio at adjacent, wall and center of vertical and horizontal pair from upstream to downstream for $d_p=1.3 \mu\text{m}$, $1.5 \mu\text{m}$ and $2.1 \mu\text{m}$

まとめ

- **PTの概要 ソフトフィールドとハードフィールド**
- **ソフトフィールドPT**
 - **原理、プラントへの展開、血流への展開、マイクロ流路への展開**
- **ハードフィールドPT**
 - **Optical CT、X ray CT、 γ ray CT、Neutron Radiography、Ultrasound CT、MRI、Positron Emission Tomography (PET)**

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